08/01/91 [REVISOR] LMB/BD AR1543 1 Department of Health 2 3 Adopted Permanent Rules Relating to Ionizing Radiation 4 5 Rules as Adopted 6 4730.0100 DEFINITIONS. Subpart 1. Scope. For purposes of this chapter, the terms 7 in this part have the meanings given them. 8 Subp. 2. Absorbed dose. "Absorbed dose" means the mean 9 10 energy imparted by ionizing radiation to matter of a known volume-and mass. The special unit of absorbed dose is the rad 11 under the conventional system of measurement and is the gray 12 13 under the SI system of measurement. Subp. 4. Accelerator. "Accelerator" means a device that 14 15 accelerates charged subatomic particles or nuclei to energies useful for research and therapy. 16 Subp. 5. Accelerator-produced material. 17 "Accelerator-produced material" means material made radioactive 18 by a particle accelerator. 19 Subp. 6. Added filtration. "Added filtration" means 20 filtration that is in addition to the inherent filtration. 21 Subp. 7. Aluminum equivalent. "Aluminum equivalent" means 22 the thickness of type 1100 aluminum alloy affording the same 23 attenuation, under specified conditions, as the material in 24 25 question. Subp. 8. Applicator. "Applicator" means an added device 26 that determines the extent of the treatment field at a given 27 distance from the virtual source. 28 Subp. 9. Appropriate limit. "Appropriate limit" or 29 "appropriate limits" means the maximum permissible dose or doses 30 of radiation that may be administered to the whole body or a 31 given part of a human being. 32 Subp. 10. Arc therapy. "Arc therapy" means rotation of 33 34 the beam during irradiation. Subp. 11. [See repealer.] 35

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Subp. 12. Assembler. "Assembler" means a person engaged 1 2 in the business of assembling, replacing, or installing one or more components into an x-ray system or subsystem. Assembler 3 4 includes the owner of an x-ray system or the owner's employee or agent who assembles components into an x-ray system that is 5 6 subsequently used to provide professional or commercial services. 7 Subp. 2. [Renumber as Subp. 13.] Subp. 14. Attenuation block. "Attenuation block" means a 8 block or stack, having dimensions 20 centimeters by 20 9 10 centimeters by 3.8 centimeters, of type 1100 aluminum alloy or other materials having equivalent attenuation. 11 12 Subp. 15. Automatic exposure control (AEC). "Automatic 13 exposure control" or "(AEC)" means a device that automatically controls one or more technique factors to obtain a required 14 quantity of radiation at a preselected location. 15 16 Subp. 16. Beam axis. "Beam axis" means a line from the 17 source through the centers of the x-ray fields. 18 Subp. 17. [See repealer.] Subp. 18. Beam-limiting device (BLD). "Beam-limiting 19 20 device" or "(BLD)" means a device used to restrict the dimensions of the x-ray field. 21 22 Subp. 19. Beam monitoring system. "Beam monitoring system" means a system designed to detect and measure the radiation 23 present in the useful beam. 24 25 Subp. 20. Beam scattering filter. "Beam scattering filter" 26 means a filter or foil used to scatter a beam of electrons. 27 Subp. 21. [See repealer.] Subp. 22. Becquerel (Bq). "Becquerel" or "(Bq)" means a 28 29 unit of measurement of radioactivity. One becquerel is equal to one disintegration per second. One curie is equal to 3.7 x 10^{10} 30 becquerels. Multiples included in these regulations are 31 32 kilobecquerel (kBq), megabecquerel (MBq), gigabecquerel (GBq), terabecquerel (TBq), and petabecquerel (PBq). The conventional 33 34 system equivalent is the curie. Subp. 23. Bucky. "Bucky" means an apparatus under the 35 x-ray table or in a vertical cassette holder that holds the grid 36

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[REVISOR] LMB/BD AR1543 08/01/91 1 and cassette during the radiographic exposure. Subp. 24. By-product material. "By-product material" 2 3 means: 4 A. any radioactive material, except special nuclear 5 material, yielded in or made radioactive by exposure to the radiation incident to the process of producing or using special 6 nuclear material; and 7 8 B. the tailings or wastes produced by the extraction or concentration of uranium or thorium from ore processed 9 primarily for its source material content. 10 11 Subp. 25. C-arm. "C-arm" means an x-ray system in which 12 the image receptor and the x-ray tube housing assembly are 13 connected by a common mechanical support system to maintain a desired spatial relation. 14 Subp. 26. Calibration. "Calibration" means the 15 determination of: 16 17 A. the response or reading of an instrument relative 18 to a series of known radiation values over the range of the instrument; 19 20 в. the strength of a source of radiation relative to a standard; or 21 22 C. the radiation dose rate at a designated distance from a radiation source under specified conditions of 23 24 measurement. 25 For-therapeutic-systems, -the-units-of-calibration-shall-be cGy-(rads)-per-minute-or-cGy-(rads)-per-monitor-unit: 26 27 Subp. 27. [See repealer.] Subp. 27a. Central axis of the beam. "Central axis of the 28 beam" means a line passing through the virtual source and the 29 center of the plane figure formed by the edge of the first 30 beam-limiting device. 31 32 Subp. 28. Cephalometric device. "Cephalometric device" means a device intended for the radiographic visualization and 33 measurement of the dimensions of the human head. 34 Subp. 29. [See repealer.] 35 36 Subp. 30. Certified components. "Certified components"

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means components of x-ray systems that are subject to the x-ray
 equipment performance standards adopted under Public Law Number
 90-602, the Radiation Control for Health and Safety Act of 1968.

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Subp. 31. [See repealer.]

5 Subp. 32. Certified system. "Certified system" means an 6 x-ray system that has one or more certified components.

Subp. 33. Changeable filter. "Changeable filter" means a
filter, exclusive of inherent filtration, that can be removed
from the useful beam through any electronic, mechanical, or
physical process.

Subp. 34. Clinical range. "Clinical range" means the range of control console technique settings that a facility would use in its routine x-ray projections. Quality assurance control tests are performed over clinical ranges.

15 Subp. 35. Coefficient of variation or C. "Coefficient of 16 variation" or "C" means the ratio of the standard deviation to 17 the mean value of a population of observations.

18 Subp. 36. Cold flow. "Cold flow" means the viscous flow 19 of a solid at ordinary temperatures; or, the distortion of a 20 solid under sustained pressure especially with an accompanying 21 inability to return to its original dimensions when pressure is 22 removed.

23 Subp. 4. [Renumber as Subp. 37.]

Subp. 38. Collimator. "Collimator" means a mechanism connected to the x+ray tube housing that controls the dimensions of the primary radiation beam. Types of collimators are cones, diaphragms, and variable-aperture beam-limiting devices.

28 Subp. 5. [Renumber as Subp. 39.]

Subp. 40. Computed tomography (CT). "Computed tomography" or "(CT)" means the production of a tomogram by the acquisition and computer processing of x-ray transmission data.

32 Subp. 41. [See repealer.]

33 Subp. 42. Contact therapy system. "Contact therapy system" 34 means an x-ray system used for therapy with the x-ray tube port 35 placed in contact with or-within-five-centimeters-of the surface 36 being treated.

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1 Subp. 43. Control panel. "Control panel" means the part of the x-ray control located-behind-a-protective-barrier upon 2 which are mounted the switches, knobs, pushbuttons, and other 3 hardware necessary for manually setting the technique factors. 4 Subp. 44. Controlled area. "Controlled area" means a 5 defined area in which the exposure of persons to radiation is 6 under the supervision of a radiation safety officer. (This 7 implies that a controlled area is one that requires control of

10 protection purposes.)

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where:

11 Subp. 45. Coulomb per kilogram (C/kg). "Coulomb per 12 kilogram" or "(C/kg)" means the unit of exposure. One roentgen is equal to 2.58 x 10^{-4} coulomb per kilogram. Submultiples of 13 this unit are the millicoulomb per kilogram (mC/kg) and the 14 15 microcoulomb per kilogram (uC/kg).

access, occupancy, and working conditions for radiation

16 Subp. 46. CT conditions of operation. "CT conditions of 17 operation" means all selectable parameters governing the 18 operation of a CT system including, but not limited to, nominal 19 tomographic section thickness, filtration, and the technique factors as defined in subpart 196. 20

21 Subp. 47. CT dose index (CTDI). "CT dose index" or 22 (CTDI)" means the integral from minus 7T to plus 7T of the dose 23 profile along a line perpendicular to the tomographic plane 24 divided by the product of the nominal tomographic section 25 thickness (T) and the number of tomograms produced in a single 26 scan (n), that is:



34 z = position along a line perpendicular to the tomographic 35 plane;

36 D(z) = dose at position z;

37 T = nominal tomographic section thickness; and

n = number of tomograms produced in a single scan. 38

This definition assumes that the dose profile is centered 39

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around z=0 and that, for a multiple tomogram system, the scan
 increment of adjacent scans is nT.

3 Subp. 48. **CT gantry.** "CT gantry" means the tube housing 4 assemblies, beam-limiting devices, detectors, and supporting 5 structures and frames that hold these components.

6 Subp. 49. **CT number**. "CT number" means the number used to 7 represent the x-ray attenuation associated with each elemental 8 area of the CT image.

9 Subp. 50. Curie (CI). "Curie" or "(Ci)" means a unit of 10 radioactivity. One curie (Ci) is the quantity of radioactive material that decays at the rate of 3.7 x 10^{10} disintegrations 11 12 per second (dps). Commonly used submultiples of the curie are the millicurie and the microcurie. One millicurie (mCi) equals 13 0.001 curie = 3.7×10^7 dps. One microcurie (µCi) equals 14 0.000001 curie = 3.7×10^4 dps. The SI equivalent is the 15 16 becquerel.

17 Subp. 51. Dead-man switch. "Dead-man switch" means a 18 switch so constructed that a circuit-closing contact can be 19 maintained only by continuous pressure on the switch by the 20 operator.

Subp. 52. Densitometer. "Densitometer" means an instrument that measures the <u>optical</u> density of a film by measuring the amount of light transmitted through the film.

Subp. 53. Diagnostic source assembly. "Diagnostic source assembly" means the tube housing assembly with a beam-limiting device attached.

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Subp. 9. [Renumber as Subp. 54.]

28 Subp. 55. Diagnostic radiographic imaging system.

29 "Diagnostic radiographic imaging system" means an assemblage of 30 components for the generation, transmission, and reception of an 31 x-ray and the transformation, storage, and visual display of the 32 resultant radiographic image.

33 Subp. 56. Diagnostic radiographic system. "Diagnostic 34 radiographic system" means an x-ray system designed for 35 irradiation of any part of the human or animal body for 36 diagnosis or visualization.

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Subp. 57. Dose. "Dose" means absorbed dose or dose
 equivalent as appropriate.

3 Subp. 58. Dose commitment. "Dose commitment" means the 4 total radiation dose to a part of the body that will result from 5 retention in the body of radioactive material. For purposes of 6 estimating the dose commitment, it is assumed that from the time 7 of intake the period of exposure to retained material will not 8 exceed 50 years.

9 Subp. 59. Dose equivalent (DE). "Dose equivalent" or "(DE)" means a quantity used for radiation protection purposes 10 11 that expresses on a common scale for all radiations the 12 1 irradiation incurred by exposed persons. It is defined as the 13 product of the absorbed dose and the quality factor. For x rays 14 and gamma rays, the dose equivalent in rems is usually assumed 15 to be numerically equal to either the exposure in roentgens or 16 the absorbed dose in rads. The special unit dose equivalent is 17 the rem under the conventional measurement system and is the sievert under the SI measurement system. 18

19 Subp. 60. Dose monitoring system. "Dose monitoring system" 20 means a system of devices for the detection, measurement, and 21 display of quantities of radiation that can be related to the 22 absorbed dose at a given location within a defined geometry.

Subp. 61. Dose monitor unit. "Dose monitor unit" means a unit response from the dose monitoring system from which the absorbed dose has been calculated.

26 Subp. 62. Dose profile. "Dose profile" means the dose as 27 a function of position along a particular plane.

Subp. 63. Effective dose equivalent. "Effective dose equivalent" means the sum over specified tissues of the products of the dose equivalent in a tissue and the weighting factor for that tissue.

32 Subp. 64. Electron-beam generator. "Electron-beam 33 generator" means a type of electron accelerator in which the 34 electron beam is brought out into the atmosphere for irradiation 35 purposes.

36 Subp. 65. Elemental area. "Elemental area" means the

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1 smallest area within a tomogram for which the x-ray attenuation
2 properties of a body are depicted.

3 Subp. 66. Entrance exposure rate. "Entrance exposure rate" 4 means the exposure per unit of time at the point where the 5 center of the useful beam enters the patient.

6 Subp. 67. ESE. "ESE" means the entrance skin exposure 7 that is measured free in air.

8 Subp. 68. Exposure. For purposes of part 4730.2150, 9 "exposure" means the quotient of dQ by dm where dQ is the 10 absolute value of the total charge of the ions of one sign 11 produced in air when all the electrons (negatrons and positrons) 12 liberated by photons in a volume element of air having mass (dm) 13 are completely stopped in air. The unit of exposure is the 14 <u>Roentgen (R).</u>

15 Subp. 69. Exposure rate. "Exposure rate" means the 16 exposure per unit of time, such as roentgen per minute and 17 milliroentgen per hour.

18 Subp. 70. Facility. "Facility" means the location at 19 which one or more sources of radiation are installed or located 20 within one building, vehicle, or under one roof, and are under 21 the same administrative control.

Subp. 71. Field emission equipment. "Field emission equipment" means equipment that uses an x-ray tube in which electron emission from the cathode is due solely to the action of an electric field.

Subp. 72. Field-flattening filter. "Field-flattening filter" means a permanent filter used to provide dose uniformity over the area of a useful beam of x-rays at a specified depth. Subp. 73. Filter or filtration. "Filter" or "filtration"

30 means material placed in the useful beam to absorb 31 preferentially selected radiations.

32 Subp. 74. Fluoroscopic imaging assembly. "Fluoroscopic 33 imaging assembly" means a subsystem in which x-ray photons 34 produce a fluoroscopic image. It includes image receptors such 35 as the image intensifier and spot-film device, electrical 36 interlocks, if any, and structural material providing linkage

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1 between the image receptor and diagnostic source assembly.

2 Subp. 75. Focal spot. "Focal spot" means the area of the 3 anode from which x-rays originate.

4 Subp. 76. Gantry. "Gantry" means the part of the system 5 supporting and allowing possible movements of the radiation head.

Subp. 77. General purpose radiographic x-ray system.
"General purpose radiographic x-ray system" means a radiographic
x-ray system that, by design, is not limited to radiographic
examination of specific anatomical regions.

10 Subp. 78. Gonad shield. "Gonad shield" means a protective 11 barrier for the testes or ovaries.

Subp. 79. Gray (Gy). "Gray" or "(Gy)" means the unit of absorbed dose equal to one joule per kilogram. One rad gray is equal to $\pm -x - \pm \theta = 2 - gray \pm 100$ rad. Submultiples included in these regulations are the milligray (mGy), the microgray (μ Gy) and the centigray (cGy). The conventional system equivalent is the rad.

17 Subp. 80. Half-value layer (HVL). "Half-value layer" or 18 "(HVL)" means the thickness of a specified material that 19 attenuates the beam of radiation to such an extent that the 20 exposure rate is reduced to one-half of its original value. The 21 contribution of all scattered radiation, other than any that 22 might be present initially in the beam concerned, is considered 23 excluded.

Subp. 81. Healing arts. "Healing arts" means health professions for diagnostic and/or healing treatment of human and animal maladies including but not limited to the following which are duly licensed by the state of Minnesota for the lawful practice of: medicine, dentistry, veterinary medicine, osteopathy, chiropractic, and podiatry.

30 Subp. 82. Healing arts screening or screening. "Healing 31 arts screening" or "screening" means the testing of individuals 32 using x-ray equipment to detect or evaluate health conditions 33 when the tests are not specifically and individually ordered by 34 a licensed practitioner of the healing arts who is legally 35 authorized to prescribe the tests for the purpose of diagnosis 36 or treatment.

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1 Subp. 14. [Renumber as Subp. 83.]

2 Subp. 84. Human use. "Human use" means the internal or 3 external administration of radiation or radioactive material to 4 an individual.

5 Subp. 85. Image intensifier. "Image intensifier" means a 6 device, installed in its housing, that instantaneously converts 7 an x-ray pattern into a corresponding light image of higher 8 energy density or higher luminance.

9 Subp. 86. Image receptor. "Image receptor" means a 10 device, such as a fluorescent screen or radiographic film, that 11 transforms incident x-ray photons either into a visible image or 12 into another form that can be made into a visible image by 13 further transformations.

14 Subp. 87. Image receptor support. "Image receptor support" 15 means, for mammographic systems, the part of the system designed 16 to support the image receptor during mammography.

Subp. 88. Individual. "Individual" means a human being.
Subp. 15. [Renumber as Subp. 89.]

19 Subp. 16. [Renumber as Subp. 90.]

20 Subp. 91. Inherent filtration. "Inherent filtration" 21 means the filtration of the useful beam provided by the 22 permanently installed components of the tube housing assembly. 23 Subp. 92. Inspection. "Inspection" means an official 24 examination or observation including but not limited to tests, 25 surveys, and monitoring to determine compliance with rules, regulations, orders, requirements, and conditions of the 26 27 commissioner.

Subp. 93. Interlock. "Interlock" means a device which automatically causes a reduction of the exposure rate upon entry by personnel into a high radiation area. Alternatively, an interlock may prevent entry into a high radiation area, or a device arranged or connected so the occurrence of an event or condition is required before a second event or condition can occur or continue to occur.

35 Subp. 94. Ionizing radiation. "Ionizing radiation" means 36 gamma rays, x-rays, alpha particles, beta particles, high speed

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electrons, neutrons, protons, and other nuclear particles,
 capable of producing ions directly or indirectly, by interaction
 with matter.

4 Subp. 95. Irradiation. "Irradiation" means the exposure 5 of matter to ionizing radiation.

6 Subp. 96. Isocenter. "Isocenter" means a fixed point in 7 space through which pass the central axes of radiation beams for 8 all possible beam orientations and field sizes.

9 Subp. 20. [Renumber as Subp. 97.]

10 Subp. 98. **Kilovolt peak (kVp).** "Kilovolt peak" or "(kVp)" 11 means the maximum value in kilovolts of the potential difference 12 of an x-ray generator. When only one half of the wave is used, 13 the value refers to the useful half of the cycle.

14 Subp. 99. Kilowatt second (kWs). "Kilowatt second" or 15 "(kWs)" means the equivalent of 10³ kV X mA X s.

16 Subp. 100. Lead equivalence or lead equivalent. "Lead 17 equivalence" or "lead equivalent" means the thickness of lead 18 affording the same attenuation, under specified conditions, as 19 the material in question.

Subp. 101. Leakage radiation. "Leakage radiation" means all radiation coming from within the source or tube housing except the useful beam. Leakage radiation includes the portion of the direct radiation not absorbed by the protective source or tube housing as well as the scattered radiation produced within the housing.

Subp. 102. Leakage technique factors. "Leakage technique factors" means the technique factors associated with the diagnostic or therapeutic source assembly that are used in measuring leakage radiation, as defined in items A to C.

A. For diagnostic source assemblies intended for capacitor energy storage equipment, the maximum-rated kVp and the maximum-rated number of exposures in an hour for operation at the maximum-rated kVp with the quantity of charge per exposure being ten millicoulombs, for example, ten milliampere seconds, or the minimum obtainable from the unit, whichever is larger.

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B. For diagnostic source assemblies intended for
 field emission equipment for pulsed operation, the maximum-rated
 kVp and the maximum-rated number of x-ray pulses in an hour for
 operation at the maximum-rated kVp.

5 C. For all other diagnostic or <u>x-ray tube</u> therapeutic 6 source assemblies, the maximum-rated kVp and the maximum-rated 7 continuous milliamperage for the maximum-rated kVp.

8 Subp. 103. Licensed practitioner of the healing arts. 9 "Licensed practitioner of the healing arts" means health 10 professionals for diagnostic or healing treatment of human and 11 animal maladies including but not limited to the following, 12 which are licensed by the state of Minnesota for the lawful 13 practice of medicine, dentistry, veterinary medicine, 14 osteopathy, chiropractic, and podiatry.

15 Subp. 104. Light field. "Light field" means the area of 16 the intersection of the light beam from the beam-limiting device 17 and one of the set of planes parallel to and including the plane 18 of the image receptor whose perimeter is the locus of points at 19 which the illumination is one-fourth of the maximum in the 20 intersection.

Subp. 105. Line-voltage regulation. "Line-voltage regulation" means the difference between the no-load and the load line potentials expressed as a percent of the load line potential. It is calculated using the following equation: Percent line-voltage regulation = 100 $(V_n - V_1)/V_1$

26 where:

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 V_n = no-load line potential; and

28 $V_1 = 1$ oad line potential.

Subp. 106. Linear attenuation coefficient or μ . "Linear attenuation coefficient" or " μ " means the quotient of dN/N divided by dl when dN/N is the fraction of uncharged ionizing radiation that experience interactions in traversing a distance dl in a specified material. The linear attenuation coefficient is the photon fraction attenuated per centimeter for small thicknesses of the attenuator.

36 Subp. 107. mA. "mA" means milliampere.

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Subp. 108. mAs. "mAs" means milliampere-second.
 Subp. 109. Maximum line current. "Maximum line current"
 means the root-mean-square current in the supply line of an
 x-ray system operating at its maximum rating.

5 Subp. 110. Medical particle accelerator. "Medical 6 particle accelerator" means a system capable of accelerating 7 electrons, protons, or other charged particles in a vacuum and 8 of discharging the resultant particulate or other radiation into 9 a medium at energies usually in excess of one MeV.

10 Subp. 111. Maximum permissible concentrations (MPC). 11 "Maximum permissible concentrations" or "(MPC)" means those 12 amounts listed as maximum permissible concentrations in Handbook 13 69, Maximum Permissible Body Burdens and Maximum Permissible 14 Concentrations of Radionuclides in Air and in Water for Occupational Exposure, U.S. Department of Commerce, National 15 16 Bureau of Standards (NBS), June 5, 1959, and in the Code of 17 Federal Regulations, title 10, part 20, appendix B. The NBS 18 report is incorporated by reference, may be viewed at the 19 Biomedical Library of the University of Minnesota, Minneapolis, 20 Minnesota, and is available through the Minitex interlibrary 21 loan system. This report is not subject to frequent change. Subp. 112. Maximum permissible dose or dose equivalent 22 (MPD). "Maximum permissible dose" or "dose equivalent (MPD)" 23 means, for radiation protection purposes, the maximum dose 24 equivalents that persons shall be allowed to receive in a stated 25 period of time (see parts 4730.0310 to 4730.0380). This excludes 26 patients receiving radiation for diagnostic or therapeutic 27 purposes under supervision of licensed practitioners of the 28 healing arts. 29

30 Subp. 26. [Renumber as Subp. 113.]

31 Subp. 114. NCRP. "NCRP" means the National Council on 32 Radiation Protection and Measurements. Specific NCRP reports 33 are incorporated by reference in this chapter. The reports may 34 be viewed at the Biomedical Library of the University of 35 Minnesota, Minneapolis, Minnesota, are available through the 36 Minitex interlibrary loan system, and are not subject to

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1 frequent change.

2 Subp. 115. NARM. "NARM" means a naturally occurring or 3 accelerator produced radioactive material. It does not include 4 by-product, source, or special nuclear material.

5 Subp. 116. Neutron generator. "Neutron generator" means a 6 type of accelerator in which the ion beam is used mainly for the 7 production of neutrons. Neutron generation is also possible for 8 high energy photon producing equipment.

9 Subp. 117. Nominal tomographic section thickness. 10 "Nominal tomographic section thickness" means the full width at 11 half-maximum at the center of the cross-sectional volume over 12 which x-ray transmission data are collected.

Subp. 118. Nonstochastic effects. "Nonstochastic effects" means effects for which the severity of the effect in affected individuals varies with the dose, and for which a threshold usually exists.

Subp. 119. Nominal treatment distance. "Nominal treatment distance" means:

A:--for-electron-irradiation;-the-virtual-source-to
 surface-distance-along-the-central-axis-of-the-useful-beam-as
 specified-by-the-manufacturer-for-the-applicator;-and

B.--for-x-ray-irradiation,-the-virtual-source-to
isocenter-distance-along-the-central-axis-of-the-useful
beam that distance at which the field size readouts are set.
For nonisocentric equipment, this distance shall-be-specified-by
the-manufacturer is usually the source-to-axis distance.

Subp. 120. Occupational dose. "Occupational dose" means exposure of an individual to radiation (1) in a restricted area; or (2) in the course of employment in which the individual's duties involve exposure to radiation; provided that occupational dose does not include exposure of an individual to radiation for the purpose of diagnosis or therapy of the individual.

33 Subp. 121. Optical density or O.D. "Optical density" or 34 "O.D." means the logarithm of the reciprocal-of-the-transmitted 35 <u>incident light intensity minus the logarithm of the transmitted</u> 36 light intensity.

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Subp. 122. Patient. "Patient" means an individual or
 animal subjected to healing arts examination, diagnosis, or
 treatment.

Subp. 123. Peak tube potential. "Peak tube potential"
means the maximum value of the potential difference across the
x-ray tube during an exposure.

Subp. 124. Permanent radiographic installation.
"Permanent radiographic installation" means an installation or
structure designed or intended for radiography and in which
radiography is regularly performed.

11 Subp. 28. [Renumber as Subp. 125.]

12 Subp. 126. Personnel monitoring equipment. "Personnel 13 monitoring equipment" means devices such as film badges, pocket 14 dosimeters, and thermoluminescent dosimeters designed to be worn 15 or carried by an individual for the purpose of estimating the 16 dose received by the individual.

17 Subp. 127. Phantom. "Phantom" means a volume of material 18 behaving in a manner similar to tissue with respect to the 19 attenuation and scattering of radiation.

Subp. 128. Phototimer. "Phototimer" means a method for controlling radiation exposures to image receptors by measuring the amount of radiation that reaches a radiation monitoring device. The radiation monitoring device is part of an electronic circuit that controls the duration of time the tube is activated. See automatic exposure control.

Subp. 30. [Renumber as Subp. 129.]

27 Subp. 130. Pixel. "Pixel" means an elemental area of a 28 digital image.

29 Subp. 131. Port film or portal imaging. "Port film" <u>or</u> 30 <u>"portal imaging"</u> means a diagnostic film <u>or electronic image</u> 31 taken with a therapeutic x-ray system to verify proper setup of 32 the treatment field.

33 Subp. 132. Position indicating device (PID). "Position 34 indicating device" or "(PID)" means a device on dental 35 radiographic x-ray equipment used to indicate the beam position 36 and to establish the source-to-skin distance.

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1 Subp. 133. Primary dose monitoring system. "Primary dose 2 monitoring system" means a system that will monitor the useful 3 beam during irradiation and will terminate irradiation when a 4 preselected number of dose monitor units have been acquired.

Subp. 134. Primary protective barrier. "Primary
protective barrier" means the material, excluding filters,
placed in the useful beam for protection purposes to reduce the
radiation exposure.

9 Subp. 33. [Renumber as Subp. 135.]

10 Subp. 136. Protective barrier or barrier. "Protective 11 barrier" or "barrier" means a barrier of radiation absorbing 12 material(s) used to reduce radiation exposure. Types of 13 protective barriers are primary protective barriers and 14 secondary protective barriers.

15 Subp. 35. [Renumber as Subp. 137.]

Subp. 138. Quality assurance program. "Quality assurance program" means the program and procedures contained in parts 4730.1655 to 4730.1695.

19 Subp. 139. Quality factor. "Quality factor" means a factor used for radiation protection purposes that accounts for 20 21 differences in biological effectiveness between different 22 radiations. The quality factors are: one for gamma rays, 23 x-rays, beta particles, and electrons; five for thermal neutrons; and 20 for neutrons other than thermal, protons, alpha 24 25 particles, and multiple-charged particles of unknown energy. 26 Subp. 140. Rad. "Rad" means the special unit of absorbed. dose. 27 One rad equals one one-hundredth of a joule per kilogram of any material. One millirad (mrad) equals 0.001 rad. 28 The SI equivalent is the gray. 29

30 Subp. 141. Radiation. "Radiation" means ionizing 31 radiation.

32 Subp. 142. Radiation area. "Radiation area" means an area 33 accessible to individuals in which there exists radiation at 34 such levels that a major portion of the body could receive in 35 one hour a dose equivalent in excess of five millirems (0.05 36 millisievert), or in five consecutive days a dose equivalent in

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08/01/91 [REVISOR] LMB/BD AR1543 l excess of 100 millirems (one millisievert). 2 Subp. 143. Radiation detector or detector. "Radiation 3 detector" or "detector" means a device that in the presence of radiation provides a signal or other indication suitable for use 4 5 in measuring one or more quantities of incident radiation. 6 Subp. 38. [Renumber as Subp. 144.] 7 Subp. 145. Radiation head. "Radiation head" means the 8 structure from which the useful beam emerges. 9 Subp. 39. [Renumber as Subp. 146.] 10 Subp. 40. [Renumber as Subp. 147.] 11 Subp. 42. [Renumber as Subp. 148.] 12 Subp. 149. Radiation safety officer. "Radiation safety 13 officer" means an individual who has the knowledge and responsibility to apply appropriate radiation protection 14 15 regulations, who has been designated by the facility in compliance with part 4730.0400, item B. 16 Subp. 150. Radiation therapy simulation system. 17 18 "Radiation therapy simulation system" means a radiographic or fluoroscopic x-ray system intended for localizing the volume to 19 20 be exposed during radiation therapy and confirming the position 21 and size of the therapeutic irradiation field. 22 Subp. 43. [Renumber as Subp. 151.] 23 Subp. 152. Radioactivity. "Radioactivity" means the 24 transformation of unstable atomic nuclei by the emission of ε. 25 radiation. Subp. 153. Radiograph. "Radiograph" means an image that 26 27 is created directly or indirectly by x-rays resulting in a permanent record or image. 28 29 Subp. 154. Radiography. "Radiography" means the process of making an image on a radiosensitive surface, such as a 30 photographic film, by radiation other than visible light, 31 especially by x-rays passed through an object or by 32 33 photographing a fluoroscopic image. Subp. 44. [Renumber as Subp. 155.] 34 35 Subp. 156. Rating. "Rating" means the operating limits as 36 specified by the component manufacturer.

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08/01/91 [REVISOR] LMB/BD AR1543 1 Subp. 157. Recording. "Recording" means producing a permanent form of an image resulting from x-ray photons. 2 Subp. 158. Reference plane. "Reference plane" means a 3 plane that is displaced from and parallel to the tomographic 4 5 plane. 6 Subp. 45. [Renumber as Subp. 159.] 7 Subp. 160. Registration. "Registration" means 8 registration with the commissioner according to parts 4730.0400 to 4730.0700. 9 Subp. 161. Rem. "Rem" means a special unit of dose 10 11 equivalence. One millirem (mrem) equals 0.001 rem. The SI equivalent is the sievert. For the purpose of this chapter, any 12 13 of the following is considered to be equal to one rem: 14 an exposure of one roentgen of x or gamma Α. radiation; 15 в. 16 an absorbed dose of one rad due to x, gamma, or 17 beta radiation; 18 C. an absorbed dose of 0.05 rad due to particles 19 heavier than protons and with sufficient energy to reach the lens of the eye; or 20 21 D. an absorbed dose of 0.1 rad due to neutrons or high energy protons. 22 23 Note: If it is more convenient to measure the neutron flux or equivalent than to determine the neutron absorbed dose in rads, 24 one rem of neutron radiation may, for purposes of this chapter, 25 26 be assumed to be equivalent to 14 million neutrons per square 27 centimeter incident upon the body; or, if there exists 28 sufficient information to estimate with reasonable accuracy the approximate distribution in energy of the neutrons, the incident 29 30 number of neutrons per square centimeter equivalent to one rem 31 may be estimated from the neutron flux dose equivalence table. 32 Neutron Flux Dose Equivalence 33 Number of neutrons per Average flux density to Neutron square centimeter for 34 energy deliver 100 millirems 35 a dose equivalent of 1 (one millisievert) in

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1	(MeV)	rem (10 millisieverts)	40 hours (neutrons/
2		(neutrons/cm ²)	cm ² per second)
3			
4	Thermal	970 x 10 ⁶	670
5	0.0001	720 x 10 ⁶	500
6	0.005	820 x 10 ⁶	570
7	0.02	400×10^{6}	280
8	0.1	120×10^{6}	80
9	0.5	43 x 10 ⁶	30
10	1.0	26×10^{6}	18
11	2.5	29×10^{6}	20
12	5.0	26 x 10 ⁶	18
13	7.5	24 x 10 ⁶	17
14	10.0	24 x 10 ⁶	17
15	10 to 30	14 x 10 ⁶	10

16 Subp. 162. Response time. "Response time" means the time 17 required for an instrument system to reach 90 percent of its 18 final reading when the radiation-sensitive volume of the 19 instrument system is exposed to a step change in radiation flux 20 from zero sufficient to provide a steady state midscale reading. 21 Subp. 47. [Renumber as Subp. 163.]

22 Subp. 48. [Renumber as Subp. 164.]

Subp. 165. Scan. "Scan" means the complete process of collecting x-ray transmission data for the production of a tomogram. Data can be collected simultaneously during a single scan for the production of one or more tomograms.

27 Subp. 166. Scan increment. "Scan increment" means the 28 amount of relative displacement of the patient with respect to 29 the CT system between successive scans measured along the 30 direction of the displacement.

31 Subp. 167. Scan sequence. "Scan sequence" means a 32 preselected set of two or more scans performed consecutively 33 under preselected CT conditions of operation.

34 Subp. 168. Scan time. "Scan time" means the time between 35 the beginning and end of x-ray transmission data accumulation

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1 for a single scan.

Subp. 169. Scattered radiation. "Scattered radiation" means radiation that, during passage through matter, has been deviated in direction and may have also been modified by a decrease in energy.

Subp. 170. Secondary dose monitoring system. "Secondary
dose monitoring system" means a system that will terminate
irradiation if the primary system fails.

9 Subp. 171. Secondary protective barrier. "Secondary 10 protective barrier" means a barrier sufficient to attenuate 11 stray radiation to the required degree.

12 Subp. 172. Secondary radiation. "Secondary radiation" 13 means radiation emitted by an irradiated material such as bone 14 or tissue and all inanimate objects.

Subp. 173. Sensitometer. "Sensitometer" means an instrument designed to produce a series of exposures with known ratios to each other.

Subp. 174. Shadow tray. "Shadow tray" means a device attached to the radiation head to support auxiliary beam limiting material.

Subp. 175. Shutter. "Shutter" means a device attached to the tube housing assembly that can totally intercept the useful beam and has a lead equivalency not less than that of the tube housing assembly.

Subp. 176. SI equivalent. "SI equivalent" means units
that conform to the international system of units.

Subp. 177. Sievert (Sv). "Sievert" or "(Sv)" means the unit of dose equivalent that is equal to one joule per kilogram. One rem is equal to 0.01 sievert or ten millisievert (mSv). Submultiples included in this chapter are the millisievert (mSv) and the microsievert (µSv).

32 Subp. 52. [Renumber as Subp. 178.]

33 Subp. 179. Source of radiation. "Source of radiation" 34 means a radioactive material, device, or equipment which emits, 35 or is capable of producing, radiation.

36 Subp. 180. Source-to-image distance (SID).

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"Source-to-image distance" or "SID" means the distance from the
 source to the center of the input surface of the image receptor.
 Subp. 181. Source-to-skin distance (SSD). "Source-to-skin
 distance" or "SSD" means the distance between the source and the
 skin of the patient.

6 Subp. 182. Spot check. "Spot check" means a procedure 7 that is performed to assure that a previous calibration 8 continues to be valid.

9 Subp. 183. Spot film. "Spot film" means a radiograph that 10 is made during a fluoroscopic examination.

Subp. 184. Spot-film device. "Spot-film device" means a 11 device intended to transport and/or position a radiographic 12 13 image receptor between the x-ray source and fluoroscopic image 14 receptor. It includes a device intended to hold a cassette over the input end of an image intensifier to make a radiograph. 15 Subp. 185. Stationary beam therapy. "Stationary beam 16 therapy" means radiation therapy without relative displacement 17 of the useful beam and the patient during irradiation. 18

Subp. 186. Stepless adjustment. "Stepless adjustment"
means a method of adjusting collimator blades continuously
rather than in fixed increments.

Subp. 187. Stochastic effects. "Stochastic effects" means effects, the probability of which, rather than their severity, is a function of radiation dose without threshold. More generally, stochastic means random in nature.

26 Subp. 53. [Renumber as Subp. 188.]

27 Subp. 189. Stray radiation. "Stray radiation" means the 28 sum of leakage radiation and scattered radiation.

29 Subp. 190. Survey or radiation safety survey. "Survey" or 30 "radiation safety survey" means an evaluation of the adequacy of radiation protection and assessment of the situation incident to 31 32 the production, use, release, disposal, or presence of sources of ionizing radiation under a specific set of conditions. When 33 34 appropriate, such evaluation includes a physical survey of the location of materials and equipment, and measurements of levels 35 36 of radiation or concentrations of radioactive material present

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1 in and around the facility.

2 Subp. 191. Target. "Target" means the part of a radiation 3 head that by design intercepts a beam of accelerated particles 4 with subsequent emission of other radiation.

5 Subp. 192. Technique factors. "Technique factors" means 6 the conditions of operation, specified as follows:

A. for capacitor energy storage equipment, peak tube
8 potential in kV and quantity of charge in mAs;

9 B. for field emission equipment rated for pulsed
10 operation, peak tube potential in kV and number of x-ray pulses;

11 C. for CT x-ray systems designed for pulsed 12 operation, peak tube potential in kV, scan time in seconds, and 13 either tube current in mA, x-ray pulse width in seconds, and the 14 number of x-ray pulses per scan, or the product of

15 milliamperage, x-ray pulse width, and the number of x-ray pulses
16 in mAs;

D. for CT x-ray systems not designed for pulsed operation, peak tube potential in kV, and either tube current in mA and scan time in seconds, or the product of milliamperage and exposure time in mAs and the scan time when the scan time and exposure time are equivalent;

22 E. for phototimed or automatic exposure controlled 23 equipment, all necessary indicators including anatomical, if 24 applicable, that must be activated before exposure; and

F. for all other equipment, peak tube potential in kV and either tube current in mA and exposure time in seconds, or the product of milliamperage and exposure time in mAs.

28 Subp. 56. [Renumber as Subp. 193.]

Subp. 194. Teratogenic effects. "Teratogenic effects" means effects occurring in offspring as a result of insults sustained in-utero.

32 Subp. 195. Termination of irradiation. "Termination of 33 irradiation" means the stopping of irradiation in a fashion that 34 will not permit continuance of irradiation without the resetting 35 of operating conditions at the control panel.

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Subp. 196. Therapeutic field size. "Therapeutic field

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size" means the dimensions along the major axes of an area in a

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plane perpendicular to the specified direction of the beam of 2 3 incident radiation at-the-normal-therapy-treatment-distance-and defined-by-the-intersection-of-the-major-axes-and-the-50-percent 4 isodose-line. The therapeutic field size is that distance 5 6 between the 50 percent of central axis values locations on the 7 beam profile measured at the depth of dose maximum. Material shall be placed in the beam so that dose maximum is produced at 8 the normal treatment distance when field size is being 9 determined. 10 11 Subp. 57. [Renumber as Subp. 197.] 12 Subp. 198. Tomogram. "Tomogram" means an x-ray image of a 13 thin section of the body. 14 Subp. 199. Tomographic plane. "Tomographic plane" means 15 the geometric plane that is identified as corresponding to the 16 output tomogram. 17 Subp. 200. Tomographic section. "Tomographic section" 18 means the volume of an object whose x-ray attenuation properties 19 are imaged in a tomogram. 20 Subp. 201. Traceable to a standard. "Traceable to a 21 standard" means a comparison, either directly or indirectly, to 22 a standard maintained by the National Institute of Standards and Technology (NIST) and that all comparisons have been documented. 23 24 Subp. 202. Tube housing assembly. "Tube housing assembly" means the tube housing with tube installed. 25 26 Subp. 203. Tube rating chart. "Tube rating chart" means the set of curves that specify the rated limits of operation of 27 the tube in terms of the technique factors. 28 29 Subp. 204. Type 1100 aluminum alloy. "Type 1100 aluminum alloy" means an alloy of aluminum that has a nominal chemical 30 composition of 99 percent minimum aluminum and 0.12 percent 31 32 copper. Subp. 205. Unit of exposure. "Unit of exposure" means the 33 34 roentgen in the conventional system of measurement or the coulomb per kilogram in the SI system of measurement. 35 Subp. 206. Unit of radioactivity. "Unit of radioactivity" 36 Approved 23 by Revisor _

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means the curie under the conventional system of measurement or
 the becquerel in the SI system of measurement.

3 Subp. 207. Units of radiation dose. "Units of radiation 4 dose" means the rad (unit of absorbed dose) and the rem 5 (radiation to body tissues in terms of its estimated biological 6 effect relative to an exposure of one roentgen of x-ray). Under 7 the SI measurement system the equivalent is the gray and the 8 sievert.

9 Subp. 208. Unrestricted area. "Unrestricted area" means 10 an area, the access to which is not controlled by the registrant 11 for purposes of protection of individuals from exposure to 12 radiation and radioactive material, and any area used for 13 residential quarters.

14 Subp. 209. Useful beam. "Useful beam" means radiation 15 that passes through the window, aperture, cone, or other 16 collimating device of the source housing by a direct path from 17 the x-ray tube or a radioactive source located in the radiation 18 source housing.

Subp. 210. Variable-aperture beam-limiting device.
"Variable-aperture beam-limiting device" means a beam-limiting
device that has a capacity for stepless adjustment of the x-ray
field size at a given SID.

Subp. 211. Virtual source. "Virtual source" means a point
from which radiation appears to originate.

25 Subp. 212. Visible area. "Visible area" means the portion 26 of the input surface of the image receptor over which incident 27 x-ray photons are producing a visible image.

Subp. 213. Wedge filter. "Wedge filter" means an added filter effecting continuous progressive attenuation on all or and part of the useful beam.

Subp. 214. X-ray control. "X-ray control" means a device that controls input power to the x-ray high-voltage generator and/or the x-ray tube. It includes components such as timers, phototimers, automatic brightness stabilizers, and similar devices that control the technique factors of an x-ray exposure. Subp. 215. X-ray equipment. "X-ray equipment" means an

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x-ray system, subsystem, or component. Types of x-ray equipment
 are listed in items A to C.

A. "Mobile x-ray equipment" means x-ray equipment 4 mounted in a self-contained transport vehicle.

B. "Portable x-ray equipment" means x-ray equipment
6 designed to be brought to the patient.

7 C. "Stationary x-ray equipment" means x-ray equipment 8 that is installed in a fixed location within a facility.

9 Subp. 216. X-ray field. "X-ray field" means the area of 10 the intersection of the useful beam and any one of the set of 11 planes parallel to and including the plane of the image 12 receptor, whose perimeter is the locus of points at which the exposure rate is one-fourth of the maximum in the intersection. 13 14 Subp. 217. X-ray generator. "X-ray generator" means a type of electron accelerator in which the electron beam is used 15 16 mainly for the production of x-rays.

17 Subp. 218. X-ray high-voltage generator. "X-ray 18 high-voltage generator" means a device that transforms 19 electrical energy from the potential supplied by the x-ray 20 control to the tube operating potential. The device may also 21 include means for transforming alternating current to direct 22 current filament transformers for the x-ray tube, high-voltage 23 switches, electrical protective devices, and other appropriate 24 elements.

25 Subp. 219. X-ray subsystem. "X-ray subsystem" means a 26 combination of two or more components of an x-ray system. 27 Subp. 220. X-ray system. "X-ray system" means an 28 assemblage of components for the controlled production of 29 x-rays. It includes minimally an x-ray high-voltage generator, 30 an x-ray control, a tube housing assembly, a beam-limiting device, and the necessary supporting structures. Additional 31 32 components that function with the system are considered integral 33 parts of the system.

34 Subp. 221. X-ray tube or tube. "X-ray tube" or "tube" 35 means an electron tube designed to be used primarily for the 36 production of x-rays.

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1 4730.0200 PURPOSE AND SCOPE.

2 Whereas, ionizing radiation can be instrumental in the improvement of health, welfare, and productivity of the public 3 4 if properly used, and may impair the health of the people and the industrial and agricultural potentials of the state if 5 improperly used, and the commissioner of health has the 6 7 statutory authority and duty to adopt, alter, and enforce 8 regulations for the preservation of the public health and 9 thereby to control sources of ionizing radiation and the 10 handling, storage, transportation, use, and disposal of 11 radioactive isotopes and fissionable materials within this 12 state, and to observe their effect upon human health, it is 13 hereby declared to be the purpose of the commissioner of health in this chapter to secure information concerning the nature and 14 15 extent of the employment of ionizing radiation equipment and radioactive materials within this state, and to control or 16 17 prevent dangers to health from ionizing radiation without 18 limiting or interfering with the constructive uses of ionizing 19 radiation consistent with a policy of reducing ionizing 20 radiation exposure to persons and the general public by all 21 practical means. The scope of this chapter does not include, 22 except for the provision of registration, those sources of 23 ionizing radiation known as by-product materials, source 24 materials, or special nuclear material.

25 4730.0300 PRECAUTIONARY PROCEDURES.

26 Subpart 1. Radiation symbol and labeling. Each radiation 27 sign or label shall bear the standard symbol specified in these 28 rules and the specified printed warning in capital block letters. The warning CAUTION RADIATION AREA or DANGER RADIATION 29 30 AREA shall appear on signs in an area in which a radiation hazard may exist. The warning CAUTION, RADIOACTIVE MATERIAL(S) 31 or DANGER, RADIOACTIVE MATERIAL(S) shall appear on containers 32 33 containing radioactive materials greater than the applicable 34 quantities listed in parts 4730.3500 and 4730.3605. The 35 standard symbol for designating any radiation hazard shall be a

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The boundaries of the three blades of the propeller-like 17 symbol shall be confined within a 60-degree sector of the circle 18 19 delineated by their outer edges, and said blades shall be symmetrically distributed 60 degrees apart. The radius (R) of 20 21 the central circle of the symbol shall be the standard for its 22 other dimensions as follows: Overall radius of symbol = 5R, 23 shortest distance from circumference of central circle to inner 24 edge of nearest blade = R/2. The standard color specifications 25 shall be a background of yellow with lettering and distinctive symbol in magenta or purple. The symbol and lettering shall be 26 as large as practical, consistent with the size of the equipment 27 or material upon which they appear. 28

29 [For text of subps 2 and 3, see M.R.]
30 Subp. 4. [See repealer.]

31 4730.0310 PERMISSIBLE DOSES, LEVELS, AND CONCENTRATIONS.

32 Subpart 1. Applicability. This part applies to all 33 registrants.

34 Subp. 2. Radiation dose standards for individual workers 35 in restricted areas. To determine the doses specified in item

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1 A, a dose from x-rays or gamma rays up to ten million electron 2 volts (MeV) may be assumed to be equivalent to the exposure 3 measured by a properly calibrated appropriate instrument in air 4 at or near the body surface in the region of the highest dose 5 rate.

A. According to part 4730.0340, and except as provided in item C, no registrant shall possess, use, receive, or transfer sources of radiation in such a manner as to cause any individual in a restricted area to receive in any period of one calendar quarter from all sources of radiation a total cocupational dose in excess of the standards specified in the following table:

13 Radiation limits per calendar quarter:

14 (1) Effective dose equivalent limit (stochastic 15 effects)... ±-±/4 1.25 rem (12.5 mSv);

16 (2) Dose equivalent limits for tissues and organs 17 (nonstochastic effects):

18 (a) Lens of eyes... 3-3/4 3.75 rem (37.5
19 mSv);

20 (b) All others (red bone marrow, breast, 21 lungs, gonads, skin, and extremities)... $\frac{12-\frac{1}{2}}{\frac{12.5}{2}}$ rem (125 22 mSv).

23 (3) Cumulative exposure... one rem X age in years
24 (ten mSv X age in years).

B. A registrant may permit an individual worker in a restricted area to receive a planned special occupational exposure to the whole body, including gonads, red bone marrow, breast, lungs, head and trunk, or lens of eye, provided:

(1) the individual worker receives an effective
dose equivalent (sum of external and internal effective dose
equivalent, if both exist) of no more than ten rems (100 mSv) in
a single planned event in a year;

(2) the effective dose equivalent received in all
 special planned exposures does not exceed 25 rems (250 mSv) over
 the individual's working lifetime;

(3) the registrant has determined the individual

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1 worker's accumulated occupational dose to the whole body and has otherwise complied with the requirements of this subpart; 2 (4) all planned special exposures are authorized 3 in writing by the registrant or the radiation safety officer 4 5 before exposure; 6 (5) individual workers who are without 7 procreative potential and have low lifetime effective dose 8 equivalents are selected whenever possible; and 9 (6) exposures resulting from planned special 10 exposures are included in the lifetime record of exposure for 11 each individual worker but are separately identified. No registrant shall possess, use, receive, or 12 c. 13 transfer sources of radiation in such a manner as to cause any 14 woman working in a restricted area to receive a total dose equivalent limit, excluding medical exposure, of 0.5 rem (five 15 16 mSv (θ -5-rem) to the woman's embryo and fetus. Once a pregnancy becomes known, exposure of the embryo and fetus shall be no 17 18 greater than θ -5-mSv 0.05 rem (θ - θ 5-rem 0.5 mSv) in any month, 19 excluding medical exposure. Special attention is required to 20 ensure that, if occupational exposures are received, they are 21 distributed uniformly with time so the embryo and fetus does not 22 receive more than its limit before pregnancy is known. 23 4730.0340 DETERMINATION OF ACCUMULATED OCCUPATIONAL DOSE. 24 Subpart 1. Disclosure before first entry into registrant's 25 restricted area. Before an individual starts work in the 26 registrant's restricted area where the individual will receive or is likely to receive in one calendar guarter an occupational 27 28 dose in excess of 25 percent of the applicable standards 29 specified in part 4730.0310, subpart 2, item A, subitem (1), the registrant must require that the individual disclose in a 30 written, signed statement, either: 31 32 A. that the individual had no prior occupational dose during the current calendar quarter; or 33 34 в. the nature and amount of any occupational dose 35 which the individual may have received during the specifically

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identified current calendar quarter, from sources of radiation
 possessed or controlled by another person.

The registrant must maintain records of the statements for the lifetime of the individual worker or a minimum of 20 years fafter termination of employment with the facility, whichever is less.

Subp. 2. Disclosure before entry into registrant's area exceeding occupational limits. Before allowing an individual worker to be exposed in a restricted area to limits in excess to those in part 4730.0310, subpart 2, item C, the registrant must:

A. calculate, using the information in subpart 1, item B, the accumulated dose to those individual workers who will be exposed to radiation in the registrant's restricted area; and

B. calculate the additional dose allowed for that
individual worker under part 4730.0310, subpart 2, item C.

17 Subp. 3. Preparation of accumulated dose records. Ιn 18 preparing accumulated dose records, the registrant must make a 19 reasonable effort to obtain reports of the individual's 20 previously accumulated occupational dose. For each period for 21 which the registrant obtains such reports, the dose shown in the 22 report must be used. In any case where a registrant is unable 23 to obtain reports of the individual's occupational dose for a 24 previous complete calendar quarter, it must be assumed that the individual worker has received the occupational dose specified 25 26 in whichever of the following columns that applies:

27 Column 1 Column 2 28 29 Part of Body Assumed dose in Assumed dose in rems 30 rems (mSv) for (mSv) for calendar 31 calendar quarters quarters beginning 32 before January 1, on or after 33 1961 January 1, 1961 34 Whole body, gonads 35 3-3/4 (37.5 mSv) 1-1/4 (12.5 mSv) active blood-36 37 forming organs, 38 head and trunk, 39 lens of eye 40The registrant must retain and preserve records used in 41 preparing the accumulated dose record for the lifetime of the 42 43 individual worker or a minimum of 20 years after the

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1 individual's termination of employment with the facility,
2 whichever is less. If calculation of the individual worker's
3 accumulated occupational dose for all periods before January 1,
4 1961, yields a result higher than the applicable accumulated
5 dose value for the individual as of that date, as specified in
6 part 4730.0310, subpart 2, item B, the excess may be disregarded.

7 4730.0360 EXPOSURE OF MINORS.

8 No registrant shall possess, use, or transfer sources of 9 radiation in such a manner as to cause any individual within a 10 restricted area who is under 18 years of age to receive any 11 occupational radiation dose except for training purposes. 12 Notwithstanding the limits in parts 4730.0310 and 4730.0380, the 13 occupational exposure-limit dose equivalent for training 14 purposes for a minor shall be no more than 0.1 rem (1.0 mSv) per 15 year.

16 4730.0380 PUBLIC PERMISSIBLE LEVELS OF RADIATION FROM EXTERNAL 17 SOURCES IN UNRESTRICTED AREAS.

18 No registrant shall possess, use, or transfer sources of 19 radiation in a manner that creates in any unrestricted area from 20 the sources of radiation in the registrant's possession:

21

A. radiation levels which:,

22 (±) if an individual were continuously present in 23 the area, could result in the individual receiving an annual 24 effective dose equivalent in excess of 0.1 rem (1.0 mSv) [sum of 25 external and internal exposures];-or

26 (2)-if-an-individual-were-periodically-present-in 27 the-area;-could-result-in-the-individual-receiving-an-annual 28 effective-dose-equivalent-in-excess-of-0.5-rem-(5.0-mSv)-[sum-of 29 external-and-internal-exposures]; and

B. radiation levels which, if an individual were present in the area, could result in the individual receiving an annual effective dose for the lens of the eye, skin, and extremities in excess of 5.0 rem (50 mSv) [sum of external and internal exposures].

1 4730.0400 REGISTRATION REQUIREMENTS. 2 The owner or person having possession of any source of 3 ionizing radiation except those specifically exempted under this 4 part or under part 4730.0800 or in the case of nuclear facilities which are registered according to the special 5 6 procedures required by part 4730.3000, shall: [For text of item A, see M.R.] 7 8 в. Designate an individual who will be responsible 9 for radiation protection from the source. The individual who is the radiation safety officer, shall: 10 11 (1) be qualified by training and experience concerning all hazards and precautions involved in operating or 12 13 in using the source for which the radiation safety officer is 14 responsible; 15 (2) establish a detailed program of radiation 16 safety for effective compliance with the applicable requirements 17 of this chapter; 18 (3) give instructions concerning hazards and 19 safety practices to individuals under the radiation safety 20 officer's supervision who may be exposed to radiation from the source; and 21 22 (4) make surveys and carry out other procedures as required by this chapter. 23 When, in the opinion of the commissioner of health, the 24 25 individual designated to be responsible for radiation safety does not have qualifications sufficient to ensure safe operation 26 or use of the source, the commissioner of health may require the 27 registrant to designate another individual who meets the 28 requirements of this item. 29 30 [For text of items C to E, see M.R.] 31 The registrant shall be subject to all applicable F. 32 requirements of this chapter. The registration requirements specified in parts 33 G. 4730.0400 to 4730.0700 shall not apply to facilities subject to 34 part 4730.3000, nor to sources or conditions exempted under part 35 36 4730.0800, nor to by-product materials, source materials, or

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special nuclear materials licensed by the United States Nuclear
 Regulatory Commission not in excess of the kind and quantity
 specified in parts 4730.3500 and 4730.3605.

4 4730.0500 RENEWAL OF REGISTRATION.

5 Subpart 1. Biennial renewal of registration. Each registration pursuant to this chapter shall be renewed 6 7 biennially according to the staggered schedule specified in subpart 2 so long as the activity requiring registration 8 9 continues. If there has been no substantial change in the 10 matters described in the last prior registration or renewal, the 11 renewal of the registration shall so state. If there has been 12 any accession of additional radiation sources or other 13 substantial change in the matters described in the preceding 14 registration or renewal, the renewal shall state the accession 15 or other change and give the information relating to the 16 accession or other change that would be required upon original registration. 17

18 Subp. 2. Staggered schedule for renewal of registration. 19 Each registration pursuant to this chapter shall be renewed on 20 or before the first day of the calendar quarter specified in 21 items A to H. The schedule is based on the registrant's 22 business address within the state.

23	[For	text	of	items	A	to I	H,	see l	M.R.]
24	[For	text	of	subps	3	and	4,	see	M.R.]

25 4730.0700 PERIODIC TESTING REQUIREMENTS.

26 Subpart 1. and 2. [See repealer.]

Subp. 3. Periodic testing requirements. Each owner, renter, or other person in possession of a source of radiation shall perform or cause to be performed such reasonable procedures as are necessary to assure radiation safety including, but not limited to, tests of:

32

A. sources of radiation;

B. facilities where sources of radiation are used orstored; and

35

C. radiation detectors, monitoring instruments, and

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08/01/91 [REVISOR] LMB/BD AR1543 1 other equipment and devices used in connection with use or storage of sources of radiation. 2 3 Results of such tests shall be available for submission to the commissioner of health when requested. 4 4730.0800 EXEMPTIONS. 5 6 This chapter shall not apply to the following sources or conditions: 7 8 [For text of items A to H, see M.R.] 4730.0900 VENDOR RESPONSIBILITY. 9 10 Subpart 1. Generally. No person shall make, sell, lease, 11 transfer, lend, or install x-ray or fluoroscopic imaging 12 assembly equipment or the supplies used in connection with such equipment unless the supplies and equipment, when properly 13 14 placed in operation and properly used, meet the requirements of 15 this chapter. This includes, but is not restricted to, 16 responsibility for the delivery of cones or collimators, 17 filters, adequate timers, and fluoroscopic shutters (where applicable). 18 [For text of subp 2, see M.R.] 19 4730.1110 REPORTS OF THEFT OR LOSS OF RADIATION SOURCES. 20 21 A registrant must report to the commissioner the theft or 22 loss of any radiation source immediately after the theft or loss The report must be made by telephone or 23 becomes known. 24 facsimile. After normal business hours or on weekends, this report must be made through the Minnesota Department of Public 25 Safety's duty officer. 26 4730.1120 REPORTS OF INCIDENTS INVOLVING RADIATION SOURCES. 27 28 Subpart 1. Immediate notification. During normal business hours a registrant must immediately notify the commissioner by 29 telephone or facsimile, and after normal business hours or on 30 weekends through the Minnesota Department of Public Safety's 31 duty officer, of any incident involving any source of radiation 32 possessed by the registrant which may have caused or threatens 33 34 to cause an unintended or unprescribed:

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dose to the whole body of any individual of 25 1 Α. rems (250 mSv) or more of radiation; 2 dose to the skin of the whole body of any 3 в. individual of 150 rems (1.50 Sv) or more of radiation; 4 dose to the feet, ankles, hands, or forearms of 5 C. any individual of 375 rems (3.75 Sv) or more of radiation; 6 release of radioactive material in concentrations 7 D. which, if averaged over a period of 24 hours, would exceed 5,000 8 times the limits specified for the material in part 4730.3605; 9 Ε. loss of one working week or more of the operation 10 of any facility affected; or 11 damage to property in excess of \$200,000. 12 F. Subp. 2. Notification within 24 hours. A registrant 13 possessing any source of radiation must notify the commissioner 14 by telephone or facsimile within 24 hours of any incident 15 involving that source which may have caused or threatens to 16 cause an unintended or unprescribed: 17 A. dose to the whole body of any individual of five 18 rems (50 mSv) or more of radiation; 19 dose to the skin of the whole body of any в. 20 21 individual of 30 rems (300 mSv) or more of radiation; 22 c. dose to the feet, ankles, hands, or forearms of any individual of 75 rems (750 mSv) or more of radiation; 23 D. release of radioactive material in concentrations 24 which, if averaged over a period of 24 hours, would exceed 500 25 times the limits specified for the material in part 4730.3605; 26 loss of one day or more of the operation of any E. 27 28 facility affected; or damage to property in excess of \$2,000. 29 F. 4730.1130 MANDATORY REPORTS OF OVEREXPOSURES AND EXCESSIVE 30 LEVELS AND CONCENTRATIONS. 31 Subpart 1. Additional reports. In addition to any 32 notification required by part 4730.1120, a registrant must 33 submit a written report within 30 days to the commissioner of: 34 each exposure of an individual to radiation in 35 Α.

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08/01/91 [REVISOR] LMB/BD AR1543 1 excess of the applicable standards in part 4730.0310, subpart 2, 2 or 4730.0360; B. any incident for which notification is required by 3 part 4730.1120; and 4 5 c. levels of radiation or concentrations of radioactive material, whether or not any individual is 6 excessively exposed, if in an unrestricted area and the exposure 7 is in excess of ten times any applicable limit specified by part 8 4730.0380 or 4730.3605. 9 10 Subp. 2. Reports on individuals. In the report required 11 under subpart 1 the registrant must describe the extent of 12 exposure of any individual to radiation or to radioactive material, including: 13 14 Α. estimates of each individual's exposure as 15 required by subpart 3; 16 в. the levels of radiation and concentrations of 17 radioactive material involved; 18 c. the cause of the exposure, levels, or 19 concentrations; and 20 D. corrective steps taken or planned to assure 21 against a recurrence. 22 Subp. 3. Report of individual dose. Any report filed with 23 the commissioner under this part must include, for each 24 individual exposed, the individual's name, date of birth, and an 25 estimate of the individual's dose. 4730.1140 NOTIFICATIONS AND REPORTS TO INDIVIDUAL WORKERS. 26 27 Report to individual worker. The registrant Subpart 1. 28 must report to an exposed individual worker the radiation 29 exposure data for that individual and the results of any measurements, analyses, and calculations of radioactive material 30 deposited or retained in the body of that individual worker. 31 The information reported must include the exposure data and 32 results obtained under this chapter, as shown in records 33 34 maintained by the registrant pursuant to part 4730.1520, subpart 4. Each notification and report must: 35

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A. be in writing;

B. include appropriate identifying data such as the name of the registrant or the name of the exposed individual worker; and

5 C. include the individual worker's exposure 6 information.

Subp. 2. Quarterly exposure report. A registrant must
advise each worker at least quarterly of the worker's exposure
to radiation or radioactive material as shown in records
maintained by the registrant under part 4730.1520, subpart 4.

Subp. 3. Report at end of employment. A registrant must 11 12 furnish to a worker who is terminating employment, or to a 13 worker who, while employed by another person, is terminating a 14 work assignment involving radiation dose in the registrant's 15 facility within a calendar quarter, a report of the worker's exposure to radiation or radioactive material. The report must 16 be furnished within 30 days from the time of termination of 17 employment or within 30 days after the exposure of the worker 18 19 has been determined by the registrant, whichever is later. The 20 report must cover each calendar quarter in which the worker's 21 activities involved exposure to radiation sources and must include the dates and locations of work under the registrant in 22 23 which the worker participated.

Subp. 4. Report to worker of exposure. When a registrant is required under part 4730.1130 to report to the commissioner any exposure of an individual to radiation, the registrant must also provide the worker with a report of the worker's exposure data. The reports must be transmitted at a time no later than the transmittal to the commissioner.

30 4730.1210 PROHIBITED USES OF RADIATION.

31 Subpart 1. General provision. No individual shall be 32 exposed to the useful beam except for healing arts purposes and 33 only if the exposure has been authorized by a licensed 34 practitioner of the healing arts. Any exposure of an individual 35 for the following other purposes is prohibited:

08/01/91 [REVISOR] LMB/BD AR1543 A. exposure for nonhealing arts training, 1 instruction, or demonstration, or other purposes; 2 3 в. exposure for the purpose of healing arts screening 4 except as authorized by part 4730.1310; exposure for healing arts training except as 5 с. specified in part 4730.0360; and 6 7 D. occupational or training exposure except as 8 specified in part 4730.0310. 9 Subp. 2. Prohibited radiation producing equipment and 10 procedures. The equipment specified in this subpart shall not 11 be used nor the specified procedures performed: 12 Α. fluoroscopic devices for fitting shoes; 13 в. photofluorographic equipment; 14 с. dental fluoroscopic imaging assemblies; 15 hand-held radiographic or fluoroscopic imaging D. 16 devices; 17 Ε. the use of fluoroscopy for positioning a patient 18 for general radiographic imaging, except for radiation therapy 19 simulators; 20 F. the use of fluoroscopy and c-arm fluoroscopes by a 21 person other than a licensed practitioner of the healing 22 arts when the licensed practitioner of the healing arts is not 23 physically present in the room; 24 G. the use of direct exposure x-ray film (without 25 intensifying screens) for all procedures other than intraoral 26 dental radiography, therapeutic portal imaging, and industrial 27 radiography; 28 nonimage intensified fluoroscopic x-ray equipment; н. 29 I. dental intraoral radiography with kilovoltages less than 50 kVp; and 30 J. 31 the use of x-ray equipment not specifically designed by the manufacturer for imaging of the breast. 32 Subp. 3. Unauthorized exposure of personnel monitoring 33 equipment. Exposure of personnel monitoring equipment to 34 deceptively indicate a dose delivered to an individual is 35 36 prohibited.

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1 4730.1310 HEALING ARTS SCREENING.

Subpart 1. General. Any person who desires to perform diagnostic x-ray screening in Minnesota must seek commissioner approval before x-ray screening may proceed. All applicants must meet the requirements specified in parts 4730.0100 to 4730.1950 and 4730.2150 to 4730.2250. In addition:

A. all applicants must be registered with the
8 commissioner before application for screening is initiated; and
9 B. the registrant must submit an application to the

9 B. the registrant must submit an application to the 10 commissioner requesting permission to perform diagnostic x-ray 11 screening.

Subp. 2. Content of application. In the application for screening the registrant must:

A. Provide his or her business name and address. If the registrant is a corporation or other business or nonbusiness association, the name of the person and phone number representing the association must be given.

B. Give the location of the proposed screening and the name and telephone number of a contact person at each location.

21 C. State the purpose of the proposed screening 22 program planned. The purpose must include a detailed statement 23 specifying the compelling health reasons, health benefits, and 24 health emergency, if any, that justifies the radiation exposure 25 to which any individual will be subjected by the proposed 26 screening.

D. Explain why alternate screening methods that do
not require the use of ionizing radiation are not being used.
E. Name all practitioners of the healing arts who
will interpret the radiographic images.

31 F. State the proposed interval for which permission 32 to perform screening is requested.

33 G. List the radiographic projections or views being 34 proposed in the screening program.

35 H. Specify the x-ray equipment to be used in

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1 connection with the proposed x-ray screening.

I. Describe the retention or disposition of the
images and other records pertaining to the screening x-ray
examinations after the screening project is completed.
J. Describe the population to be examined in the
screening program, including age, sex, and physical condition.

For mammography, the selection of the screening population must 7 meet the criteria specified by the Conference of Radiation 8 9 Control Program Directors, Inc. in "Mammography Screening 10 Guide," publication 87-4, February 1987, published in conjunction with the Food and Drug Administration's Center for 11 Devices and Radiological Health. This publication is 12 13 incorporated by reference, is not subject to frequent change, 14 and is available at the Minnesota Department of Health library, 15 Minneapolis, or through the Minitex interlibrary loan system.

16 K. Provide exposure measurements of the exposure at 17 skin entrance (ESE) and specific organ doses, for the type of 18 screening proposed. These exposures must be consistent with 19 those produced with state-of-the-art techniques. If no 20 guidelines are available for exposure measurements, the 21 commissioner may request peer review to establish such 22 guidelines.

L. Provide a written evaluation of the radiation safety survey and the quality assurance program as required by parts 4730.1655, 4730.1670, 4730.1675, 4730.1690, and 4730.1691. This must have been performed within three months prior to the application.

28 M. Any individual screened must be personally 29 informed by the registrant of the results, interpretation, or 30 findings. The screening application must:

(1) describe how this information will be
communicated to the individual who has been screened;
(2) describe where the results, interpretation,
or findings will be sent; and
(3) describe what arrangements will be made to

36 ensure that the individual who has been screened will be

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informed as to the need for further medical and health care
 evaluation or treatment.

3 Subp. 3. Additional information. The commissioner may 4 request the submission of additional information and data 5 subsequent to the submission of the original or renewal 6 application.

Subp. 4. Notification of commissioner's decision. The registrant shall be notified in writing of the commissioner's decision. If an application is granted, the notification shall specify the time, not to exceed one year, for which the application will be effective.

12 Subp. 5. Changes in screening program. The registrant is 13 responsible for informing the commissioner of any changes in the 14 screening program from that which was described in the content 15 of the application in subpart 2. The registrant must obtain 16 commissioner approval of the changes before the commencement of 17 the requested changes in the screening program.

18 Subp. 6. Denial of approval. The commissioner may deny or 19 revoke approval of any healing arts screening program if the 20 registrant fails to or refuses to comply with this chapter.

21 Subp. 7. Appeal procedure. The registrant may appeal the 22 denial, revocation, or refusal to approve an application or renewal application by requesting a contested case hearing under 23 the provisions of the Administration Procedure Act, Minnesota 24 Statutes, chapter 14. The registrant shall submit, within 15 25 26 days of the receipt of the department's decision, a written 27 request for a hearing. The request for a hearing shall set 28 forth in detail the reasons why the registrant contends the decision of the department should be reversed or modified. 29

30 Subp. 8. Renewal of screening application. Any request 31 for the renewal of a screening program application shall be 32 submitted in writing before its expiration date. Renewal 33 requests shall contain the information specified in subpart 2.

34 4730.1400 VIOLATIONS.

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Subpart 1. Prohibition of violation. If in the opinion of

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the commissioner it is necessary to protect any individual from 1 a radiation hazard, an injunction or other court order may be 2 3 obtained prohibiting any violation of any provision of any 4 regulation or order issued thereunder. Any person who willfully violates any provision of any regulation or order issued 5 thereunder may be guilty of a crime, and, upon conviction, may 6 be punished by fine or imprisonment or both, as provided by law. 7 8 Subp. 2. Commissioner approved healing arts screening. The commissioner may inspect the healing arts screening program 9 10 while in progress to assure that it is being carried out as described in the application in part 4730.1310 and in compliance 11 12 with this chapter.

[For text of subp 3, see M.R.] 13 14 Subp. 4. Withdrawal of approval for noncompliance with 15 application. Approval for healing arts screening may be withdrawn if, after an inspection, the commissioner finds 16 17 discrepancies between the screening program as implemented and as described in the application in part 4730.1310 or for 18 violation of this chapter. A hearing shall be held if requested 19 20 by the applicant within three days after the receipt of the 21 notice of withdrawal of approval. The hearing may be held upon granting the applicant three days' notice. If a hearing is 22 23 requested, withdrawal of approval shall not take effect until a 24 final order is issued by the commissioner.

25 4730.1450 OPPORTUNITY TO INSPECT.

Each registrant, owner, renter, or other person possessing a radiation source subject to registration or exempted under part 4730.0400 or 4730.0800 must allow the commissioner at all reasonable times and during the hours of operation to inspect adiation sources and the premises and facilities where these radiation sources are used or stored, and must make available to the commissioner records required by this chapter.

33 4730.1475 VARIANCES.

The commissioner shall grant a variance on the requirements of this chapter, except parts 4730.0400 and 4730.0600, only

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according to the criteria and procedures specified in parts
 4717.7000 to 4717.7050 as proposed at 15 State Register 985
 (October 29, 1990), and as later adopted.

4 4730.1510 REGISTRANT'S SAFETY REQUIREMENTS.

5 Subpart 1. Registrant responsibility. The registrant is 6 responsible for directing the operation of all x-ray systems 7 under the registrant's administrative control. The registrant 8 or the registrant's agent shall assure that the requirements 9 specified in this part are met in the operation of all x-ray 10 systems.

11 Subp. 2. X-ray system compliance. An x-ray system that 12 does not meet the provisions of this chapter shall not be operated for diagnostic, therapeutic, or industrial purposes. 13 14 Subp. 3. Individuals who may apply radiation. Only those individuals who are licensed practitioners of the healing arts, 15 16 or individuals who are qualified by training and experience and who are under the direct supervision of a licensed practitioner 17 of the healing arts, may intentionally apply radiation to an 18 19 individual.

Subp. 4. Procedure and safety instruction. All individuals who operate an x-ray system shall be initially instructed and annually retrained in safe operating procedures, emergency procedures for malfunctioning equipment, and quality assurance procedures. Written safety procedures shall be provided by the registrant to the individuals specified in subpart 3 including:

A. information on the effects of radiation exposure to thehuman body and the embryo-fetus;

29 в. projections where holding devices cannot be used; and 30 any restrictions of the operating technique required c. for the safe operation of the particular x-ray system. 31 Subp. 5. Radiographic technique chart. A radiographic 32 technique chart shall be provided in the vicinity of the 33 diagnostic x-ray system's control panel which specifies, for all 34 examinations performed with that system, the following 35

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08/01/91 [REVISOR] LMB/BD AR1543 1 information: 2 Α. the patient's anatomical size and corresponding technique factors to be used; 3 4 в. the type and-size of the screen-film combination, or direct exposure x-ray film for dental intraoral radiography, 5 6 to be used; 7 C. the type and focal distance of the grid to be used, if any; 8 9 the source-to-image distance to be used; and D. 10 E. the size, type, and proper placement of gonad shielding, if it can be used. 11 12 For computed tomography systems, a current technique chart for each routine examination, and the computed tomography 13 conditions of operation must be provided. 14 Subp. 6. Exposure of individuals other than the patient. 15 16 All diagnostic radiographic procedures and therapeutic x-ray procedures must meet the requirements of this subpart. 17 A. Except for the patient only the staff and 18 ancillary personnel required for the medical, dental, and 19 veterinary medicine procedure or training shall be in the room 20 during the radiographic exposure. 21 22 B. All staff and ancillary personnel required for assistance with the diagnostic radiographic procedures shall be 23 positioned so no part of the body, including the hands, will be 24 struck by the useful beam unless protected by 0.5 millimeter 25 lead equivalent material. 26 27 C. All staff and ancillary personnel who must remain in the room to assist during diagnostic radiographic and 28 computed tomography procedures must be protected from scattered 29 radiation by protective aprons or whole body protective barriers 30 of not less than 0.5 millimeter lead equivalence. 31 32 D. Patients and individuals who are not involved in diagnostic radiographic procedures using either stationary or 33 34 portable x-ray equipment, who cannot leave the room and who cannot be protected by adequate distance for the exam being 35

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performed must be protected from scattered radiation by

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protective aprons or whole body protective barriers of at least
 0.25 millimeters lead equivalence.

E. During any radiographic or fluoroscopic exposure, any door which is part of the protective barrier must be closed. F. No individual other than the patient shall be in a therapy treatment room during exposures from a therapeutic x-ray system operating above 50 kVp.

8 Subp. 7. Gonad protection. Except for cases in which it 9 would interfere with the diagnostic procedure, during 10 radiographic procedures in which the gonads are in or within two 11 inches (5cm) of the useful beam, gonad shielding of not less 12 than θ-25 <u>0.5</u> millimeter lead equivalence must be used for 13 patients who have procreative potential.

14 Subp. 8. Holding. When a patient, film cassette, or 15 intraoral film must be provided with auxiliary support during a 16 radiation exposure, items A to E apply.

A. Mechanical holding devices shall be used when the
technique permits. The-written-safety-procedures,-required-by
part-4730:1510,-subpart-4,-must-list-individual-projections
where-holding-devices-cannot-be-used.

B. Written safety procedures, as required by part 4730.1510, subpart 4, must indicate the requirements for selecting the individual holding and the procedure that individual shall follow.

C. The human holder must be protected as required by
part 4730.1510, subpart 6.

D. No individual shall be used routinely to hold intraoral film, film cassettes, or patients. In those cases where the patient must hold the film cassette or intraoral film, any portion of the body other than the area of clinical interest struck by the useful beam shall be protected by not less than 0.5 millimeter lead equivalent material.

E. If a patient must be held in position during therapeutic x-ray treatment, mechanical supporting or restraining devices shall be used.

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Subp. 9. Prevention of unauthorized use. Therapy x-ray

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systems shall not be left unattended unless they are secured
 against unauthorized use.

3 Subp. 10. Radiological practice standards. Procedures and 4 auxiliary equipment designed to minimize patient and personnel 5 exposure commensurate with the needed diagnostic information 6 shall be used.

A. The speed of screen-film combinations, or direct exposure x-ray film in intraoral dental radiography, shall be the fastest speed consistent with the diagnostic objective of the examinations.

B. Intensifying screens shall be used in combination with the compatible film, with the exception of dental intraoral films and radiation therapy port films.

14 C. The radiation exposure to the patient shall be the 15 minimum exposure required to produce images of good diagnostic 16 quality.

D. The darkroom for film development must be free of extraneous light so fog is not added to film during handling and processing.

20 E. Darkroom safelight filters must be compatible with21 the films being processed.

The darkroom for film development must be tested 22 F. 23 for film fog at least every three months; any time fog is 24 suspected; whenever there is a change in film speed or a change of safelight bulb or filters; or any time the integrity of any 25 seal around the processor, other equipment, or the darkroom may 26 27 have been compromised. The amount of fog (increase in optical density) for a two-minute fog test must not exceed 0.04 for 28 29 facilities doing mammographic film development and 0.08 for all other radiographic film development. 30

31 G. Portable x-ray equipment shall be used only for 32 examinations where it is impractical to transfer the patient to 33 a stationary x-ray system.

H. X-ray systems subject to part 4730.1850 shall not be used in procedures where the source-to-skin distance is less than 30 centimeters (11.8 inches).

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I. Protective aprons and gloves shall be monitored annually for lead protection integrity. A record of the monitoring shall be maintained until the next inspection by the commissioner.

5 Subp. 11. Personnel monitoring. Each registrant shall 6 supply the personnel specified in items A and B with personnel 7 monitoring equipment and shall require the personnel to use the 8 equipment.

9 A. Each individual who enters a restricted area under 10 such circumstances that the individual receives, or is likely to 11 receive, a dose in any calendar quarter over 25 percent of the 12 applicable value specified in part 4730.0310, subpart 2, item A, 13 subitem (1).

B. Each individual who enters a high radiation area.
Subp. 12. Placement of personnel monitoring equipment.
When protective clothing or-personnel-monitoring-equipment is
worn on portions of the body and personnel monitoring equipment
is required, at least one such piece of personnel monitoring
equipment shall be used, according to items A to C.

A. When a protective apron is worn, the personnel monitoring equipment shall be worn at the collar outside of the protective apron.

B. When more than one piece of personnel monitoring equipment is used and a record is made of the data, the record must identify the location of the monitor on the body and must state whether it was worn outside or under the protective clothing. The dose to the whole body based on the maximum dose attributed to the most critical organ shall be recorded in the reports required by part 4730.1520, subpart 4.

30 C. The control devices which accompany personnel 31 monitoring equipment during shipment to-the-registrant must be 32 kept in a nonradiation area at the facility between shipments of 33 personnel-monitoring-equipment.

34 Subp. 13. Facility design requirements. The registrant 35 must assure that the applicable structural shielding 36 requirements as specified in parts 4730.1610 to 4730.1630 are

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08/01/91 [REVISOR] LMB/BD AR1543 If an analysis of operating conditions indicates the 1 met. possibility of an individual receiving a dose over the limits in 2 part 4730.0310, the commissioner may require that structural 3 shielding modifications be made. 4 4730.1520 RECORDS TO BE MAINTAINED BY THE REGISTRANT. 5 6 Subpart 1. Individual x-ray systems. The registrant must maintain the following information for each x-ray system for 7 8 inspection by the commissioner. The maximum rating of the x-ray tube and generator. 9 Α. 10 в. The model manufacturer and serial numbers or other 11 permanent identification number of all-components the control 12 console and x-ray tubes. The-maximum-technique-factors-used-on-the-x-ray 13 с. 14 equipment. 15 D---The-type-of-examinations-or-treatments-which-will 16 be-performed-with-the-equipment-including-the-average-technique 17 factors-(kVp7-mA7-and-time-settings-or-mAs-settings)-E---Information-on-the-anticipated-workload-of-each 18 x-ray-system-in-number-of-examinations-or-treatments-per-week7 19 20 or-alternatively,-mA-minutes-per-week-of-examinations-or 21 treatments. 22 F. The half-value layer of the x-ray beam and the kVp at which the half-value layer was measured. 23 24 6. D. Records of radiation safety surveys, radiation 25 leakage measurements, calibrations, quality control measurements, maintenance, and equipment modifications performed 26 27 on the x-ray system with the names of individuals who performed the services. 28 29 H---A-floor-plan-of-the-room-in-which-a-stationary 30 therapeutic-or-diagnostic-x-ray-system-is-located. 31 (1)-The-scale-drawing-must-indicate-the-use-of 32 areas-adjacent-to-the-x-ray-room-and-an-estimate-of-their 33 occupancy-(2)-The-scale-drawing-must-include-the-normal 34 location-of-the-x-ray-system's-radiation-port,-the-port's-travel 35

and-traverse-limits,-all-directions-of-the-useful-beam,-the 1 2 location-of-any-windows-and-doors7-the-location-of-the operator's-booth7-the-location-of-the-x-ray-control-panel7-and 3 4 the-location-of-any-upright-cassette-holder. 5 (3)-The-scale-drawing-must-include-the-results-of 6 a-survey-for-radiation-levels-present-at-the-x-ray-system 7 operator's-position-and-at-pertinent-points-outside-the-room-at 8 specified-test-conditions-or-the-type-and-thickness-of 9 materials,-or-lead-equivalency,-of-each-protective-barrier. 10 (4)-The-plan-must-be-revised-when-necessary-to 11 reflect-any-change-in-the-room-or-system-which-may-affect 12 shielding-or-the-safety-of-individuals. 13 If-all-walls7-doors7-and-viewing-windows-in-a-diagnostic 14 exposure-room-are-shielded-with-a-minimum-of-1.6-millimeter-lead 15 or-lead-equivalent-material-(1/16th-inch-or-four-pounds-per 16 square-foot)-including-the-protective-barrier7-then-it-is-not 17 necessary-to-provide-the-information-required-in-this-item. 18 Subp. 2. Mammographic image retention. All original 19 baseline mammographic images must be maintained for seven years. If no additional mammographic images of the patient are 20 21 taken during this period, the original baseline images may be 22 discarded. 23 Subp. 3. Facilities. The registrant must maintain records

of personnel monitoring, radiation safety surveys, and quality control measurements for inspection by the commissioner.

A. Each registrant must maintain records of personnel monitoring required by subpart 4, and information required by parts 4730.1655 to 4730.1695 in the radiation measurement units used in this chapter.

B. Each registrant must maintain records in any of the following forms: the original, a computer file, a reproduced copy, or microfilm. A reproduced copy or microfilm must be duly authenticated by the registrant and must be clear and legible.

35 C. At all times, the registrant is responsible for 36 record retention required by this chapter. If the registrant

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ceases operation for any reason, provision must be made for
 record retention required by this chapter.

3 Subp. 4. Personnel monitoring records. Each registrant 4 shall maintain records showing the radiation exposures of all 5 individuals for whom personnel monitoring is required under part 6 4730.1510, subpart 11. The records must be clear and legible. 7 The doses entered on the records shall be for periods of time 8 not exceeding one calendar quarter or the period covered in the 9 personnel monitoring reports.

10 A. Records of individual exposure to radioactive 11 material as specified in part 4730.0340, subpart 1, and the 12 personnel monitoring records in this subpart shall be preserved 13 for the lifetime of the individual worker or a minimum of 20 14 years after termination of employment with the facility, 15 whichever is less.

B. In the absence of personnel monitoring data, records of the results of incident exposure surveys to determine external radiation dose shall be preserved indefinitely for the lifetime of the individual worker or for a minimum of 20 years after termination of employment with the facility, whichever is less.

C. A registrant must advise each worker at least quarterly of the worker's exposure to radiation or radioactive material as shown in records maintained by the registrant pursuant to this subpart.

D. The results of radiation safety surveys of medical particle accelerators and records of the results of surveys used to evaluate the release of radioactive effluents to the environment must be preserved until the next inspection by the commissioner.

31 4730.1530 ORDERING OF RADIOGRAPHIC EXAMINATIONS.

The registrant shall be responsible for assuring that the following requirements on ordering radiographic examinations are met except when the radiographic examination is part of a healing arts screening program approved by the commissioner.

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A. The request for a radiographic examination must be
 in writing and signed by a practitioner of the healing arts.
 B. The written request for a radiographic examination
 must include clearly stated clinical indications for the
 examination.

6 4730.1610 GENERAL SHIELDING REQUIREMENTS FOR MEDICAL,
7 CHIROPRACTIC, PODIATRIC, OSTEOPATHIC, AND VETERINARY MEDICINE
8 FACILITIES.

9 Subpart 1. Applicability. This part applies to all 10 medical, chiropractic, podiatric, osteopathic, and veterinary 11 medicine facilities.

12 Subp. 2. General shielding requirements for diagnostic radiographic facilities constructed or structurally remodeled 13 14 six months after the effective date of this chapter. For 15 diagnostic radiographic facilities constructed or structurally remodeled six months after the effective date of this chapter, 16 17 the requirements of this part apply. In addition, these facilities must meet the criteria for the particular type of 18 19 installation as presented in:

A. NCRP Report Number 36, "Radiation Protection in
 21 Veterinary Medicine" (1970);

B. NCRP Report Number 38, "Protection Against Neutron
Radiation" (1971);

C. NCRP Report Number 49, "Structural Shielding
Design and Evaluation for Medical Use of X-rays and Gamma Rays
of Energies Up to Ten MeV" (1976); and

D. NCRP Report Number 51, "Radiation Protection Design Guidelines for 0.1-100 MeV Particle Accelerator Facilities" (1977).

30 The NCRP reports in this subpart are incorporated by 31 reference, are not subject to frequent change, and are available 32 at the Biomedical Library of the University of Minnesota, 33 Minneapolis, Minnesota, or through the Minitex interlibrary loan 34 system.

35 Subp. 3. Requirements for lead or lead equivalent

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1 shielding for a diagnostic radiographic facility constructed or
2 structurally remodeled six months after the effective date of
3 this chapter. The requirements specified in this subpart apply
4 to a diagnostic radiographic facility constructed or
5 structurally remodeled six months after the effective date of
6 this chapter.

7 A. Sheet lead must be installed so it is supported to 8 prevent cold flow.

9 B. All lead lining must extend to a height of seven 10 feet (2.1 meters).

C. If the wall containing a door is shielded, the door must have the same lead equivalency as the adjoining walls.

D. All lead must be installed so that adjoining pieces of lead are overlapped by a minimum of one-half inch (1.3 centimeters). The shielding of the diagnostic radiographic room must be constructed so the protection is not impaired by joints; openings such as ducts and pipes passing through the barriers; or conduits or service boxes embedded in the barriers.

E. All protective barriers that attenuate the primary
x-ray beam must be shielded as primary protective barriers.
This includes, but is not limited to, areas of walls containing
chest cassette holders and upright buckys.

Subp. 4. Design requirements for a diagnostic radiographic facility. For a diagnostic radiographic facility constructed or structurally remodèled six months after the effective date of this chapter, the design requirements specified in subparts 5 to 8 apply.

Subp. 5. Space requirements for an operator's booth in a diagnostic radiographic facility. The requirements in items A to D are required for an operator's booth in a diagnostic radiographic facility.

A. The operator must be allotted not less than 7.5 square feet (0.7 square meters) of unobstructed floor space in the operator's booth.

35 B. The operator's booth may be any geometric 36 configuration provided no dimension is less than two feet (0.6

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1 meters). 2 Space allocated for the operator's booth must C. 3 exclude any space occupied by the x-ray control panel, including an overhang, cables, or other encroachments. 4 5 The booth must be located and constructed so the D. 6 unattenuated direct scattered radiation originating on the examination or treatment table, or at the upright cassette 7 8 position does not reach the operator's station in the booth and 9 does not exceed the exposure limits specified in part 4730.0310. 10 Subp. 6. Structural requirements for an operator's booth 11 in a diagnostic radiographic facility. The requirements in 12 items A to D apply to an operator's booth in a diagnostic 13 radiographic facility: 14 Α. The booth walls must be permanently fixed barriers 15 of at least seven feet (2.1 meters) high. 16 в. The booth must not be used as a primary barrier. 17 c. When a door or movable panel is used as an integral part of the booth structure, it must have an interlock 18 19 which prevents the exposure when the door or panel is not closed. 20 D. Shielding must be provided to meet the requirements of part 4730.0310. If a facility's workload does 21 not exceed 100 milliampere-minutes per week and all walls in the 22 23 diagnostic exposure room are shielded with a minimum of 1.6 24 millimeter lead (1/16th inch or four pounds per square foot) 25 including the protective barrier, then it is not necessary to 26 estimate the shielding requirements necessary to meet the requirements of part 4730.0310. 27 28 Subp. 7. X-ray control placement for an operator's booth 29 in a diagnostic radiographic facility. The x-ray control must be fixed within the booth so: 30 31 A. the exposure button is at least 39 inches (one 32 meter) from any open edge of the control booth wall which is nearest to the examining table; and 33 34 B. the operator is able to use the full viewing 35 window. Subp. 8. Viewing system requirements for an operator's 36

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08/01/91 [REVISOR] LMB/BD AR1543 1 booth in a diagnostic radiographic facility. An operator's booth in a diagnostic radiographic facility must meet the 2 requirements in items A and B. 3 4 Α. A booth must have at least one viewing device 5 which is placed so the operator: 6 (1) can view the patient during any exposure; 7 (2) has full view of any occupant of the room; and 8 9 (3) can view any entry into the room. 10 в. When the viewing system is a window, the 11 requirements in subitems (1) to (4) apply. 12 (1) The window must have the same lead equivalency as the surrounding barrier. 13 14 (2) The viewing area must be at least eight inches (20.32 cm) by ten inches (25.4 cm). 15 16 (3) The booth must be designed so the operator's 17 expected viewing position is at least 18 inches (0.46 meters) from the edge of the booth. 18 19 (4) In diagnostic radiographic facilities 20 constructed or structurally remodeled after the effective date 21 of this chapter, the minimum window size must be 18 24 inches 22 high (θ -46 0.61 meters) X 24 18 inches wide (θ -61 0.46 meters) and placed on a five foot two inch (1.57 meters) center 23 with the long dimension of the window in the vertical direction. 24 25 4730.1620 GENERAL SHIELDING REQUIREMENTS FOR DENTAL RADIOGRAPHIC FACILITIES. 26 27 Subpart 1. General requirements. The structural shielding 28 requirements in this subpart apply to all dental radiographic 29 facilities. 30 A. Dental rooms containing intraoral radiographic 31 systems must provide barriers at all areas struck by the useful beam. Shielding must meet the criteria in NCRP Report Number 32 33 35, "Dental X-Ray Protection," (1970). 34 B. When dental intraoral radiographic systems are 35 installed in adjacent rooms or areas, protective barriers must

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1 be provided between the rooms or areas. 2 C. Each installation must be provided with a protective barrier for the operator or must be arranged so the 3 4 operator can stand at least six feet from the patient and the 5 tubehead and not be in the path of the useful beam. Subp. 2. Requirements for new or structurally remodeled 6 7 facilities. Dental radiographic facilities constructed or structurally remodeled six months after the effective date of 8 this chapter must meet the shielding requirements in this part. 9 For an intraoral dental radiographic facility, the 10 Α. facility must meet the criteria in NCRP Report Number 35, 11 "Dental X-Ray Protection," (1970). 12 13 в. For a facility using dental radiographic equipment 14 for extraoral radiographs including but not limited to 15 cephalometric, temporomandibular joint and panoramic 16 radiographs, the general lead or lead equivalent shielding 17 requirements in part 4730.1610, subpart 2, apply. In addition, the facility must meet the criteria presented in NCRP Report 18 19 Number 49, "Structural Shielding Design and Evaluation for 20 Medical Use of X-rays and Gamma Rays of Energies up to Ten MeV" 21 (1976). 22 The NCRP reports specified in this part are incorporated by 23 reference, are not subject to frequent change, and are available 24 at the Biomedical Library of the University of Minnesota, 25 Minneapolis, Minnesota, or through Minitex interlibrary loan 26 system. 27 4730.1630 GENERAL REQUIREMENTS FOR THERAPEUTIC X-RAY FACILITIES. Subpart 1. Applicability. All therapeutic x-ray 28 29 facilities must meet the criteria for the particular type of 30 installation as presented in: A. NCRP Report Number 38, "Protection Against Neutron 31 Radiation" (1971); 32

B. NCRP Report Number 49, "Structural Shielding
Design and Evaluation for Medical Use of X rays and Gamma Rays
of Energies Up to Ten MeV" (1976);

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1 c. NCRP Report Number 51, "Radiation Protection 2 Design Guidelines for 0.1-100 MeV Particle Accelerator 3 Facilities" (1977); D. NCRP Report Number 69, "Dosimetry of X Ray and 4 5 Gamma Ray Beams for Radiation Therapy in the Energy Range Ten keV to 50 MeV (1981); 6 E. NCRP Report Number 72, "Radiation Protection and 7 Measurement for Low Voltage Neutron Generators" (1983); 8 9 F. NCRP Report Number 79, "Neutron Contamination from Medical Electron Accelerators (1984); and 10 11 G. NCRP Report Number 102, "Medical X-ray, Electron 12 Beam and Gamma Ray Protection for Energies Up To 50 MeV (Equipment Design, Performance and Use)" (1989). 13 The NCRP reports in items A to G are incorporated by 14 15 reference, are not subject to frequent change, and are available at the Biomedical Library of the University of Minnesota, 16 17 Minneapolis, Minnesota, or through the Minitex interlibrary loan 18 system. 19 Subp. 2. Shielding requirements for therapeutic x-ray 20 systems and medical particle accelerators. Each therapeutic 21 x-ray system and medical particle accelerator system installed in a facility must be provided with primary and secondary 22 23 barriers to assure compliance with parts 4730.0310, 4730.0340, 4730.0360, and 4730.0380. 24 25 Subp. 3. Facility design requirements for therapeutic 26 x-ray systems with energies of 50 kVp and above. Therapeutic x-ray systems with energies of 50 kVp and above: 27 28 must have two-way audio communication between the Α. patient and the operator at the control panel; and 29 30 B. must provide for patient observation; using: 31 (1) a closed curcuit television system; or 32 (2) for systems with energies of 150 kVp or less, E---must-have a window containing the appropriate lead 33 equivalence so the operator at the control panel may directly 34 observe the patient, any other individual in the room, and any 35

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doorways into the room; -and

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1 D:--may-have-a-closed-circuit-television-system-as-a
2 means-of-observing-the-patient.

3 Subp. 4. Additional requirements for therapeutic x-ray 4 systems with energies of 150 kVp and above, and medical particle accelerators. In addition to the requirements specified in 5 subpart 3, therapeutic x-ray systems with energies of 150 kVp 6 7 and above and medical particle accelerators must have protective 8 barriers which are fixed except for entrance doors or beam interceptors and the control panel must be located outside the 9 10 treatment room.

Subp. 5. Additional requirements for medical particle accelerators. In addition to the requirements specified in subparts 3 and 4, facilities with a medical particle accelerator must meet the standards in items A to D.

A. Closed-circuit television, or an equivalent system, must be provided to permit continuous observation of the patient during irradiation and must be located so the operator may observe the patient from the control panel.

B. Two-way audio communication between the patient and the operator must be provided at the control panel. However, where excessive noise levels or treatment requirements make audio communication impractical, other methods of communication must be used.

C. Treatment room entrances must be provided with warning lights in readily observable positions near the outside of all access doors to indicate when the useful beam is in the on position.

D. Interlocks must be provided so all entrance doors close before treatment is initiated or continued. If the useful radiation beam is interrupted by any door opening, it must not be possible to restore the system to operation without closing the door and reinitiating irradiation by manual action at the control panel.

34 4730.1655 REQUIRED QUALITY ASSURANCE PROGRAM PROCEDURES.
 35 Subpart 1. General. Within three months after the

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08/01/91 [REVISOR] LMB/BD AR1543 1 effective date of this chapter, each registrant must implement a quality assurance program which includes: 2 3 the quality assurance control measurements Α. specified in parts 4730.1655 and 4730.1665; 4 5 в. radiation safety surveys as specified in part 4730.1670; 6 C. calibrations as required in part 4730.1675; 7 8 D. in-service education for employees as specified in 9 parts 4730.1510, subpart 4, and 4730.1688; and 10 Ε. the records required in part 4730.1690. In addition to items A to E, each registrant with 11 12 therapeutic x-ray equipment must also make spot checks as specified in part 4730.1680. Medical particle accelerators must 13 have separate quality assurance control procedures as specified 14 in part 4730.1685. 15 16 Subp. 2. General quality assurance program procedures. 17 Each registrant conducting diagnostic radiographic procedures or therapeutic x-ray procedures must implement a quality assurance 18 19 program. The program must include: 20 a quality assurance manual that contains written Α. policies and procedures for radiation protection and describes 21 the quality assurance program; 22 the performance of quality assurance control tests 23 в. 24 and the correction of any deficiencies as specified in the quality assurance manual; and 25 C. the calibration record of any electronic equipment . 26 27 used in the quality assurance control tests within the preceding The calibration of any electronic equipment must be 28 two years. traceable to its calibration standard at the National Institute 29 30 of Standards and Technology (NIST). Subp. 3. Quality assurance control measurements for all 31 32 diagnostic x-ray facilities. Each registrant operating a diagnostic radiographic facility must implement the quality 33 assurance measures specified in items A to C. 34 The quality assurance manual described in subpart 35 Α. 36 2 must include the required tests and the minimum performance

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1 criteria specified in part 4730.1691 for the registrant's 2 diagnostic radiographic equipment and processing equipment. The 3 registrant is not limited to the quality assurance control tests 4 required in part 4730.1691 but may also include tests from item 5 C.

B. The manual must specify the minimum frequency of performance for the quality **assurance** <u>control</u> tests. In addition, the tests must be done after any change in the facility or equipment which might cause an increase in radiation hazard <u>or a change in equipment that results in the minimum</u> performance criteria not being met.

12 c. The registrant and the registrant's employees must 13 be familiar with the contents and recommendations of the NCRP report 99, "Quality Assurance for Diagnostic Imaging Equipment" 14 15 and may incorporate portions of the NCRP report 99 into the 16 facility's quality assurance manual described in subpart 2, item NCRP report 99, "Quality Assurance for Diagnostic Imaging 17 Α. 18 Equipment," (December 30, 1988) is-incorporated-by-reference,-is 19 not-subject-to-frequent-change, and is available at the Biomedical Library of the University of Minnesota, Minneapolis, 20 21 Minnesota, or through the Minitex interlibrary loan system.

4730.1665 COMPUTED TOMOGRAPHY QUALITY ASSURANCE CONTROL
MEASUREMENTS.

Subpart 1. Applicability. This part applies to computed tomography facilities and must be done in addition to the requirements in part 4730.1655.

Subp. 2. General quality assurance <u>control</u> measurements. The registrant must ensure that the quality <u>assurance control</u> measurements and calibration procedures specified in this part are performed. The quality <u>assurance control</u> measurements and calibration procedures must be in writing and include:

A. Those measurements and calibration procedures specified in part 4730.1691 for CT scanners at the frequency specified and those aspects of processing at the frequency specified. In addition, the quality **assurance** control

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1 measurements and calibration procedures must be done after any 2 change in the facility or equipment which might cause a 3 significant an increase in radiation hazard or a change in 4 equipment that results in the minimum performance criteria not 5 being met.

6 Β. The computed tomography dose index in the two 7 positions in item D, subitem (3)(b). The CT dosimetry phantom 8 must be oriented so that the measurement point of 1.0 centimeter beneath the surface is in the angular location where the 9 10 computed tomography dose index is maximum. For the purpose of 11 determining the computed tomography dose index, the manufacturer's statement as to the nominal tomographic section 12 thickness for that particular system may be used. 13

14 15 C.

D. Radiation output measurements.

The procedures specified in subpart 3, item A.

16 (1) Measurements of radiation output from a 17 computed tomography x-ray system must be performed as specified 18 in part 4730.1691 and after any change or replacement of 19 components which could cause a change in the radiation output.

(2) The measurement of the radiation output of the computed tomography x-ray system must be performed with a calibrated dosimetry system. The calibration of the dosimetry system must be traceable to its calibration standard at the National Institute of Standards and Technology (NIST). The dosimetry system must have been calibrated within the preceding two years.

(3) Computed tomography dosimetry phantoms must
be used in determining the radiation output of the computed
tomography x-ray system. The phantoms must comply with Code of
Federal Regulations, title 21, section 1020.33.

31 (a) All dose measurements must be performed 32 with the computed tomography dosimetry phantom placed on the 33 patient couch or support device without additional attenuation 34 materials present.

35 (b) Computed tomography dosimetry phantoms36 must provide a means for the placement of a dosimeter along the

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axis of rotation and along a line parallel to the axis of
 rotation 1.0 centimeter from the outer surface and within the
 phantom. Means for the placement of dosimeters or alignment
 devices at other locations may be provided.

5 (c) Any effects on the doses measured due to 6 the removal of phantom material to accommodate dosimeters must 7 be accounted for through appropriate corrections to the reported 8 data or included in the statement of maximum deviation for the 9 values obtained using the phantom.

10 (4) The dose measurements must be made for the 11 head and body technique used at the facility. The image quality 12 measurements must be made using a typical clinical technique in 13 the head and body scan modes of operation.

14 Subp. 3. Additional operator quality assurance <u>control</u> 15 measurements. In addition to the quality assurance <u>control</u> 16 measurements described in subpart 2, the quality assurance 17 <u>control</u> measurements specified in items A and B must be 18 performed by an operator.

A. The operator's computed tomography quality assurance <u>control</u> procedures must be those with the monthly or daily frequencies in part 4730.1691, and include all processing procedures noted in part 4730.1691.

23 в. The registrant or radiation safety officer must 24 review and initial all of the operator's quality assurance 25 control measurement's at least quarterly. An operator's quality assurance control measurements must include acquisition of 26 images obtained with the CT dosimetry phantoms using the same 27 processing mode and CT conditions of operation as are used to 28 29 perform the quality assurance control measurements required by subpart 2. 30

31 4730.1670 RADIATION SAFETY SURVEYS.

32 Subpart 1. Applicability. Each registrant conducting 33 diagnostic and or therapeutic x-ray procedures must ensure that 34 the radiation safety surveys specified in this part are 35 performed. Each registrant must make or have made the radiation

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l safety surveys necessary for establishing compliance with this 2 chapter. A survey must be performed at the time of initial installation and after any change in the facility or equipment 3 4 which might cause a change in radiation hazard. A report of 5 each survey must be prepared, maintained at the facility 6 according to the record requirements in part 4730.1520, and made 7 available to the commissioner on request. 8 Subp. 2. General Radiation safety-survey-requirements-for 9 all-diagnostic-radiography-systems monitoring equipment. Each 10 registrant-must-make-or-have-made-the-radiation-safety-surveys 11 necessary-for-establishing-compliance-with-these-regulations---A

12 survey-must-be-performed-at-the-time-of-initial-installation-and at-least-once-annually-after-that---In-addition,-a-survey-must 13 14 be-done-after-any-change-in-the-facility-or-system-which-might 15 cause-a-significant-increase-in-radiation-hazard---A-report-of 16 each-survey-must-be-prepared,-maintained-at-the-facility 17 according-to-the-record-requirements-in-part-4730-1520,-and-made 18 available-to-the-commissioner-upon-request At each medical 19 particle accelerator facility, portable monitoring equipment 20 designed for the types of radiation produced at the facility must be available. The portable monitoring equipment must be 21 22 operable and calibrated for the radiation being produced at the facility. The equipment must be tested for proper operation 23 prior to each use and calibrated at intervals not to exceed two 24 25 years and after each servicing or repair.

26 Subp. 3. Radiation-safety-survey-requirements-for-computed 27 tomography-systems Written procedures. The registrant must 28 ensure that all computed-tomography-systems-have-a radiation 29 safety surveys are performed at-the-time-of-initial installation-and-at-least-once-annually-after-that.--In 30 31 addition,-a-survey-must-be-done-after-any-change-in-the-system 32 or-equipment-which-might-cause-a-significant-increase-in radiation-hazard --- The-registrant-must-generate-a according to 33 34 written report-of-the procedures established by the radiation safety survey --- A-copy-of-the-report-must-be-maintained-at-the 35 36 facility officer and are in accordance with the-record

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requirements-in this part 4730-15207-and-shall-be-made-available 1 2 to-the-commissioner-on-request. 3 Subp--4---Radiation-safety-survey-requirements-for 4 therapeutic-x-ray-systems---All-therapeutic-x-ray-systems-must have-a-radiation-safety-survey-performed-at-the-time-of-initial 5 installation-and-at-least-once-annually-after-that---In 6 addition-a-radiation-safety-survey-must-be-done-after-any 7 change-in-the-facility-or-system-which-might-cause-a-significant 8 increase-in-radiation-hazard---The-registrant-must-generate-a 9 10 written-report-of-the-radiation-safety-survey---A-copy-of-the 11 report-must-be-maintained-at-the-facility-in-accordance-with-the 12 requirements-in-part-4730-15207-and-must-be-made-available-to 13 the-commissioner-on-request. 4730.1675 CALIBRATIONS. 14 Subpart 1. Diagnostic radiographic system calibrations. 15 16 The registrant must ensure that calibrations are performed on a diagnostic radiographic system whenever that system does not 17 meet the minimum performance criteria specified in part 18 19 4730.1691 and when there is any change or replacement of 20 components which could cause a change in the radiation output of 21 that system. 22 Subp. 2. Therapeutic x-ray system calibrations for systems of less than one MeV. Each registrant operating a therapeutic 23 24 x-ray system of less than one MeV must ensure that the 25 calibrations specified in this subpart are performed. A. The calibration of the radiation output of a 26 therapeutic x-ray system must be performed: 27 28 (1) at intervals not to exceed 12 months; 29 (2) after any change or replacement of components 30 which could cause a change in the radiation output; and 31 (3) with a calibrated dosimetry system. The calibration of the dosimeter must be traceable to its 32

33 calibration standard at the National Institute of Standards and 34 Technology (NIST). Verification of the dosimeter calibration 35 must be performed every two years.

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The calibration and beam characteristics of the 1 Β. 2 therapeutic x-ray system must include, but not be limited to: (1) the exposure rates dose rate as a function of 3 field size, technique factors, filter, and treatment distance 4 5 used; 6 (2) the degree of congruence between the 7 radiation field and the field indicated by the localizing device if the device is present; and 8 (3) an evaluation of the uniformity of the 9 largest radiation field used; 10 11 (4) verification of the applicability of the 12 inverse square law if needed for timer set calculations; 13 (5) verification of the accuracy of any 14 source-to-skin distance (SSD) indicators; (6) value of timer end effects; and 15 (7) verification of half value layer (HVL). 16 17 с. A copy of the current therapeutic x-ray system's dosimetry table data must be available in the area of the 18 19 control panel. 20 Subp. 3. Calibrations for therapeutic x-ray systems greater than one MeV MV. Each registrant operating a 21 therapeutic x-ray system of greater than one MeV \underline{MV} must ensure 22 that the calibrations specified in this subpart are performed. 23 A. The calibration of systems subject to part 24 25 4730.2450 must be performed according to the protocol endorsed by the American Association of Physicists in Medicine. 26 The protocol known as TG-21 is titled "A protocol for the 27 determination of absorbed dose from high energy photon and 28 electron beams" and is published in Medical Physics, volume 10, 29 number 6, pages 741 to 771, (1983). The TG-21 protocol is 30 incorporated by reference and is available at the Biomedical 31 Library of the University of Minnesota, Minneapolis, Minnesota, 32 or through the Minitex interlibrary loan system. This 33 publication is not subject to frequent change. This calibration 34 protocol must be performed: 35 (1) before the system is first used for the 36

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irradiation of a patient; 1 2 (2) at time intervals which do not exceed 12 3 months; and (3) after any change which might significantly 4 alter the calibration, spatial distribution, or other 5 characteristics of the therapy beam. 6 B. Calibration radiation measurements required by 7 item A must be performed using a dosimetry system traceable to 8 9 its calibration standard at the National Institute of Standards 10 and Technology (NIST). The dosimetry system must: 11 (1) have a calibration factor for cobalt-60 gamma 12 rays traceable to a standard maintained by the National 13 Institute of Standards and Technology (NIST); (2) have a calibration which has been verified 14 every two years by an Accredited Dosimetry Calibration 15 Laboratory (ADCL) or by intercomparison with another dosimetry 16 system that has been calibrated by an ADCL within two years; 17 18 (3) be calibrated after any servicing that may have affected its calibration; and 19 20 (4) be-calibrated-so-an-accuracy-can-be-stated for-the-radiation-quantities-monitored-by-the-system;-and 21 (5) have constancy checks as specified in part 22 4730.1695, subpart 1, item B. 23 C. Ealibration-of-radiation-beam-output-must-be 24 25 performed-at-a-reference-point-under-specified-conditions-in soft-tissue-that-may-be-calculated-to-within-an-accuracy-of-two 26 27 percent-The calibration documentation of the each therapy 28 Ð÷ 29 beam must include, but not be limited to, the following determinations: 30 (1) verification that the equipment is operating 31 in compliance with the design specifications for the light 32 localizer, side-light, and back-pointer all readouts, the 33 optical distance indicator, laser and cross-hairs alignment with 34 the isocenter, (when applicable), radiation isocenter variation 35 36 in-the-axis-of-rotation-for-the-table with collimator, gantry

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and table support rotation, and-jaw-system, and beam flatness, 1 2 and symmetry at the a specified depth; 3 (2) the absorbed dose rate at various depths of water-for-the-range-of-field-sizes-used7-for-each-effective 4 5 energy;-that-will-verify-the-accuracy-of-the-dosimetry-of-all therapy-procedures-used-with-that-therapy-beam the variation 6 7 with field size of the absorbed dose rate at a reference depth 8 in-phantom (or air) as a fraction of its value for the field 9 size used to determine the calibration as specified in part 4730.1675, subpart 3, item A; 10 11 (3) the uniformity of the radiation field and any 12 dependency on the direction of the useful beam; 13 (4) verification that existing depth-dose data 14 and isodose charts applicable to the specific system continue to be valid or are updated to existing system conditions; and 15 16 (5) verification of transmission for all 17 accessories such as wedges, shadow trays, and compensators. E. D. A copy of the latest-calibration-performed 18 under-item-A-shall most recent beam data must be available in 19 20 the area of the control panel. 4730.1680 THERAPEUTIC X-RAY SYSTEM SPOT CHECKS OF CALIBRATION. 21 22 Subpart 1. Spot checks of calibration for therapeutic x-ray systems of less than one MeV MV. The registrant must 23 24 ensure that spot checks of calibration are performed on 25 therapeutic x-ray systems capable-of-operation-at-greater-than 26 $\pm 5\theta - k \forall p$. Spot checks must be performed at a minimum frequency of every six months and meet the requirements specified in this 27 28 subpart. Spot-check procedures must be in writing, must be 29 Α. 30 maintained in the facility in accordance with part 4730.1520, 31 and must be available to the commissioner on request. Parameters exceeding the tolerance specified in 32 в. part 4730.1695 must be corrected to within the tolerance 33 specified before the system is used for patient irradiation. 34 C. Whenever a spot check indicates a change in the 35

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08/01/91 [REVISOR] LMB/BD AR1543 1 operating level of a system which exceeds the minimum tolerance 2 level specified in part 4730.1695, the system must be recalibrated as required in part 4730.1675, subpart 2. 3 4 D. Items to be spot checked include those calibrations and beam characteristics in part 4730.1675, subpart 5 6 2, items A and B. 7 Subp. 2. Spot checks of calibration for therapeutic x-ray systems greater than one Me∀ MV. The registrant must ensure 8 that spot checks of calibration are performed on systems subject 9 10 to part 4730.2450 during calibrations and at intervals not to 11 exceed one month. Spot checks must meet the requirements specified in items A to G: 12 13 Α. Spot-check procedures must be in writing. 14 The spot-check procedures must specify the в. 15 frequency at which tests or measurements are to be performed and 16 the acceptable tolerance for each parameter measured in the spot check when compared to the value for that parameter determined 17 in the calibration. 18 19 At intervals not to exceed one month, spot checks с. 20 must be made of absorbed dose measurements at a minimum of two depths in a phantom. 21 D. Where a system has built-in devices that provide a 22 measurement of any parameter during irradiation, the measurement 23 24 must not be used as a spot-check measurement. 25 E. A parameter exceeding a tolerance level specified 26 in part 4730.1695 must be corrected to within the tolerance level before the system is used for patient irradiation. 27 28 Whenever a spot check indicates a change in the F. tolerance level of a system which exceeds the minimum tolerance 29 30 level as specified in part 4730.1695, the system must be recalibrated as required in part 4730.1675, subpart 3. 31 G. Where a spot check involves a radiation 32 measurement, the measurement must be obtained using a dosimetry 33 system satisfying the requirements of part 4730.1675, subpart 3, 34 item B7-or-dosimetry-system-which-has-been-compared-with-a 35 dosimetry-system-meeting-those-requirements-within-the-previous 36

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l year.

2 4730.1685 MEDICAL PARTICLE ACCELERATOR QUALITY-ASSURANCE
3 RADIATION MONITORING EQUIPMENT.

4 Subpart-1---Radiation-monitoring-equipment. At each 5 medical particle accelerator facility, portable monitoring 6 equipment designed for the types of radiation produced at the 7 facility must be available. The portable monitoring equipment must be operable and calibrated for the radiation being produced 8 at the facility. The equipment must be tested for proper 9 10 operation prior to each use and calibrated at intervals not to 11 exceed one-year two years and after each servicing or repair.

Subp:-2:--Radiation-safety-survey:--The-registrant-must
ensure-that-a-radiation-safety-survey-is-performed-at-the-time
of-initial-installation;-at-least-annually-after-that;-and-when
changes-are-made-in-shielding;-operation;-equipment;-or
occupancy-of-areas-adjacent-to-the-facility:--A-report-of-each
survey-must-be-prepared;-maintained-at-the-facility-according-to
the-record-requirements-in-part-4730:1520;-and-made-available-to

19 the-commissioner-on-request:

Subp.-3.--Written-procedures.--The-registrant-must-ensure that-all-surveys-specified-in-this-part-are-performed-according to-written-procedures-established-by-the-radiation-safety officer-and-are-in-accordance-with-part-4730.1670.

24 4730.1688 IN-SERVICE EDUCATION IN QUALITY ASSURANCE.

Each registrant must provide the in-service training. program on quality assurance for employees specified in part 4730.1510, subpart 4. <u>Employees must sign or initial their</u> <u>attendance on a record to be kept for inspection by the</u> commissioner.

30 4730.1690 QUALITY ASSURANCE RECORDS.

31 Subpart 1. Diagnostic radiographic facility records. The 32 registrant must ensure that diagnostic radiographic equipment 33 records are maintained for each diagnostic imaging system, 34 including test results, requests for repairs and service,

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records of diagnostic radiographic equipment repairs and 1 service, and other information specified in part 4730.1520 until 2 3 the next inspection by the commissioner. 4 Subp. 2. Computed tomographic x-ray facility records. The 5 registrant must ensure that records of-computed-tomographic 6 x-ray-system-calibrations-performed-and-the-quality-control measurements-for-computed-tomographic-systems are recorded, 7 plotted, and maintained until the next inspection by the 8 9 commissioner. The records must indicate: 10 A. calibrations performed; 11 B. quality control measures for computed tomographic 12 systems; and C. requests for repair and service and the repairs 13 14 made. Subp. 3. Therapeutic x-ray facility records. 15 The 16 registrant must ensure that the following records are maintained 17 for therapeutic x-ray systems until the next inspection by the commissioner: 18 19 A. calibration records for therapeutic x-ray systems less than one MeV; 20 21 Β. calibration records of measurements for 22 therapeutic x-ray systems greater than one MeV as required under part 4730.1675, subpart 3, item A, and dosimetry system 23 24 calibrations as required by part 4730.1675, subpart 3, item B; spot-check measurements and any necessary 25 C. 26 corrective actions for therapeutic x-ray systems less than one MeV; and 27 28 spot-check measurements and any necessary D. corrective actions for therapeutic x-ray systems greater than 29 30 one MeV; and 31 E. requests for repair and service and the repairs 32 made. Subp. 4. Medical particle accelerator facility records. 33 The registrant must ensure that records of all radiation safety 34 surveys, calibrations, and instrumentation tests are maintained 35 for a medical particle accelerator at the facility until the 36

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08/01/91 [REVISOR] LMB/BD AR1543 next inspection by the commissioner. 1 4730.1691 MINIMUM DIAGNOSTIC QUALITY ASSURANCE CONTROL TESTS 2 FOR ALL-FACILITY ASSURANCE PROGRAM. 3 4 Subpart 1. Image receptors. 5 MINIMUM 6 TEST MINIMUM PERFORMANCE 7 TEST TYPE INTERVAL CRITERIA 8 9 Screen-film contact Α. Annually No significant areas of 10 poor contact 11 12 Screen-film-cassette Densities within в. Annually ± 0.10 O.D. for all cassettes used for each 13 speed match 14 15 diagnostic task 16 17 Subp. 2. Automatic processing. 18 MINIMUM 19 TEST MINIMUM PERFORMANCE TEST TYPE 20 INTERVAL CRITERIA 21 22 Darkroom fog < 0.08 O.D. increase in Α. Quarterly 23 density (measured at 24 approximately 1.00 O.D.) after 2 minutes using 25 26 preexposed film. For 27 mammography the O.D. 28 increase must be ≤ 0.04. 29 30 в. Sensitometry and Daily Density ± 0.15 O.D. 31 densitometry Before 32 processing 33 first film 34 of the day 35 36 с. Follow manufacturer's Temperature check Baily 37 At the recommendations. time of 38 sensitometry 39 40 41 Subp. 3. Manual processing. 42 **N** 1. MINIMUM 43 TEST MINIMUM PERFORMANCE 44 TEST TYPE INTERVAL CRITERIA . 45 46 Darkroom fog < 0.08 O.D. increase in Α. Quarterly density (measured at 47 48 approximately 1.00 O.D.) after 2 minutes using 49 50 preexposed film 51 Density ± 0.15 O.D. 52 в. Sensitometry and Daily 53 densitometry Before 54 processing first film 55 56 of the day 57 58 Temperature check Before Follow manufacturer's с. time and temperature 59 processing any-film chart 60 61 each batch of film 62 63

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All diagnostic radiographic tubes; required when Subp. 4.

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1 applicable. 2 MINIMUM 3 TEST MINIMUM PERFORMANCE 4 TEST TYPE INTERVAL CRITERIA 5 6 7 SID accuracy Α. Annually ± 2% of measured value 8 X-ray and light field alignment ± 2% of SID any one в. Annually 9 direction, 10 ± 3% of SID, both 11 directions (total) 12 13 X-ray and bucky ± 2% of SID с. Annually 14 alignment 15 16 D. Collimator dial Annually ± 2% of SID 17 accuracy 18 19 Ē. Reproducibility Annually ±-5%-of-the-average-of 20 a-set-of-exposures 21 Coefficient of 22 variation ≤ 5% 23 ± 10% of baseline (Baseline should be as 24 F. mR/mAs Annually 25 26 low as reasonably 27 achievable without 28 degrading image quality) 29 30 G. Linearity Annually ± 10% over clinical range 31 32 Ħ. Timer accuracy Annually Single Phase - Use 33 Table 4730.1692 Three 34 Phase - \pm 5% of setting 35 36 Half-value layer Annually Use part 4730.1750, I. 37 subpart 6, item A 38 39 J. kVp accuracy Annually ± 5% of indicated kVp 40 41 Κ. Phototimer reproduci-Annually ± 5% of average exposure bility, if present 42 43 Subp. 5. For facilities with fluoroscopes and C-arm 44 45 fluoroscopes, except radiation therapy simulators. 46 MINIMUM », · 47 MINIMUM PERFORMANCE TEST 48 TEST TYPE INTERVAL CRITERIA 49 < 5 R (1.3 mC kg⁻¹)
per minute for manual; Annually 50 Maximum output at Α. 51 tabletop or equivaand every tube change $\leq 10 \text{ R} (2.6 \text{ mC kg}^{-1})$ per minute for automatic 52 lent minimum SSD 53 brightness control systems 54 55 High level control maximum output at \leq 20 R (5.0 mC kg⁻¹) Annually 56 в. per minute 57 and every 58 tabletop or equivatube change 59 lent minimum SSD 60 Error between fluoro-61 с. Image size Annually graphic beam size and 62 63 observed image size must be no more than ± 3% of SID for all modes and at 64 65 any tower height 66 67 Annually Error between actual 68 D. Actual spot-film

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08/01/91 [REVISOR] LMB/BD AR1543 1 size vs indicated fluorographic beam size 2 at image receptor and 3 indicated image size must 4 5 be no more than ± 3% of SID for all modes and at 6 any tower height 7 8 Ε. Spot-film reproduci-Annually ± 5% of average exposure 9 bility 10 11 Phototimer reproduci-Annually ± 5% of average exposure F. bility, if present 12 13 14 Subp. 6. For facilities with mammography systems. 15 MINIMUM 16 TEST MINIMUM PERFORMANCE TEST TYPE 17 INTERVAL CRITERIA 18 19 Α. Same test types and 20 minimum performance 21 criteria as Diagnostic Radiographic Tubes as 22 23 specified in subpart 4, 24 unless listed below 25 26 kVp accuracy ± 1 kVp of indicated kVp в. Annually 27 Glandular dose (50% glandular and 50% 28 c. Annually < 400 millirads for Α. 29 a single view 30 adipose tissue screen film 4.5 cm 31 composition) compressed breast; 32 cranial caudal 33 view; or 34 35 B. \leq 100 millirads for a single screened 36 film without grid 37 38 Mammographic low and Quarterly D. No noticeable 39 high contrast deterioration 40 resolution (phantom in performance 41 image quality) 42 43 Phototimer reproduci-Ε. Annually ± 5% of average exposure 44 bility 45 Subp. 7. For facilities with tomography systems other than 46 47 computed tomography. 48 MINIMUM 49 TEST MINIMUM PERFORMANCE 50 TEST TYPE INTERVAL CRITERIA 51 52 53 Section level Α. Annually ± 5 mm 54 в. Level incrementation Annually ± 2 mm 55 56 с. Section thickness Follow manufacturer's Annually 57 specifications 58 59 Subp. 8. For facilities with computed tomography scanners. 60 MINIMUM MINIMUM PERFORMANCE 61 TEST TEST TYPE 62 INTERVAL CRITERIA 63 64 Α. Accuracy of scout Annually ± 1 mm localization view 65 66 в. Accuracy of dis-Annually ± 1 mm 67

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1		tance measurements						
2 3 4 5 6 7 8 9 0 1 1 2 3 4 5 6 7 8 9 0 1 1 2 3 4 5 6 7 8 9 0 1 2 3 4 5 6 7 8 9 0 1 2 2 1 2 1 2 1 2 1 2 1 2 1 2 1 2 1 2 1 2 1 2 1 1 2 1 1 2 1 1 2 1	c.	Patient dosimetry	Annually	± 20%				
	D.	CT number dependence on slice thickness	Semi- annually	Mean ± 3 CT numbers averaged over 100 pixels				
	E.	CT number calibration	Monthly	Air: -1,000 ± 3 <u>30</u> CT numbers; Water: 0 ± ± .5 5 CT numbers				
	F.	Low contrast resolution	Monthly	0.5 cm holes				
	G.	CT number uniformity	Monthly	Variation ± 5 CT numbers among a mean of 100 pixels				
	H.	Hard copy output and visual display	Daily	Luminance and contrast not significantly different				
22	Subp. 9. For facilities with cinefluorographic systems.							
23 24 25 27 29 31 33 35 37 39 41 23 44 44 44 44 44 44 44 44 44 44 44 44 44	TES	T TYPE	MINIMUM TEST INTERVAL	MINIMUM PERFORMANCE CRITERIA				
	Α.	Cinefluorographic exposure rates	Semi- annually	Approximately 10 to 20 uR (2.6 to 5.0 nC/kg) per frame at intensifier for nine inch (23 cm) mode; approximately 20 to 30 uR (5 to 8 nC/kg) per frame at intensifier for six inch (15 cm) mode				
	в.	Cinefluorographic film exposure	Semi- annually	Approximately 15 uR (4 nC kg ⁻¹) per frame at intensifier for nine inch (23 cm) mode; approximately 27 uR (7 nC kg ⁻¹) per frame at intensifier for six inch (15 cm) mode				
	C.	Cinefluorographic image size and beam limitation	Semi- annually	Within ± 3% of SID for all modes and at any tower height				
		Subp. 10. For facilities with cardiac catheterization						
50	syst	cems.	ì					
51 52 55 55 55 55 55 55 60 12 34 56 66 66 66 66 66 68	TEST	T TYPE	MINIMUM TEST INTERVAL	MINIMUM PERFORMANCE CRITERIA				
	Α.	Same test types and minimum performance criteria as Diagnostic Radiographic Tubes as specified in subpart 4, unless indicated in this subpart						
	Β.	Same test types and minimum performance criteria as fluoroscopes and C-arm fluoroscopes as specified in subpart 5, unless indicated	es					

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1 in this subpart 2 3 с. Film changer screen-Semi-No significant differ-4 film contact annually ence between static 5 and dynamic conditions 6 7 Low and high D. Semi-No significant differ-8 contrast resolution annually ence between static 9 and dynamic conditions 10 11 Optical density of Ε. Semi-< ± 0.2 O.D. difference films over duration 12 annually of filming run 13 14 15 F. Cinefluorographic 16 exposure rates (use 17 cinefluorographic 18 tests, minimum frequency 19 and minimum performance 20 criteria in subpart 9, item A) 21 22 23 Cinefluorographic low Semi-G. No degradation from 24 and high contrast annually fluoroscopic measurements 25 resolution 26 27 н. Ancillary special Follow Meet recommendations procedures of equipment 28 recommen-29 manufacturer equipment dations of 30 equipment 31 manufacturer 32 33 Subp. 11. For facilities with dental intraoral systems. 34 MINIMUM MINIMUM PERFORMANCE 35 TEST TEST TYPE CRITERIA 36 INTERVAL 37 38 Α. Film processing Use-automatic-and-manual-processing 39 as-specified-in-subparts-2-and-3-Before the first film Between 0.75 and 1.05 O.D. on the test 40 41 of the day tool or follow 42 43 manufacturer's recommendations 44 45 Use part 4730.1750, Filtration (HVL) 46 в. Annually subpart 6, item A 47 48 × . Use part 4730.1950, 49 Radiation exposure Annually с. subpart 4, item P D at end of cone 50 51 ±10% of indicated 52 D. Timer Annually reproducibility timer setting 53 54 55 Annually ±5% of indicated kVp E. kVp accuracy 56 Coefficient of 57 F. Reproducibility Annually 58 variation < 5% 59 Subp. 12. For facilities with dental extraoral systems 60 61 including panoramic systems. MINIMUM 62 MINIMUM PERFORMANCE 63 TEST CRITERIA TEST TYPE INTERVAL 64 65 Use automatic and manual processing 66 Film processing Α. as specified in subparts 2 and 3. 67

Same test types and 1 в. 2 minimum performance 3 criteria as Diagnostic Radiographic Tubes 4 5 in subpart 4. 6 7 Source: Derived from NCRP 99, Tables A.1 to A.10. 4730.1692 EXPOSURE TIME CONTROL LIMITS FOR SINGLE PHASE 8 FULL-WAVE RECTIFIED GENERATORS. 9 Exposure time (seconds) 10 Acceptance limits 11 12 1/524±1 dot 1/10 13 12±1 dot 1/20 14 6±0 dots 15 1/30 4±0 dots 16 17 Note: when using a spinning top, the x-ray pulses are imaged as 18 dots on the film as the small hole in the top is moved rapidly 19 (rotated) over the film. Source: National Council on Radiation 20 Protection, Report No. 99, Table 7.3, December 30, 1988. 4730.1693 THERAPY QUALITY ASSURANCE. 21 PARTIAL-LISTING-OF-MINIMUM-QUALITY-ASSURANCE CONTROL TESTS 22 23 AND LIMITS FOR MEASUREMENT EOUIPMENT 24 Subpart 1. Local standard (Loc. Std.). 25 MINIMUM TEST TEST INTERVAL* 26 TOLERANCE** 27 28 (1) AAPM - accredited Every two years D 29 Dosimetry Calibration 30 Laboratory calibration 31 32 (2) Linearity Every four years 0.5 percent 33 34 (3) Venting Every four years D 35 36 (4) Extra-cameral signal Initial use 0.5 percent 37 38 (5) Leakage Each use 0.5 percent 39 40 (6) Radionuclide-check Each-use 2-percent 41 42 (7) Recombination Initial use 0.5 percent 43 44(8) (7) Collecting potential Each use D 45 46 Subp. 2. Other field instruments. 47 MINIMUM TEST TEST INTERVAL* TOLERANCE** 48 49 (1) Local standard 50 Every year 2 percent 51 Comparison 52 53 (2) Linearity Every four years D 54 55 (3) Venting Every four years D 56 57 (4) Extra-cameral signal Every four years D

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1 2 (5) Leakage Each use 0.5 percent 3 4 (6) Radionuclide-check Each-use 2-percent 5 6 (7) Recombination Initial use 0.5 percent 7 8 (8) (7) Collecting potential Each use D 9 10 Subp. 3. Relative dosimetric equipment. 11 12 MINIMUM TEST 13 TEST INTERVAL* TOLERANCE** 14 15 (1) Thermoluminescent Dosimeter 16 (a) Calibration Each batch or box D (b) Linearity 17 Initial use D 18 (c) Electronic sensitivity Each use 3 percent 19 20 (2) Film 21 (a) Dose and response Each batch or box D (b) Densitometer linearity Every year 22 D 23 (c) Position sensitivity Initial Use D 24 25 (3) Air Ionization Chamber system (a) Linearity 26 Every year D (b) Extra-cameral signal Initial use 27 1 percent 28 29 (4) Diode System) Diode System (a) Energy dependence Initial use (b) Extra-cameral signal Initial use (c) Linearity Initial use 30 D 31 D 32 D 33 34 Subp. 4. Survey instruments. 35 MINIMUM TEST 36 TEST TOLERANCE** INTERVAL* 37 38 (1) Calibration Every year Every year D (2) Linearity 39 D 40 (3) Constancy Each use 5 percent 41 (4) Battery voltage Each use D (5)-Time-constant (6)-Radiofrequency 42 No-suggestion No-suggestion 43 No-suggestion Ð 44 interference 45 46 Subp. 5. Positioning equipment. 47 MINIMUM TEST 48 TEST INTERVAL* TOLERANCE** 49 (l) Accuracy (2) Hysteresis 50 Each use 2 mm 51 Each use 2 mm 52 53 Subp. 6. Phantoms and attenuators. 54 MINIMUM TEST 55 TEST INTERVAL* TOLERANCE** 56 (1) Thickness D 57 Initial use (2) Density(3) Phantom stacked Initial use 58 D 59 Initial use D 60 density (4) Integrity 61 Each use No suggestion (5) Detector fit 62 No-suggestion D Initial use 63 64 Subp. 7. Accessory equipment. 65

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MINIMUM TEST

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TEST 1 INTERVAL* TOLERANCE** 2 3 (1) Thermometer 4 (a) Calibration Initial use 0.5 percent 5 6 (2) Barometer (mercury) 7 (a) Calibration Hg Initial use 1 mm Hg 8 (3) Barometer (aneroid) (a) Calibration Hg 9 10 Initial use 1 mm Hg 11 (b) Intercomparison Annually 1 mm Hg 12 13 Initial use = Initial use for each mode of use or following malfunction and repairs. 14 15 16 Each use = Each use (measurement sequence) or ongoing 17 evaluation. 18 Each batch or box = Each batch or box at appropriate 19 energy (dosimeter element precision also should be considered). 20 21 22 23[°] y or mo = number preceding y = year or mo = 24 month indicates frequency between 25 tests, example: 4 y means once every 26 four years. 27 ** D = Documented and correction applied or noted 28 29 in report of measurement, when appropriate. 30 31 Source: Derived from American Association of Physicists in Medicine, Report No. 13, Table I, pp. 21-22, 1984. 32 33 4730.1695 QUALITY ASSURANCE-CRITERIA CONTROL TESTS FOR EXTERNAL 34 BEAM TELETHERAPY AND SIMULATION SYSTEMS. 35 Subpart 1. Dosimetry. 36 MINIMUM 37 TEST 38 INTERVAL TOLERANCE 39 General axis dose calibration Annually 40 Α. 2 percent 41 42 Β. Constancy checks (1) Dose per monitor unit 43 Weekly 3 percent 44 along central axis 45 (2) Depth dose Monthly 2 percent 46 (3) Beam uniformity Monthly 3 percent 47 (4) Dose monitor No suggestion No-suggestion 48 Annually 49 (5) Timer constancy No-suggestion No suggestion 50 Annually 51 52 Subp. 2. Geometry. 53 MINIMUM 54 TEST 55 INTERVAL TOLERANCE 56 57 Field positioning aids Α. 58 (1) Light field and radiation Weekly 3 mm 59 field agreement 60 (2) Mechanical distance pins, Monthly 2 mm lasers, and SSD lights 61 62 (3) Scale readouts Monthly No suggestion 63 Machine alignment 64 Β.

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1 2 3 4 5 6 7 8 9 10 11 12 13		<pre>(1) Focal-spot-position (2) Jaw symmetry (3) (2) Coincidence of</pre>	Annually Annually Annually Annually Annually ipment.	No-suggestion 2 mm 2 mm 2 mm No suggestion	
14			MINIMUM		
15 16 17 18 20 21 22 23 24 25 26 27 28 29 30 31 32			TEST INTERVAL	TOLERANCE	
	Α.	Dose calibration	Annually	3 percent	
	в.	Beam uniformity	Weekly	5 percent	
	с.	Depth dose	Monthly	3 mm at 80%	
	D.	X-ray contamination	Annually	No suggestion	
	E.	Dosimetry reproducibility and linearity	Annually	No suggestion	
	F.	Dose per monitor unit constancy check	Weekly	3 percent	
	Subp. 4. Treatment accessories. *				
33 34 35 36 37 38 39	А.	Wedges and standard	MINIMUM TEST INTERVAL Annually	TOLERANCE No suggestion	
		compensation			
38 39					
38 39 40 41	в.	Field shaping blocks	Annually	No suggestion	
38 39 40 41 42	в.	Field shaping blocks Subp. 5. Simulators.	Annually	No suggestion	
38 39 40 41 42 43 43	Β.	Field shaping blocks Subp. 5. Simulators.	Annually FREQUENCY	No suggestion TOLERANCE	
38 39 40 41 42 43 44 45 46 47	в. А.	Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2	Annually FREQUENCY -	No suggestion TOLERANCE -	
38 39 40 41 42 43 44 45 46 47 48 49	в. А. в.	Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories	Annually FREQUENCY - Annually	No suggestion TOLERANCE - No suggestion	
38 39 40 41 42 43 44 45 46 47 48 49 50	в. А. в.	Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off.	Annually FREQUENCY - Annually	No suggestion TOLERANCE - No suggestion	
38 39 40 41 42 43 44 46 47 49 50 51 52 53 53	в. А. В.	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off.</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL	No suggestion TOLERANCE - No suggestion TOLERANCE	
38 39 41 42 44 44 44 40 55 53 45 55 55 55 57	в. А. В.	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off.</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL No-suggestion Annually	No suggestion TOLERANCE - No suggestion TOLERANCE No suggestion	
38 39 41 42 44 44 44 44 5 55 34 55 55 55 55 55	в. А. В.	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off. Emergency off system * Attenuation in blocks, we</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL No-suggestion Annually edge factors, and	No suggestion TOLERANCE - No suggestion TOLERANCE No suggestion compensator	
339442 444567890 555555555555555555555555555555555555	B. A. B.	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off. Emergency off system * Attenuation in blocks, we must be checked annually.</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL No-suggestion Annually edge factors, and A visual inspection	No suggestion TOLERANCE - No suggestion TOLERANCE No suggestion compensator on of the	
339 442 44444 445 555555555555555555555555	B. A. B. A. data mech	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow subpart 2 Accessories Subp. 6. Emergency off. Emergency off system * Attenuation in blocks, we must be checked annually. A anical integrity of these accessories</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL No-suggestion Annually edge factors, and A visual inspection cessories must be	No suggestion TOLERANCE - No suggestion TOLERANCE No suggestion compensator on of the done monthly.	
3894412 444567890 553455678 50 60 61	B. A. B. A. data mech Sour	<pre>Field shaping blocks Subp. 5. Simulators. Geometry, follow Subpart 2 Accessories Subp. 6. Emergency off. Emergency off system * Attenuation in blocks, we must be checked annually. anical integrity of these access ce: Derived from American Asternation Amer</pre>	Annually FREQUENCY - Annually MINIMUM TEST INTERVAL No-suggestion Annually edge factors, and A visual inspection cessories must be ssociation of Phy	No suggestion TOLERANCE - No suggestion TOLERANCE No suggestion compensator on of the done monthly. sicists in	

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4730.1750 GENERAL EQUIPMENT REQUIREMENTS FOR ALL DIAGNOSTIC
 RADIOGRAPHIC SYSTEMS.

3 Subpart 1. Applicability. All diagnostic radiographic
4 systems must meet the requirements in this part.

5 Subp. 2. Warning label. The control panel containing the 6 main power switch must bear the warning statement which is 7 legible and accessible to view: "WARNING: This x-ray unit may 8 be dangerous to patient and operator unless safe exposure 9 factors and operating instructions are observed."

10 Subp. 3. Battery charge indicator. On battery-powered 11 x-ray generators, visual means must be provided on the control 12 panel to indicate whether the battery is adequately charged for 13 proper operation.

14 Subp. 4. Leakage radiation from the diagnostic source 15 assembly. The leakage radiation from the diagnostic source 16 assembly measured at a distance of one meter (39.4 inches) in 17 any direction from the source must not exceed 100 milliroentgens 18 (25.8 uC/kg) in one hour when the x-ray tube is operated at its 19 leakage technique factors. Compliance must be determined by 20 measurements averaged over an area of 100 square centimeters 21 (15.5 square inches) with no linear dimension greater than 20 22 centimeters (7.9 inches).

23 Subp. 5. Radiation from components other than the 24 diagnostic source assembly. The radiation emitted by a 25 component other than the diagnostic source assembly must not exceed two milliroentgens (0.516 uC/kg) in one hour at five 26 27 centimeters (1.97 inches) from any accessible surface of the 28 component when it is operated in an assembled x-ray system under 29 any conditions for which it was designed. Compliance must be 30 determined by measurements averaged over an area of 100 square 31 centimeters (15.5 square inches) with no linear dimension greater than 20 centimeters (7.9 inches). 32

33 Subp. 6. Beam quality, half-value layer. The half-value 34 layer of the useful beam for a given kVp must not be less than 35 the values shown in item A. If it is necessary to determine a

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1 half-value layer at a kVp which is not listed in item A, linear 2 interpolation or extrapolation may be made.

A. Values for half-value layer of useful beam for 4 x-ray tube:

5 6 7 8 9 10	Design operating range (kVp)	Measured kVp	Half-value layer (millimeter of aluminum) Other X-ray Systems	Specified Dental Systems
12 13 14 15	Below 50	30 40 50	0.3 0.4 0.5	1.5 1.5 1.5
16 17 18 19	51-70	51 60 70	1.2 1.3 1.5	1.5 1.5 1.5
20 21 22 23 24 25 26 27 28 29	Above 70	71 80 90 100 110 120 130 140 150	2.1 2.3 2.5 2.7 3.0 3.2 3.5 3.8 4.1	2.1 2.3 2.5 2.7 3.0 3.2 3.5 3.8 4.1

B. All intraoral dental radiographic systems
installed on and after December 1, 1980, must have a minimum
half-value layer not less than 1.5 millimeters aluminum.

C. For capacitor energy storage equipment, compliance with the requirements of this subpart must be determined with the capacitors fully charged and with a technique which discharges at least half of the energy stored in the capacitors (half of the maximum milliampere-second).

38 D. The half-value layer of the useful beam must be 39 measured with all the materials in the beam which are always 40 present between the source and the patient.

Subp. 7. Beam quality, filtration controls. For x-ray systems which have variable kVp and variable filtration for the useful beam, means must be provided to prevent an exposure unless the filtration required to obtain the half-value layer specified in subpart 6, item A, is in the useful beam for the given kVp which has been selected.

47 Subp. 8. Multiple tubes. Where two or more x-ray tubes 48 are controlled by one exposure switch, the tube or tubes which

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have been selected must be clearly indicated before initiation
 of the exposure. The indication must be both on the x-ray
 control panel and at or near the tube housing assembly which has
 been selected.

5 Subp. 9. Mechanical support of tube head. The tube 6 housing assembly supports must be adjusted so it remains stable 7 during an exposure unless tube housing movement is a designed 8 function of the x-ray system.

9 Subp. 10. Technique factors. The technique factors in 10 items A to C apply to all diagnostic radiographic systems.

11 A. The technique factors to be used during an 12 exposure must be indicated before an exposure begins. If 13 automatic exposure controls are used, the technique factors 14 which are set before exposure must be indicated.

B. If automatic exposure controls are used in a system installed after the effective date of this chapter, in addition to the requirements of item A:

(1) the exposure time or milliampere-second must be displayed for x-ray generators with a constant milliamperage; and

21 (2) the milliampere-second must be displayed for22 falling load generators.

C. The requirement of item A may be met by permanent markings on systems having fixed technique factors. Indication of technique factors must be visible from the operator's position except in the case of spot films made by the fluoroscopist.

Subp. 11. Timers. The requirements in this subpart for timers apply to all general radiographic, intraoral dental, and veterinary medicine radiographic systems.

A. A means must be provided to terminate the exposure at a preset time interval, a preset product of milliamperage and time, a preset number of pulses, or a preset radiation exposure to the image receptor.

35 B. An exposure must not be possible when the timer is 36 set to a zero or off position, if either position is provided.

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C. Except for dental panoramic systems, termination
 of the exposure must cause automatic resetting of the timer to
 its initial setting or to zero.

Subp. 12. Reproducibility. With a timer setting of 0.5 seconds or less, the difference between the maximum exposure time (T_{max}) and the minimum exposure time (T_{min}) must be less than or equal to 20 percent of the average exposure time (T) when four timer tests are performed:

9 $(T_{max} - T_{min}) \le 0.2 \text{ T}.$

10 Subp. 13. X-ray control. The x-ray control must meet the 11 requirements in this subpart.

A. The exposure control switch must be a dead-man
 type which requires continuous pressure to complete the exposure.
 B. Each x-ray control console other than dental

15 intraoral systems must be located in such a way as to meet the 16 requirements in this item.

(1) Stationary x-ray systems must have the x-ray control permanently mounted behind the protective barrier so the operator remains behind that barrier during the entire exposure. (2) Portable x-ray systems that produce more than

21 25 milliamperes-minutes per week at the same location must meet 22 the requirement of subitem (1).

(3) Portable x-ray systems that produce less than
24 25 milliamperes-minutes per week at the same location, must meet
25 the requirement of subitem (1), or be provided with a 6.5 foot
26 (2.0 m) high protective barrier which is placed at least six
27 feet (1.8 m) from the tube housing assembly and at least six
28 feet (1.8 m) from the patient.

29 C. The x-ray control console must provide visual 30 indication observable at or from the operator's protected 31 position whenever x-rays are produced.

Subp. 14. Exposure reproducibility. The coefficient of variation must not exceed $\theta \rightarrow \theta = 0.05$ when all technique factors are held constant. This-requirement-shall-be-met-if,-when-four exposures-are-made,-the-difference-between-the-maximum-exposure (E_{max})-and-the-minimum-exposure-(E_{min})-is-less-than-or-equal-to

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20-percent-of-the-average-exposure-(E).

*†E*max---Emin)<u><</u>0.2-E.

3 Subp. 15. Additional requirements applicable only to 4 certified x-ray systems. Only diagnostic radiographic systems 5 incorporating one or more certified components must comply with 6 the requirements in this subpart which relate to those certified 7 components.

8 A. The radiographic system must be operated on an 9 adequate power supply as specified by the manufacturer. The 10 coefficient of variation of radiation exposures must be no 11 greater than 0.05 for any specific combination of selected 12 technique factors.

13 в. When the radiographic system allows a choice of 14 x-ray milliamperage settings and is operated on a power supply 15 as specified by the manufacturer according to the requirements of applicable federal performance standards for any fixed kVp 16 within the range of 40 to 100 percent of the maximum rating, the 17 average ratios of exposure to the milliampere-seconds product 18 obtained at any two consecutive milliamperage settings must not 19 differ by more than 0.10 times their sum: 20

21 $+\overline{x}_1 - -\overline{x}_2 + (\overline{x}_1 - \overline{x}_2) \leq 0.10 (\overline{x}_1 + \overline{x}_2),$

22 where \overline{X}_1 and \overline{X}_2 are the average mR/mAs values obtained at each 23 of two consecutive milliamperage settings.

C. Deviation of technique factors from indicated
values must not exceed the limits specified for that system by
its manufacturer.

27 D. The x-ray control console must provide a signal 28 audible to the operator that the exposure has terminated.

29 E. A certified diagnostic radiographic system and its 30 associated certified components used on humans must be 31 maintained in compliance with applicable requirements of the 32 Federal X-ray Equipment Performance Standard, Code of Federal 33 Regulations, title 21, subchapter J, in effect at the time of 34 manufacture.

35 4730.1850 DIAGNOSTIC RADIOGRAPHIC SYSTEMS OTHER THAN

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FLUOROSCOPIC, DENTAL INTRAORAL, VETERINARY MEDICINE, OR COMPUTED
 TOMOGRAPHY SYSTEMS.

3 Subpart 1. Applicability. This part applies to all diagnostic x-ray systems certified according to standards 4 provided by United States Code, title 42, section 263f, and to 5 6 diagnostic x-ray systems installed before those standards were 7 established. This part does not apply to fluoroscopic, dental 8 intraoral, veterinary medicine, or computed tomography x-ray 9 systems. The requirements in this part are in addition to the 10 requirements in parts 4730.0100 to 4730.1750.

Subp. 2. Beam limitation. The useful beam must be limited to the patient's area of clinical interest.

Subp. 3. General purpose stationary x-ray systems.
General purpose stationary x-ray systems must meet the standards
in items A to E.

16 A. A means for stepless adjustment of the size of the 17 x-ray field must be provided.

18 A method must be provided for visually defining в. 19 the perimeter of the x-ray field. The total misalignment of the edges of the visually defined field with the respective edges of 20 21 the x-ray field along either the length or width of the visually 22 defined field must not exceed two percent of the distance from the source to the center of the visually defined field when the 23 24 surface upon which it appears is perpendicular to the axis of the x-ray beam. 25

26

C. A method must be provided to:

(1) indicate when the axis of the x-ray beam isperpendicular to the plane of the image receptor;

(2) align the center of the x-ray field with
respect to the center of the image receptor to within two
percent of the SID; and

32 (3) indicate the SID to within two percent.
33 D. The beam-limiting device must numerically indicate
34 the field size at the plane of the image receptor to which it is
35 adjusted.

36

E. The indication of field size dimensions and SIDs

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1 must be:

(1) specified in inches or centimeters; and
(2) such that aperture adjustments result in
x-ray field dimensions at the plane of the image receptor which
correspond to those indicated by the beam-limiting device to
within two percent or less of the SID when the beam axis is
perpendicular to the plane of the image receptor.

8 Subp. 4. Diagnostic radiographic systems designed for one 9 image receptor size. Diagnostic radiographic systems designed 10 for only one image receptor size at a fixed SID must be provided 11 with means to limit the field at the plane of the image receptor to dimensions no greater than those of the image receptor, and 12 13 must align the center of the x-ray field with the center of the image receptor to within two percent of the SID. Alternatively, 14 15 such systems must be provided with means to both size and align the x-ray field so the x-ray field at the plane of the image 16 17 receptor does not extend beyond any edge of the image receptor.

18 Subp. 5. Diagnostic radiographic systems designed only for 19 mammography. Diagnostic radiographic systems designed only for 20 mammography must be provided with means to limit the useful beam 21 so the x-ray field at the plane of the image receptor does not 22 extend beyond any edge of the image receptor at any designated 23 SID. For the edge of an image receptor designed to be adjacent to the chest wall, the x-ray field must not extend beyond this 24 25 edge by more than two percent of the SID. This requirement can be met with a system which performs according to subpart 6, item 26 27 C. When the beam-limiting device and image receptor support device are designed to be used to compress the breast during a 28 mammographic procedure and the SID may vary, the SID indication 29 specified in subpart 6, item C, must be the maximum SID for 30 31 which the beam-limiting device or aperture is designed. 32 addition, each image receptor support intended for installation on a system designed only for mammography must have clear and 33 34 permanent markings to indicate the image receptor size for which it is designed. 35

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Facilities providing mammography must comply with the

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1 standards in items A to G. 2 Α. Radiographic equipment used for either screen-film 3 or xeroradiographic imaging of the breast must be designed specifically for mammographic imaging. 4 5 в. The x-ray tube target material must be molybdenum or tungsten-molybdenum alloy for screen-film systems, or 6 7 tungsten for xeroradiographic systems. 8 C. The half-value layer must be a minimum of 0.3 mm 9 of aluminum at 30 kVp for screen-film systems. The half-value 10 layer must be a minimum of 1.5 mm of aluminum at 45 kVp for 11 xeroradiographic systems. 12 The kilovoltage must be less than 34 kVp for D. 13 screen-film systems and between 40 to 55 kVp for 14 xeroradiographic systems for a 4.5 cm thick compressed breast, 15 comprised of 50 percent glandular, 50 percent adipose tissue. E. A screen-film system designed for mammographic 16 17 purposes must be used for screen-film imaging. Direct x-ray 18 exposed film or any other film exposed directly to x-rays must 19 not be used. 20 F. The mean glandular dose for a two view screen-film 21 mammography with grid or for a two view xeroradiography for a 22 patient with 4.5 cm thick compressed breasts breast must be no 23 more than 0.8 rad. The mean glandular dose for a two view screen-film 24 G. 25 mammography without grid, for the patient with 4.5 cm thick 26 compressed breasts breast must be no more than 0.2 rad. 27 Subp. 6. Other noncertified general purpose x-ray systems. A facility with a noncertified general purpose x-ray 28 29 system must comply with items A to C. 30 Means must be provided to limit the x-ray field in Α. 31 the plane of the image receptor so the field does not exceed each dimension of the image receptor by more than two percent of 32 the SID when the axis of the x-ray beam is perpendicular to the 33 34 plane of the image receptor. Means must be provided to align the center of the 35 в.

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x-ray field with the center of the image receptor to within two

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1 percent of the SID, or means must be provided to both size and 2 align the x-ray field so the x-ray field at the plane of the 3 image receptor does not extend beyond any edge of the image 4 receptor.

5 C. The requirements of items A and B may be met with 6 a system that meets the requirements for a general purpose x-ray 7 system as specified in subpart 3. When alignment means are also 8 provided, the requirements of items A and B may be met with 9 either:

(1) an assortment of removable, fixed-aperture, beam-limiting devices sufficient to meet the requirement for each combination of image receptor size and SID for which the system is designed with each device having clear and permanent markings to indicate the image receptor size and SID for which it is designed; or

16 (2) a beam-limiting device having multiple fixed 17 apertures sufficient to meet the requirement for each 18 combination of image receptor size and SID for which the system is designed. Permanent, clearly legible markings must indicate 19 the image receptor size and SID for which each aperture is 20 21 designed and must indicate which aperture is in position for use. 22 Subp. 7. Radiation exposure, x-ray controls. An x-ray 23 control must be incorporated into each x-ray system so an 24 exposure can be terminated by the operator at any time during exposures of greater than one-half second. During serial 25 radiography means must be provided to permit completion of any 26 27 single exposure of the series in process before terminating the 28 series.

Subp. 8. Radiation exposure, automatic exposure controls.
When an automatic exposure control is provided:

31 A. indication must be made on the control panel when 32 this mode of operation is selected;

33 B. the minimum exposure time for all radiographic 34 systems, other than that specified in item E, must be equal to 35 or less than 1/60 second or a time interval required to deliver 36 five milliamperes-second, whichever is greater;

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1 c. either the product of the kVp, milliamperage, and exposure time must be limited to not more than 60 kWs per 2 3 exposure, or the product of x-ray milliamperage and exposure 4 time must be limited to not more than 600 mAs per exposure; a visible signal must indicate when an exposure 5 D. 6 has been terminated at the limits required by item C, and manual resetting must be required before further automatically timed 7 exposures can be made; and 8

9 E. if the kVp is equal to or greater than 50 kVp, the 10 minimum exposure time for field emission equipment rated for 11 pulsed operation must be equal to or less than a time interval 12 equivalent to two pulses.

Subp. 9. Source-to-skin distance. All portable x-ray systems must be provided with means to maintain a minimum source-to-skin distance equal to or greater than 30 centimeters (11.8 inches).

17 Subp. 10. Radiation from capacitor energy storage 18 equipment in standby status. Radiation emitted from the x-ray 19 tube when the exposure switch or timer is not activated must not 20 exceed a rate of two milliroentgens (0.5 uC/kg) per hour at five 21 centimeters (1.97 inches) from any accessible surface of the 22 diagnostic source assembly, with the beam-limiting device fully 23 open.

Subp. 11. Additional requirements for certified systems only. The standards in items A to D are applicable to certified x-ray systems only.

A. Stationary and portable general purpose x-ray
systems must have means to limit the useful beam.

(1) There must be provided a means of stepless
adjustment of the size of the x-ray field. The minimum field
size at a SID of 100 centimeters (39.4 inches) must be equal to
or less than five by five centimeters (1.97 by 1.97 inches).

33 (2) When a light localizer is used to define the
34 x-ray field, it must provide an average illumination of not less
35 than 160 lux (15.0 foot candles) above ambient at 100
36 centimeters (39.4 inches) or at the maximum SID, whichever is

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1 less. The average illumination must be based upon measurements made in the approximate center of each quadrant of the light 2 field. Radiation therapy simulation systems installed on and 3 after May 27, 1980, are exempt from this requirement. 4 5 (3) The edge of the light field at 100 centimeters (39.4 inches) or at the maximum SID, whichever is 6 less, must have a contrast ratio, corrected for ambient 7 lighting, of not less than four in the case of beam-limiting 8 9 devices designed for use on stationary x-ray systems, and a 10 contrast ratio of not less than three in the case of 11 beam-limiting devices designed for use on portable x-ray 12 systems. The contrast ratio is defined as I_1/I_2 where I_1 is the 13 illumination three millimeters (0.12 inches) from the edge of the light field toward the center of the field; and I2 is the 14 illumination three millimeters (0.12 inches) from the edge of 15 the light field away from the center of the field. Compliance 16 must be determined with a measuring instrument aperture of one 17 millimeter (0.04 inches) in diameter. 18 B. The useful beam limitation for portable x-ray 19 20 systems must meet the beam limitation requirements of item A and 21 subpart 3. This item applies to those general purpose x-ray 22 c. systems which contain a tube housing assembly, an x-ray control, 23

and a table (if so equipped). The system must be certified according to Code of Federal Regulations, title 21, section 1020.30(c). The system must meet the standards in subitems (1) to (6).

(1) Positive beam limitation must be provided
according to the criteria in units (a) to (f).

30 (a) The image receptor must be inserted into31 a permanently mounted cassette holder.

32 (b) The image receptor length and width must33 each be less than 50 centimeters (19.7 inches).

34 (c) The x-ray beam axis must be within plus
35 or minus three degrees of vertical and the SID must be 90
36 centimeters to 130 centimeters (35.4 inches to 51.2 inches)

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08/01/91 [REVISOR] LMB/BD AR1543 1 inclusive; or the x-ray beam axis must be within plus or minus 2 three degrees of horizontal and the SID must be 90 centimeters to 205 centimeters (35.4 inches to 80.7 inches) inclusive. 3 (d) The x-ray beam axis must be 4 perpendicular to the plane of the image receptor to within plus 5 or minus three degrees. 6 (e) Neither tomographic nor stereoscopic 7 radiography shall be performed. 8 9 (f) The positive beam limitation system must 10 not be intentionally overridden. This override provision is subject to the provisions of item C, subitem (3). 11 12 (2) Positive beam limitation must prevent the 13 production of x-rays when: 14 (a) the length or width of the x-ray field in the plane of the image receptor differs from the 15 16 corresponding image receptor dimensions by more than three percent of the SID except as permitted by subitem (4); or 17 (b) the sum of the length and width 18 19 differences as stated in unit (a) without regard to sign exceeds four percent of the SID. 20 21 (3) If a method of overriding the positive beam 22 limitation system exists, that method must be designed for use only in the event of positive beam limitation system failure or 23 24 if the system is being serviced. If the positive beam limitation system is in a position that the operator considers 25 26 part of the operational controls or if it is referenced in the 27 operator's manual or in other materials intended for the 28 operator: 29 (a) a key must be used to override the 30 positive beam limitation; 31 (b) the key must remain in place during the entire time the positive beam limitation system is overridden; 32 and 33 34 (c) that the key or key switch must be clearly and durably labeled as follows: "FOR X-RAY FIELD 35

LIMITATION SYSTEM FAILURE."

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(4) Compliance with item C, subitem (2), must be
 determined when the equipment indicates the beam axis is
 perpendicular to the plane of the image receptor and the
 provisions of item C, subitem (1), are met. Compliance must be
 determined no sooner than five seconds after insertion of the
 image receptor.

7 (5) The positive beam limitation system must be 8 capable of operation, at the discretion of the operator, so that 9 the size of the field may be made smaller than the size of the 10 image receptor through stepless adjustment of the field size. 11 The minimum field size at an SID of 100 centimeters (39.4 12 inches) must be equal to or less than five centimeters by five 13 centimeters (1.97 inches by 1.97 inches).

14 (6) The positive beam limitation system must be 15 designed so that if a change in image receptor does not cause an 16 automatic return to positive beam limitation function as 17 described in item C, subitem (2), then any change of image 18 receptor size of SID must cause the automatic return.

19 D. For x-ray systems installed after September 5, 20 1978, designed only for mammography, the transmission of the 21 primary beam through any image receptor support provided with the system must be limited so the exposure five centimeters 22 (1.97 inches) from any accessible surface beyond the plane of 23 24 the image receptor supporting device does not exceed 0.1 milliroentgen (25.8 nC/kg) for each activation of the tube. 25 26 Exposure must be measured with the system operated at the 27 minimum SID for which it is designed. Compliance must be determined at the maximum kVp for the system and at the maximum 28 29 rated product of milliamperage and exposure time 30 (milliampere-seconds) for that kVp. Compliance must be determined by measurements averaged over an area of 100 square 31 32 centimeters (15.5 square inches) with no linear dimension greater than 20 centimeters (7.9 inches). 33

34 4730.1950 INTRAORAL DENTAL RADIOGRAPHIC SYSTEMS.
35 Subpart 1. Applicability. This part applies to x-ray

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systems used for intraoral dental radiography. Requirements for
 extraoral dental radiographic systems are covered in part
 4730.1850. This part applies in addition to the requirements in
 parts 4730.0100 to 4730.1750.
 Subp. 2. Source-to-skin distance. X-ray systems designed

6 for use with an intraoral image receptor must be provided with a 7 position-indicating-device to limit source-to-skin distance to 8 not less than 18 centimeters (7.1 inches).

9 Subp. 3. Field limitation. Radiographic systems designed 10 for use with an intraoral image receptor must be provided with 11 and used with collimation to limit the x-ray field such that:

A. if the minimum source-to-skin distance is 18 centimeters (7.1 inches) or more, the x-ray field, at the minimum, must be containable in a circle having a diameter of no more than seven centimeters (2.76 inches); or

B. with rectangular position-indicating-devices, the longer side must not exceed 5.1 centimeters (two inches); and C. the x-ray system must be operated so the useful beam at the patient's skin does not exceed the requirements of this subpart.

21 Subp. 4. Safety controls. The registrant must ensure that 22 the safety controls in this subpart are followed.

A. Intraoral film holders and bite blocks must beused. Film must not be held by hand.

25 B. The tube housing and the

26 position-indicating-device must not be hand-held during an
27 exposure and must be stable before the exposure is initiated and
28 during the exposure.

29 C. Adults of reproductive age and children must be 30 provided with gonadal protection when a full mouth series of 31 exposures are made with intraoral radiography.

32 D. Structural-shielding-in-addition-to-the
 33 requirements-of-part-4730.1620-must-be-provided.
 34 (1)-Dental-rooms-containing-intraoral

35 radiographic-systems-must-be-provided-with-barriers-at-all-areas

36 struck-by-the-useful-beam---In-many-cases-structural-materials

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of-ordinary-walls-suffice-as-a-protective-barrier-without-the 1 addition-of-special-shielding-material. 2 (2)-When-dental-intraoral-radiographic-systems 3 are-installed-in-adjacent-rooms-or-areas,-protective-barriers 4 5 must-be-provided-between-the-rooms-or-areas-6 E---Each-installation-must-be-provided-with-a 7 protective-barrier-for-the-operator-or-must-be-so-arranged-that the-operator-can-stand-at-least-six-feet-from-the-patient-and 8 9 the-tubehead-and-not-in-the-path-of-the-useful-beam-10 F. The exposure at the end of the cone must not 11 exceed the values listed in Table 4730.1950: 12 TABLE 4730.1950 13 14 "D" Speed Film "E Speed Film" kVp 15 ESE ESE 16 (milliroentgens) (milliroentgens) 425 - 575350 - 500220 - 320190 - 270 50 17 18 55 310 - 44019 60 165 - 23020 65 270 - 400140 - 200 240 - 350170 - 260150 - 23070 21 120 - 170100 - 14022 75 100 90 -23 80 120 24 130 - 20080 - 105 85 70 - 9060 - 8050 - 7025 90 120 - 180 110 - 160100 - 14026 95 27 100 28 29 Notes: 30 (1) Exposures are specified as free-in-air exposures without backscatter. 31 32 (2) The indicated kVp is often significantly 33 different from the actual kVp. The kVp must be tested at the 34 time the output per film is measured to determine the correct 35 exposure range to be applied. 36 4730.2050 VETERINARY MEDICINE RADIOGRAPHIC INSTALLATIONS. 37 Subpart 1. Applicability. This part applies to x-ray systems used for diagnostic veterinary medicine radiography and 38 39 applies in addition to the requirements in parts 4730.0100 to 4730.1750. Requirements for fluoroscopic veterinary medicine 40 systems are covered in part 4730.2150. Requirements for 41 therapeutic veterinary medicine shall be the same as those in 42

08/01/91 [REVISOR] LMB/BD AR1543 1 parts 4730.2350, 4730.2450, and 4730.2475. 2 Subp. 2. Beam limitation. Collimators must be provided to restrict the useful beam to the area of clinical interest and 3 must provide the same degree of protection as is required of the 4 5 tube housing. Α. If a variable-aperture beam limiting collimator is 6 available, the projected light and x-ray field must not exceed 7 the dimensions smallest dimension of the x-ray film cassette by 8 9 greater than two percent of the distance of the x-ray tube to 10 the film (SID) in any direction. 11 If a fixed dimension beam limiting collimator is в. 12 used, it must meet the additional requirements in subitems (1) to (3). 13 14 (1) The collimator must be labeled to indicate the field size and the SID for which it is designed. 15 16 (2) The collimator must be used only for the 17 field size and the SID for which it is designed. (3) The x-ray field must not exceed the x-ray 18 19 film cassette by greater than two percent of the distance of the x-ray tube to the film SID in the x-ray film cassette's smallest 20 dimension. 21 22 C. In the case of horizontal beam x-rays a mechanical cassette holding device must be used to ensure that no part of 23 24 the body of the individual steadying the cassette is exposed to primary beam x-rays. 25 D. If necessary, and any involved individual is 26 27 properly attired in protective apron and gloves of at least 0.5 mm lead equivalency, this does not preclude the operation of the 28 radiographic system by one of the individuals holding the animal 29 patient using a foot switch. 30 31 Subp. 3. Operating procedures. The registrant must ensure 32 that the operating procedures in this subpart are applied. The operator must not stand in the path of the 33 Α. useful beam during radiographic exposures. 34 No individual other than the operator must be in 35 Β. 36 the radiographic room while exposures are being made unless the

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1 individual's assistance is required.

C. When an animal must be held in position by an <u>individual</u> during radiography, mechanical-support,-restraint devices,-or-chemical-restraint-must-be-used.--If-the-animal-must be-held-by-an-individual, that individual must wear protective gloves and apron of at least 0.5 mm lead equivalency, and the individual must be positioned so no part of the body, protected or unprotected, will be struck by the useful beam.

9 4730.2150 FLUOROSCOPIC X-RAY SYSTEMS.

Subpart 1. Applicability. This part applies to all fluoroscopic x-ray systems in addition to the requirements in parts 4730.0100 to 4730.1750.

Subp. 2. Limitation of useful beam, primary barrier. For all fluoroscopes, the requirements in items A and B must be met. A. The fluoroscopic imaging assembly must be provided with a primary protective barrier which intercepts the entire cross section of the useful beam at any SID.

B. The x-ray tube used for fluoroscopy must not
produce x-rays unless the barrier is in position to intercept
the entire useful beam.

21 Subp. 3. Limitation of useful beam, x-ray field. All 22 fluoroscopes must be provided with image intensification 23 equipment to view the fluoroscopic images.

A. For image-intensified fluoroscopic equipment, neither the length nor the width of the x-ray field in the plane of the image receptor must exceed that of the visible area of the image receptor by more than three percent of the SID. The sum of the excess length and the excess width must be no greater than four percent of the SID. In addition, means must be provided to permit further limitations of the field:

(1) Beam-limiting devices installed after May 22, 1979, and incorporated in equipment with either a variable SID or a visible area of greater than 300 square centimeters (46.5 square inches), must be provided with means for the stepless adjustment of the x-ray field.

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1 (2) All equipment with a fixed SID and a visible area of 300 square centimeters (46.5 square inches) or less must 2 be provided with either stepless adjustment of the x-ray field 3 4 or with means to further limit the x-ray field size at the plane 5 of the image receptor to 125 square centimeters (19.4 square inches) or less. Stepless adjustment must, at the greatest SID, 6 7 provide continuous field sizes from the maximum obtainable to a field size of five by five centimeters (1.97 by 1.97 inches) or 8 9 less.

10 (3) For fluoroscopic x-ray systems installed 11 after February 25, 1978, when the angle between the image 12 receptor and beam axis is variable, means must be provided to 13 indicate when the axis of the x-ray beam is perpendicular to the 14 plane of the image receptor.

(4) Compliance must be determined with the beam axis indicated to be perpendicular to the plane of the image receptor. For rectangular x-ray fields used with circular image reception, the error in alignment must be determined along the length and width dimensions of the x-ray field which pass through the center of the visible area of the image receptor.

21 B. Spot-film devices which are certified components 22 must meet the additional requirements in subitems (1) to (4):

(1) Means must be provided between the source and 23 the patient for adjustment of the x-ray field size in the plane 24 of the film to the size of that portion of the film which has 25 been selected on the spot-film selector. Such adjustment must 26 27 be automatically accomplished, except when the x-ray field size in the plane of the film is smaller than that of the selected 28 portion of the film. For spot-film devices installed after June 29 21, 1979, if the x-ray field size is less than the size of the 30 selected portion of the film, the means for adjustment of the 31 32 field size must be only at the operator's option.

33 (2) It must be possible to adjust the x-ray field
34 size in the plane of the film to a size smaller than the
35 selected portion of the film. The minimum field size at the
36 greatest SID must be equal to, or less than, five by five

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08/01/91 [REVISOR] LMB/BD AR1543 centimeters (1.97 by 1.97 inches). 1 (3) The center of the x-ray field in the plane of 2 3 the film must be aligned with the center of the selected portion 4 of the film to within two percent of the SID. (4) On spot-film devices installed after February 5 25, 1978, if the angle between the plane of the image receptor 6 7 and beam axis is variable, means must be provided to indicate 8 when the axis of the x-ray beam is perpendicular to the plane of 9 the image receptor. Compliance must be determined with the beam 10 axis indicated to be perpendicular to the plane of the image 11 receptor. 12 c. If a means exists to override any of the automatic 13 x-ray field size adjustments required in this subpart, that 14 means must: 15 (1) be designed for use only in the event of 16 system failure; 17 (2) incorporate a signal visible at the fluoroscopist's position which indicates whenever the automatic 18 19 field size adjustment is overridden; and 20 (3) be clearly and durably labeled as follows: 21 "FOR X-RAY FIELD LIMITATION SYSTEM FAILURE." 22 Subp. 4. Activation of the fluoroscopic tube. X-ray production in the fluoroscopic mode must be controlled by a 23 24 device which requires continuous pressure by the fluoroscopist for the entire time of any exposure. When recording serial 25 26 fluoroscopic images, the fluoroscopist must be able to terminate 27 the x-ray exposure at any time, but means may be provided to permit completion of any single exposure of the series in 28 29 process. 30 Subp. 5. Entrance exposure rate allowable limits. The registrant must ensure that the entrance exposure rate allowable 31 32 limits in this subpart are applied to a fluoroscopic x-ray 33 system. 34 The exposure rate measured at the point where the Α. center of the useful beam enters the patient must not exceed ten 35

roentgens (2.6 mC/kg) per minute, except during recording of

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fluoroscopic images or when provided with optional high level 1 2 control. Under optional high level control, except during 3 recording of fluoroscopic images, the maximum entrance exposure rate must not exceed 20 roentgens (5.2 mC/kg) per minute. 4 5 в. In addition to the other requirements of this 6 part, certified systems which do not incorporate an automatic 7 exposure rate control must not be operable at any combination of 8 kVp and milliamperage, which will result in an exposure rate in excess of five roentgens (1.3 mC/kg) per minute at the point 9 10 where the center of the useful beam enters the patient. This 11 requirement must not apply during recording of fluoroscopic 12 images, or when an optional high level control is activated. 13 c. When provided with optional high level control, 14 the fluoroscopic x-ray system must not be operable at any 15 combination of kVp and milliamperage which results in an exposure rate in excess of five roentgens (1.3 mC/kg) per minute 16 17 at the point where the center of the useful beam enters the patient unless the high level control is activated. 18 19 (1) Special means of activation of high level 20 controls must be required. The high level control must only be operable when continuous manual activation is provided by the 21 22 fluoroscopist. 23 (2) A continuous signal, audible to the fluoroscopist, must indicate that the high level control is 24 25 being employed. 26 D. Compliance with the requirements of subpart 5 must 27 be determined as specified in this item: (1) A one-eighth inch (3 mm) thick sheet of lead 28 29 that covers the entire cross section of the primary beam must be placed in the beam at a minimum distance of 15 centimeters (5.9 30 31 inches) from the point of measurement on the image receptor side of the patient. 32 33 (2) If the source is below the tabletop or cradle, the exposure rate must be measured one centimeter (0.4 34 inch) above the tabletop or cradle. 35 36 (3) If the source is above the tabletop or

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1 cradle, the exposure rate must be measured at 30 centimeters
2 (11.8 inches) above the tabletop or cradle with the end of the
3 beam-limiting device or spacer positioned as close as possible
4 to the point of measurement.

5 (4) All C-arm fluoroscopes, both stationary and portable, must meet the entrance exposure rate limits in subpart 6 7 5, items A and B, at a point 30 centimeters (11.8 inches) from the input surface of the fluoroscopic imaging assembly, with the 8 source positioned at any available SID provided so that the end 9 10 of the spacer assembly or beam-limiting device is not closer than 30 centimeters (11.8 inches) from the input surface of the 11 12 fluoroscopic imaging assembly.

E. Periodic measurement of the maximum and clinical exposure rate must be performed as specified in this item:

(1) The measurements must be made annually or after any maintenance of the system which might affect the exposure rate.

(2) The results of these measurements must be 18 19 posted where any fluoroscopist may have ready access to them 20 while using the fluoroscope and in the record required in part 4730.1520, subpart 1, item D. The measurement results must be 21 stated in roentgens or mC/kg per minute and must include the 22 23 technique factors used in determining such results. The name of the individual performing the measurements and the date the 24 25 measurements were performed must be included in the results. 26 (3) The conditions for the periodic measurement 27 of the clinical entrance exposure rate are as follows: 28 (a) the measurement must be made under the 29 conditions that satisfy the requirements of item D, subitems 30 (2), (3), and (4); (b) the kVp must be the kVp typical of 31 32 clinical use of the x-ray system; 33 (c) the x-ray system that incorporates the automatic exposure rate control must have sufficient material 34 placed in the useful beam to produce a kilovoltage and 35 milliamperage typical of the use of the x-ray system; and 36

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1 (d) the x-ray system that does not
2 incorporate an automatic exposure rate control must use a
3 kilovoltage and milliamperage typical of the clinical use of the
4 x-ray system.

5 (e) Materials must be placed in the useful 6 beam when conducting these periodic measurements to protect the 7 imaging system.

8 (4) The periodic measurement of the maximum 9 entrance exposure rate must be made under the conditions that 10 satisfy the requirements of item D. For x-ray systems that do 11 not incorporate an automatic exposure rate control, the 12 kilovoltage and milliamperage must be manually adjusted to 13 produce the maximum entrance exposure rate.

14 Subp. 6. Barrier transmitted radiation rate limits. The 15 exposure rate due to transmission through the primary protective 16 barrier with the attenuation block in the useful beam, combined 17 with radiation from the image intensifier, must not exceed two 18 milliroentgens (0.5 uC/kg) per hour at ten centimeters (3.9 19 inches) from any accessible surface of the fluoroscopic imaging 20 assembly beyond the plane of the image receptor for each 21 roentgen per minute or millicoulomb per kilogram per minute of entrance exposure rate. 22

Subp. 7. Measuring compliance of barrier transmission.
Compliance with subpart 6 shall be determined according to this
subpart.

A. The exposure rate due to transmission through the primary protective barrier combined with radiation from the image intensifier must be determined by measurements averaged over an area of 100 square centimeters (15.5 square inches) with no linear dimension greater than 20 centimeters (7.9 inches).

31 B. If the source is below the tabletop or cradle, the 32 measurement must be made with the input surface of the 33 fluoroscopic imaging assembly positioned 30 centimeters (11.8 34 inches) above the tabletop or cradle.

35 C. If the source is above the tabletop or cradle and 36 the SID is variable, the measurement must be made with the end

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of the beam-limiting device or spacer as close to the tabletop 1 2 as it can be placed, provided that it must not be closer than 30 3 centimeters (11.8 inches). 4 D. The attenuation block must be positioned in the useful beam ten centimeters (3.9 inches) from the point of 5 measurement of entrance exposure rate and between this point and 6 7 the input surface of the fluoroscopic imaging assembly. Subp. 8. Indication of potential kilovoltage and current 8 9 milliamperage. For fluoroscopic x-ray systems manufactured and 10 installed after February 25, 1978, during fluoroscopy and 11 cinefluorography, the kilovoltage and the milliamperage must be 12 continuously indicated. 13 Subp. 9. Source-to-skin distance. The source-to-skin distance must not be less than: 14 15 Α. 38 centimeters (15 inches) on stationary 16 fluoroscopes; 17 в. 35.5 centimeters (14 inches) on stationary fluoroscopes manufactured prior to August 1, 1974; 18 19 C. 30 centimeters (11.8 inches) on all portable 20 fluoroscopes; and 21 D. 20 centimeters (7.9 inches) for image intensified 22 fluoroscopes used for specific surgical applications. The written safety procedures must provide precautionary measures to 23 24 be adhered to when image intensified fluoroscopes are used for 25 specific surgical applications. 26 The 20 centimeter (7.9 inch) spacer cone must be replaced 27 with the 30 centimeter (11.8 inch) spacer cone immediately after 28 the end of the fluoroscopic surgical procedure. 29 Subp. 10. Fluoroscopic timer. Means must be provided to preset the cumulative on-time of the fluoroscopic x-ray tube. 30 31 The maximum cumulative time of the timing device must not exceed 32 five minutes without resetting. A signal audible to the fluoroscopist must indicate the completion of any preset 33 34 cumulative on-time. The signal must continue to sound while x-rays are produced, until the timing device is reset. 35 36 Subp. 11. Control of scattered radiation. The procedures

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1 in this subpart must be used to control scattered radiation from 2 all fluoroscopes.

A. When a fluoroscopic table with an undertable x-ray tube is used, the bucky opening must be attenuated by 0.25 millimeter lead equivalent. Drapes must be attached to the intensifier tower to attenuate scattered radiation. The drapes must provide 0.25 millimeter lead equivalent attenuation of the scattered radiation.

9 B. For other undertable configurations, provisions 10 must be made through equipment design or radiation protection 11 measures to assure that individuals do not receive a dose in 12 excess of the allowable dose limits listed in part 4730.0310.

(1) Any individual who must be in the room during a fluoroscopic procedure must wear a protective apron of not less than 0.5 millimeter lead equivalence.

16 (2) All fluoroscopic x-ray systems must be 17 provided with a bucky-slot cover panel and either drapes on <u>or</u> 18 self-supporting curtains of not less than 0.5 millimeter lead 19 equivalent material.

C. For single-tube above table combination 20 21 radiographic and fluoroscopic x-ray systems used in the 22 fluoroscopic mode, protective aprons of not less than 0.5 millimeter lead equivalence must be used to assure that any 23 individual who must be in the room during a fluoroscopic 24 procedure does not receive a dose greater than the allowable 25 26 dose limits listed in part 4730.0310. In addition, portable 27 lead shields, barriers, or aprons of not less than 0.5 millimeter lead equivalence must be used. 28

D. For portable C-arm fluoroscopes, provision must be made through the use of protective aprons of not less than 0.5 millimeter lead equivalence to assure that any individual other than the patient who may be exposed during a fluoroscopic procedure does not receive a dose in excess of the allowable dose limits listed in part 4730.0310.

35 Subp. 12. Radiation therapy simulation systems. A 36 radiation therapy simulation system is exempt from the

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1 requirements of subpart 5, provided:

A. the system is designed and used so no individual other than the patient is in the simulation room when the system is producing x-rays; and

B. a system which does not meet the requirements of subpart 10 has a means to indicate the cumulative time that an individual patient has been exposed to x-rays. Procedures must require in such cases that the timer be reset between examinations.

10 4730.2250 COMPUTED TOMOGRAPHY SYSTEMS.

Subpart 1. Applicability. This part applies to all computed tomography systems in addition to the requirements in parts 4730.0100 to 4730.1750.

14 Subp. 2. Termination of exposure. A visible signal must 15 indicate when the x-ray exposure has been terminated. The 16 operator must be able to terminate the x-ray exposure at any 17 time during a scan, or series of scans under CT x-ray system 18 control, of greater than one-half second duration.

19 Subp. 3. Tomographic plane indication and alignment. The20 provisions in items A to C apply.

A. For any single slice tomogram system, means must be provided to permit visual determination of the tomographic plane or a reference plane offset from the tomographic plane.

B. For any multiple slice tomogram system, means must be provided to permit visual determination of the location of a reference plane. This reference plane can be offset from the location of the tomographic planes.

28 C. If a device using a light source is used to 29 satisfy either item A or B, the light source must provide 30 illumination levels of not less than 160 lux (15.0 foot candles) 31 above the room ambient illumination level.

32 Subp. 4. Beam-on and shutter status indicators. The x-ray 33 control and gantry must visually indicate whenever x-rays are 34 produced and, if applicable, whether the shutter is open or 35 closed. All emergency buttons or switches must be clearly

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1 labeled as to their functions.

2 Subp. 5. Indication of computed tomography conditions of 3 operation. The computed tomography x-ray system must be 4 designed so the computed tomography conditions of operation to be used during a scan or a scan sequence are indicated prior to 5 the initiation of the scan or a scan sequence. On equipment 6 7 having all or some of these conditions of operation at fixed 8 values, this requirement may be met by permanent markings. Indication of computed tomography conditions of operation must 9 10 be visible from any position from which scan initiation is 11 possible.

Subp. 6. Extraneous radiation. When data is not being 12 13 collected for image production, the radiation adjacent to the 14 tube port must not exceed the leakage radiation from the 15 diagnostic source assembly that is measured at a distance of one 16 meter (39.4 inches) in any direction from the source. That leakage must not exceed 100 milliroentgens (26 uC/kg) in one 17 hour when the x-ray tube is operated at its leakage technique 18 factors. Compliance must be determined by a measurement 19 20 averaged over an area of 100 square centimeters (15.5 square inches) with no linear dimension greater than 20 centimeters 21 22 (7.9 inches).

Subp. 7. Maximum surface computed tomography dose index identification. The angular position where the maximum surface computed tomography dose index occurs must be identified to allow for reproducible placement of a computed tomography dosimetry chamber.

Subp. 8. Additional requirements. Items A to D are applicable to computed tomography x-ray systems containing a gantry manufactured after September 3, 1985.

A. The total error in the indicated location of the tomographic plane or reference plane must not exceed five millimeters (0.2 inches).

B. If the x-ray production period is less than one-half second, the indication of x-ray production must be actuated for at least one-half second. Indicators at or near

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1 the patient side of the gantry must be discernible to the 2 operator.

The deviation of indicated scan increment versus 3 С. actual increment must not exceed plus or minus one millimeter 4 (0.04 inches) with a mass of 100 kilograms (220 pounds) resting 5 6 on the support device. The patient support device must be 7 incremented from a typical starting position to the maximum incremented distance or 30 centimeters (11.8 inches), whichever 8 9 is less, and then returned to the starting position. Measurement of actual versus indicated scan increment may be 10 11 taken anywhere along this incremented distance.

D. Premature termination of the x-ray exposure by the operator must necessitate resetting of the computed tomography conditions of operation before the initiation of another scan.

15 Subp. 9. Audio communication. Within the computed 16 tomography area, provision must be made for two-way audio 17 communication between the patient and operator at the control 18 panel.

19 Subp. 10. Patient observation. Within the computed 20 tomography area, provision must be made for a shielded window 21 containing the same lead equivalence as the adjoining walls so 22 the operator at the control panel may directly observe the 23 patient, any other individual in the room, and any doorways into 24 the room. A closed circuit television system may be used as a 25 secondary means of observing the patient.

Subp. 11. Location of control panel and x-ray control. The control panel and x-ray control must be mounted in a permanently protected area outside the computed tomography room. The operator is required to remain in that protected area during the entire exposure.

31 Subp. 12. Operating procedure information. Information 32 about the operation, radiation safety surveys, and quality 33 control measurements of the system must be available at the 34 control console. This information must contain:

35 A. the dates of the last radiation safety survey and 36 quality control measurements;

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1 в. written results of the most recent radiation safety survey and quality control measurements including: 2 3 (1) those specified in part 4730.1665, subparts 2 and 3; 4 5 (2) photographic images obtained from the 6 photographic image recording device; and 7 (3) images stored in digital form. 8 с. instructions on the use of the computed tomography phantoms, including a schedule of quality control checks 9 10 appropriate for the system, allowable variations for the 11 indicated measurements, and the results of the last two years' 12 quality control measurements in addition to the original quality control and acceptance test measurements, images, and digital 13 14 data; and 15 D. the distance in millimeters between the 16 tomographic plane and the reference plane if a reference plane 17 is used. 18 Subp. 13. Corrective action. If the quality assurance 19 control measurements required by part 4730.1665, subparts 2 and 20 3, of the computed tomography systems identify that a 21 measurement has exceeded a tolerance specified in part 4730.1691, the registrant must correct the measurement to within 22 the tolerances specified in part 4730.1691. Correction of the 23 24 problem must take place within five working days and must be 25 verified by performing the quality assurance control 26 measurements specified in part 4730.1665, subparts 2 and 3. 27 4730.2350 THERAPEUTIC X-RAY SYSTEMS OF LESS THAN ONE MeV MV. 28 Subpart 1. Applicability. In addition to the requirements 29 in parts 4730.0100 to 4730.1695, this part applies to all 30 therapeutic x-ray systems of less than one MeV MV. Subp. 2. Leakage radiation. When the tube is operated at 31 its leakage technique factors, the instantaneous exposure rate 32 leakage radiation must not exceed the value specified at the 33 34 distance specified in this subpart for the classification of

35 that x-ray system.

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A. Leakage radiation for contact therapeutic x-ray systems must not exceed 100 milliroentgens (25.8 uC/kg) per hour at five centimeters (1.97 inches) from the surface of the tube housing assembly.

5 B. Zero to 150 kVp systems installed prior to the 6 effective date of this chapter must have a leakage radiation 7 which does not exceed one roentgen (0.258 mC/kg) in one hour at 8 one meter (39.4 inches) from the source.

9 C. Zero to 150 kVp systems installed on or after the 10 effective date of this chapter must have a leakage radiation 11 which does not exceed 100 milliroentgens (25.8 uC/kg) in one 12 hour at one meter (39.4 inches) from the source.

D. 151 to 999 kVp systems must have leakage radiation which does not exceed one roentgen (0.258 mC/kg) in one hour at one meter (39.4 inches) from the source. However, systems that operate in excess of 500 kVp may have a leakage radiation <u>rate</u> at one meter (39.4 inches) from the source not to exceed 0.1 percent of the useful beam one meter (39.4 inches) from the source.

20 Subp. 3. Leakage from permanent beam limiting devices. 21 Permanent fixed diaphragms or cones used for limiting the useful 22 beam must provide the same or a higher degree of protection as 23 required for the tube housing assembly in subpart 2.

Subp. 4. Removable beam limiting devices. Removable beam limiting devices must, for the portion of the useful beam to be blocked by these devices, transmit not more than five percent of the useful beam at the maximum kilovoltage and maximum treatment filter. This requirement does not apply to auxiliary blocks or materials placed in the useful beam to shape the useful beam to the individual patient.

31 Subp. 5. Adjustable beam limiting devices. Adjustable 32 beam limiting devices installed after the effective date of this 33 chapter must meet the requirements of subpart 4. Adjustable 34 beam limiting devices installed before the effective date of 35 this chapter must, for the portion of the x-ray beam to be 36 blocked by these devices, not transmit more than five percent of

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1 the useful beam at the maximum kilovoltage and maximum treatment
2 filter.

3 Subp. 6. Filter system. The filter system must be 4 designed so:

5 A. the filters cannot be accidentally displaced at 6 any possible tube orientation;

B. the radiation at five centimeters (1.97 inches) from the filter insertion slot opening does not exceed 30 roentgens (7.74 mC/kg) per hour under any operating condition; and

11 C. each filter is marked as to its material of 12 construction and its thickness. For wedge filters, the wedge 13 angle must appear on the wedge or wedge tray.

Subp. 7. Tube immobilization. The tube housing assembly must be capable of being immobilized for stationary treatments. Subp. 8. Focal spot marking. The tube housing assembly must be marked so it is possible to determine the location of the focal spot to within five millimeters (0.2 inches), and such marking must be readily accessible for use during calibration procedures.

Subp. 9. Beam block. If the x-ray tube of a contact therapeutic x-ray system is hand-held during irradiation, the operator must wear protective gloves and apron. When practical, a cap of at least 0.5 millimeters lead equivalence must cover the aperture window of the tube housing of such apparatus when the apparatus is not being used.

27 Subp. 10. Timer. A timer which has a display must be 28 provided at the treatment control panel. The timer must:

A. have a preset time selector and an elapsed time
indicator;

31 B. be a cumulative timer which activates with the 32 production of radiation and retains its reading after the 33 irradiation is interrupted or terminated;

C. terminate irradiation when a preselected time has elapsed if any dose monitoring system present has not previously terminated irradiation;

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08/01/91 [REVISOR] LMB/BD AR1543 1 permit accurate presetting and determination of D. 2 exposure times within an accuracy of one second; 3 Ε. not permit an exposure if set at zero; and F. not activate until the shutter is opened when 4 5 irradiation is controlled by a shutter mechanism. Subp. 11. Control panel functions. The control panel must 6 7 have: 8 A. an indication of whether electrical power is available at the control panel and if activation of the x-ray 9 tube is possible; 10 11 B. an indication of whether x-rays are being produced; 12 13 С. meters that indicate kVp and mA; 14 D. means for terminating an exposure at any time; 15 Ε. a locking device which will prevent unauthorized 16 use of the x-ray system; and 17 F. for x-ray systems installed after the effective 18 date of this chapter, a positive display of all specific filters 19 in the beam. 20 Subp. 12. Multiple tubes. A control panel may energize 21 more than one x-ray tube if the x-ray tubes are located in the same room. In this situation, the following must apply: 22 23 A. it must be possible to activate only one x-ray 24 tube at any time; 25 B. there must be an indication at the control panel 26 identifying which x-ray tube is energized; and 27 C. there must be an indication at the tube housing 28 assembly when that tube is energized. 29 Subp. 13. Source-to-skin distance. There must be means of 30 determining the source-to-skin distance to within two millimeters (0.08 inches). 31 32 Subp. 14. Shutters. Unless it is possible to bring the 33 x-ray output to the prescribed exposure parameters within five 34 seconds, the beam must be automatically attenuated by a shutter 35 having a lead equivalence of not less than that of the tube 36 housing assembly. In addition:

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A. after the system is at operating parameters, the shutter must be controlled electrically by the operator from the control panel; and

B. an indication of the shutter position must appear 5 at the control panel.

6 Subp. 15. Low-filtration x-ray tubes. Each x-ray system 7 equipped with a beryllium or other low-filtration window must be 8 clearly labeled as "beryllium window" or "low-filtration window" 9 on the tube housing assembly and at the control panel.

Subp. 16. Entrance interlocks. For therapeutic x-ray 10 11 systems capable of operation above 150 kVp, interlocks must be 12 provided so all entrance doors to the radiation therapy room are closed before treatment can be initiated or continued. If the 13 14 radiation beam is interrupted by any door opening, it must not 15 be possible to restore the system to operation without closing 16 the door and reinitiating irradiation by manual action at the control panel. When any entrance door is opened while the x-ray 17 tube is activated, the exposure at a distance of one meter (39.4 18 19 inches) from the source must be reduced to less than 100 20 milliroentgens (0.001 sieverts or one millisievert) per hour.

Subp. 17. Operating procedures. The tube housing assembly must not be held by hand during operation unless the system is designed to require such holding and the kVp of the system does not exceed 50 kVp. In such cases, the holder must wear protective gloves and apron of not less than 0.5 millimeter lead equivalence at 100 kVp.

Subp. 18. Additional requirements. The x-ray system must not be used in the administration of radiation therapy unless the requirements of parts 4730.1675, subpart 2, and 4730.1680, subpart 1, item items C and D, have been met.

31 4730.2450 X-RAY AND ELECTRON THERAPY SYSTEMS WITH ENERGIES OF 32 ONE MeV MV AND ABOVE.

33 Subpart 1. Applicability. In addition to the requirements 34 in parts 4730.0100 to 4730.1695, the requirements in this part 35 shall apply to the use of therapeutic x-ray systems with

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1 energies of one MeV \underline{MV} and above.

2 Subp. 2. System requirements; leakage radiation to the 3 patient area. All x-ray and electron therapy systems or any 4 part of a system must meet the requirements in this subpart.

A. Systems or any part of a system installed after the effective date of this chapter must meet the following requirements:

8 (1) For operating conditions producing maximum 9 leakage radiation, the absorbed dose in rads (cGy) due to any 10 leakage radiation component, including x-rays, electrons, and 11 neutrons, at any point in a circular plane of two meters (78.7 12 inches) radius centered on or perpendicular to the central axis 13 of the beam at the isocenter (patient plane), or nominal treatment distance and outside the maximum useful beam size must 14 not exceed 0.1 percent of the maximum absorbed dose in rads 15 (grays) of the unattenuated useful beam measured at the point of 16 intersection of the central axis of the beam and the circular 17 18 plane surface.

Measurements, excluding those for neutrons, must be averaged over an area up to but not exceeding 100 square centimeters (15.5 square inches) at the positions specified in this item. Measurements of the portion of the leakage radiation dose contributed by neutrons must be averaged over an area up to but not exceeding 200 square centimeters (31 square inches). (2) For each system, the registrant must

26 determine or obtain from the manufacturer the leakage radiation 27 existing at the positions specified in subitem (1) for the 28 operating conditions specified in that subitem.

B. Systems installed before the effective date of
this chapter must meet the following requirements:

(1) For operating conditions producing maximum leakage radiation, the absorbed dose in rads (cGy) due to leakage radiation, excluding neutrons, at any point in a circular plane of a two meter (78.7 inch) radius centered on a plane perpendicular to the central axis of the beam two meters (78.7 inches) from the virtual source, and outside the maximum

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size useful beam, must not exceed 0.1 percent of the maximum absorbed dose in rads (grays) of the unattenuated useful beam measured at the point of intersection of the central axis of the beam and the surface of the circular plane. Measurements must be averaged over an area up to but not exceeding 100 square centimeters (15.5 square inches) at the positions specified in this item.

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8 (2) For each system, the registrant must 9 determine or obtain from the manufacturer the leakage radiation 10 existing at the positions specified in subitem (1) for the 11 operating conditions specified in that subitem.

12 Subp. 3. Leakage of radiation outside the patient area for 13 systems or any part thereof installed after the effective date 14 of this chapter. For systems or any part of a system installed 15 after the effective date of this chapter, the system must meet 16 the requirements in this subpart.

17 A. The absorbed dose in rads (cGy) due to leakage 18 radiation, except in the area specified in subpart 2, item A, 19 subitem (1), when measured at any point one meter (39.4 inches) 20 from the path of the charged particle, before the charged 21 particle strikes the target or window, must not exceed 0.1 percent of the maximum absorbed dose in rads (cGy) of the 22 23 neutrons and must not exceed 0.1 percent of the maximum absorbed 24 dose in rads (CGy) of the photons of the unattenuated useful beam measured at the point of intersection of the central axis 25 26 of the beam and the circular plane specified in subpart 2, item 27 A, subitem (1).

28 Β. The registrant must determine or obtain from the manufacturer, the actual leakage radiation existing at the 29 30 positions specified in item A for specified operating conditions. Radiation measurements, excluding neutrons, must be 31 averaged over an area up to but not exceeding 100 square 32 33 centimeters (15.5 square inches). Neutron measurements must be averaged over an area up to but not exceeding 200 square 34 35 centimeters (31 square inches).

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Subp. 4. Beam limiting devices. Adjustable or

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1 interchangeable beam limiting devices must be provided, and the 2 devices must transmit no more than five percent of the useful 3 beam at the nominal treatment distance for the portion of the 4 useful beam which is to be attenuated by the beam limiting 5 device. This requirement does not apply to auxiliary blocks or materials placed in the useful beam to shape the useful beam to 6 7 the individual patient. The neutron component of the useful 8 beam must be excluded from the calculation of the five percent limitation. 9

10 Subp. 5. Filters. All x-ray and electron therapy systems 11 must have filters that meet the requirements in this subpart.

A. All compensating removable filters must be clearly identified. Documentation available at the control panel must contain a description of the filter. For wedge filters, the wedge angle must appear on the wedge or wedge tray.

B. If the absorbed dose rate data required by subpart 17 17 relates exclusively to operation with a field flattening or 18 beam scattering filter in place, the filter must be removable 19 only with the use of tools.

20 C. For systems or any part of a system installed 21 after the effective date of this chapter, which uses a system of 22 wedge filters, interchangeable field flattening filters, or 23 interchangeable beam scattering filters:

(1) irradiation must not be possible until a
selection of a filter has been made at the treatment control
panel;

(2) an interlock system must be provided to
prevent irradiation if the filter selected is not in the correct
position;

30 (3) a display must be provided at the treatment
31 control panel showing the filters in use; and
32 (4) an interlock must be provided to prevent
33 irradiation if any filter selection operation carried out in the
34 treatment room does not agree with the filter selection
35 operation carried out at the treatment control panel.
36 Subp. 6. Electron beam quality. The registrant must

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08/01/91 [REVISOR] LMB/BD AR1543 1 determine, or obtain from the manufacturer, data sufficient to 2 assure that the electron beam quality requirements specified in this subpart are met. 3 4 Α. The absorbed dose resulting from x-rays in a 5 useful electron beam at a point on the central axis of the beam ten centimeters (3.94 inches) greater than the practical range 6 7 of the electrons must not exceed the values stated in Table 4730.2450. Linear interpolation must be used for values not 8 9 stated. 10 TABLE 4730.2450 11 Maximum Energy of Electron X-Ray Absorbed Dose as 12 Beam in MeV a Fraction of Maximum 13 Absorbed Dose 14 1 0.03 15 15 0.05 16 35 0.10 17 50 0.20 18 19 Compliance with item A must be determined using: в. 20 (1) a measurement within a phantom with the incident surface of the phantom at the nominal treatment 21 22 distance and normal to the central axis of the beam; 23 (2) the largest field size available which does not exceed 15 by 15 centimeters (5.9 by 5.9 inches); 24 25 (3) all clinically relevant collimation systems; and 26 (4) a phantom whose cross-sectional dimensions 27 28 exceed the measurement radiation field by at least five centimeters (1.97 inches) and whose depth is sufficient to 29 30 perform the required measurement. 31 C. The registrant must determine, or obtain from the 32 manufacturer, the maximum percentage absorbed dose in the useful 33 beam due to neutrons, excluding stray neutron radiation, for specified operating conditions. 34 Subp. 7. Radiation detectors monitors. All therapeutic 35 x-ray systems must be provided with radiation detectors monitors 36 37 in the radiation head. 38 Systems or any part of a system installed after Α.

39 the effective date of this chapter must measure all therapeutic 40 radiation beams with at least two radiation detectors monitors.

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(c) use a design so that any increased dose
 is displayed by increasing numbers and must be so designed that,
 in the event of an overdosage of radiation, the absorbed dose
 may be accurately determined; and

5 (d) display the dose monitoring information 6 required by this subitem at the control panel and be retrievable 7 in at least one dose monitoring system for a five-minute period 8 of time in the event of a power failure.

9 (6) The internal dose monitoring system must be 10 capable of delivering a dose that varies by less than two 11 percent over a 12-hour period.

12 Subp. 8. Beam symmetry. For any system installed after the effective date of this chapter that has the capacity to 13 produce useful beams with asymmetry exceeding five percent, the 14 15 asymmetry of the radiation beam in two orthogonal directions 16 must be monitored before the beam passes through the beam limiting device. The asymmetry must be measured for a 30 square 17 18 centimeter (4.65 square inch) field at a depth of ten 19 centimeters (3.9 inches) at the points that correspond to 80 percent of the full width half maximum (FWHM) of central axis 20 21 value.

22 Capabilities must be provided so that, if the difference in 23 dose rate between one region of-the-body and another region of 24 the-body symmetrically displaced from the central axis of the 25 beam <u>in the same plane</u> exceeds five percent of the central axis 26 dose rate, indication of the dose rate difference is made at the 27 control panel; and if the dose rate difference exceeds five 28 percent, the irradiation is terminated.

Subp. 9. Selection and display of dose monitor units. All x-ray and electron therapy systems must provide for the selection and display of dose monitor units according to this subpart.

A. Irradiation must not be possible until a selection of a number of dose monitor units has been made at the treatment control panel.

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B. The preselected number of dose monitor units must

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be displayed at the treatment control panel until reset manually
 for the next irradiation.

C. On systems installed after the effective date of this chapter, <u>following an irradiation terminated by the dose</u> <u>monitoring system</u>, it must be necessary to manually reset the preselected dose monitor units after irradiation is terminated and before irradiation can be reinitiated.

8 Subp. 10. Termination of irradiation by the dose 9 monitoring system or systems during stationary beam therapy. 10 All x-ray and electron therapy systems must meet the 11 requirements in this subpart regarding termination of 12 irradiation by dose monitoring systems during stationary beam 13 therapy.

A. Each primary system must terminate irradiation when the preselected number of dose monitor units has been detected by the system.

B. If original design of the system included a second dose monitoring system, that system must be capable of terminating irradiation when not more than 15 percent or 40 dose monitor units, whichever is smaller, above the preselected number of dose monitor units set at the treatment control panel has been detected by the second dose monitoring system.

C. Systems installed after the effective date of this chapter must have a second dose monitoring system which terminates irradiation when not more than ten percent or 25 dose monitor units, whichever is smaller, above the preselected number of dose monitor units set at the treatment control panel has been detected by the second dose monitoring system.

D. Systems installed after the effective date of this chapter must have an indicator on the control panel that shows which dose monitoring system has terminated irradiation.

32 Subp. 11. Interruption switches. All x-ray and electron 33 therapy systems must have switches that allow the interruption 34 of irradiation and meet the requirements in this subpart.

A. It must be possible to interrupt irradiation and equipment movement at any time from the operator's position at

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1 the treatment control panel.

B. Emergency off switches must be placed on <u>or near</u> the treatment console;-and-on-a-wall-outside-the-treatment-room. Inside the treatment room, emergency off switches must be placed on <u>or near both sides of</u> the treatment couch, on-walls-to-the right-and-left-of-the-couch;-in-front-of-the-primary-beam; and in on or near both sides of the gantry stand.

8 Subp. 12. Termination switches. All x-ray and electron 9 therapy systems must have termination switches that make it 10 possible to terminate irradiation and equipment movements, or go 11 from an interruption condition to termination conditions, at any 12 time from the operator's position at the treatment control panel. 13 Subp. 13. Timer. All x-ray and electron therapy systems 14 must have a timer that meets the requirements in this subpart.

A. A timer which has a visual display must be provided at the treatment control panel. The timer must have a preset time selector and an elapsed time indicator.

B. The timer must be a cumulative timer which activates with the production of radiation and returns its reading after irradiation is interrupted or terminated. After irradiation is terminated and before irradiation can be reinitiated, it must be necessary to reset the elapsed time indicator to zero.

C. For systems installed after the effective date of this chapter, after termination of irradiation and before irradiation can be reinitiated, it must be necessary to manually reset the preset time selector.

D. The timer must terminate irradiation when a preselected time has elapsed if the dose monitoring systems have not previously terminated irradiation.

E. For systems installed after the effective date of this chapter, if the backup timer is automatically set by control circuitry, the additional time must not be more than ten percent above the time determined by dividing the number of monitor units (MU) by the monitor unit irradiation rate.

36 Subp. 14. Selection of radiation type. Therapy systems

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capable of emitting both x-rays and electrons must allow for the
 selection of the radiation type according to the requirements in
 this subpart.

A. Irradiation must not be possible until a selection 5 of radiation type has been made at the treatment control panel.

B. An interlock system must be provided to ensure
that the equipment can emit only the radiation type which has
been selected.

9 C. An interlock system must be provided to prevent 10 irradiation if any selected operations carried out in the 11 treatment room do not agree with the selected operations carried 12 out at the treatment control panel.

D. An interlock system must be provided to prevent irradiation with x rays except to obtain a port film when leectron applicators are fitted.

E. <u>An interlock system must be provided to ensure</u>
electron beam irradiations do not take place with inappropriate
beam modifiers such as wedges in the beam.

19 <u>F.</u> The radiation type selected must be displayed at 20 the treatment control panel before and during irradiation. 21 Subp. 15. Selection of energy. Systems capable of 22 generating radiation beams of different energies must allow for 23 the selection of the energy value according to the requirements 24 in this subpart.

A. Irradiation must not be possible until a selectionof energy has been made at the treatment control panel.

B. An interlock system must be provided to prevent irradiation if any selected operations carried out in the treatment room do not agree with the selected operations carried out at the treatment control panel.

31 C. The nominal energy value and photon or electron 32 modality selected must be displayed at the treatment control 33 panel before and during irradiation.

34 Subp. 16. Selection of stationary beam therapy or moving 35 beam therapy. Systems capable of both stationary beam therapy 36 and moving beam therapy must allow for the selection of

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stationary beam therapy or moving beam therapy according to the
 requirements in this subpart.

A. Irradiation must not be possible until a selection of stationary beam therapy or moving beam therapy has been made at the treatment control panel.

B. An interlock system must be provided to ensure
that the equipment can operate only in the mode which has been
selected.

9 C. An interlock system must be provided to prevent 10 irradiation if any selected operations carried out in the 11 treatment room do not agree with the selected operations carried 12 out at the treatment control panel.

D. The mode of operation must be displayed at thetreatment control panel.

E. For systems installed after the effective date of this chapter, an interlock system must be provided to terminate irradiation if:

18 (1) movement of the gantry occurs during19 stationary beam therapy; or

20 (2) movement of the gantry stops during moving21 beam therapy unless such stoppage is a preplanned function.

F. Moving beam therapy must be controlled to provideaccurate total dose and arc angle.

(1) For systems installed after the effective 24 date of this chapter, where the angle of rotation terminates the 25 26 radiation, the maximum difference between the delivered and expected monitor units (MU) must not exceed three percent or one 27 monitor unit, whichever is greater. The expected MU is 28 29 calculated by multiplying the set value of MU/degree by the set value of total gantry rotation angle. The observed terminal 30 gantry angle must be within plus or minus two three degrees of 31 expected. This requirement applies for all arcs of 45 degrees 32 or more at all MU/degree values indicated as "clinically usable" 33 34 by the manufacturer.

35 (2) For systems installed after the effective36 date of this chapter, where the dose monitoring system

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terminates the irradiation, the maximum difference between the 1 observed and expected angle of rotation of the gantry shall not 2 3 exceed plus or minus two three degrees. The expected angle of 4 rotation is calculated by dividing the set value of monitor 5 units by the set value of MU/degree. The agreement of elapsed MU to MU set must be three percent, or one MU, whichever is 6 greater. This requirement applies for all arcs of 45 degrees or 7 more at all MU/degree values indicated as "clinically usable" by 8 the manufacturer. 9

10 Subp. 17. Absorbed dose rate. Systems installed after the 11 effective date of this chapter must have a component from which 12 readings of the absorbed dose rate at a reference point in the 13 treatment volume can be calculated. The radiation detectors in 14 subpart 7 may form a portion of this system. The requirements 15 in items A and B also apply.

A. The dose monitor unit rate must be displayed atthe treatment control panel.

18 в. If the system can deliver under any conditions an absorbed dose rate at the nominal treatment distance of more 19 20 than ten percent above the value specified by the manufacturer 21 for any equipment parameters used, a device must be provided 22 which terminates irradiation when the absorbed dose rate exceeds a value twice the specified maximum. The value at which the 23 irradiation will be terminated must be in a record maintained by 24 ۰ چ 25 the registrant.

Subp. 18. <u>Source</u> location of-virtual-source-and-beam orientation. The registrant shall-determine,-or-obtain-from-the manufacturer,-the-location,-with-reference-to-an-accessible point-on-the-radiation-head,-of <u>must</u>:

30 A. the-x-ray-target-or-the-virtual-source-of 31 electrons for all photon energies, verify that the location of 32 the x-ray source is within one centimeter of expected location; 33 and

B. the-electron-window-or-the-virtual-source-of
electrons-if-the-system-has-electron-beam-capabilities if
planning to treat with electrons at any distance other than the

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nominal treatment distance, determine the virtual SSD for all electron energies and collimators which will be used for nonstandard SSD treatments. Alternatively, the registrant must elect to measure the correction needed for each patient's treatment, this measurement being done within two working days

6 of the first treatment.

7 Subp. 19. System checking facilities. Capabilities shall 8 be provided so all radiation safety interlocks can be checked 9 for correct operation. When preselection of any of the 10 operating conditions requires action in the treatment room and 11 at the treatment control panel, selection at one location shall not give a display at the other location until the requisite 12 13 selected operations in both locations have been completed. Subp. 20. Operating procedures. Any therapy system with 14 energies greater than one $Me \forall MV$ shall not be used in the 15 administration of radiation therapy unless the requirements of 16 parts 4730.1670,-subpart-4; 4730.1675, subpart 3; and 4730.1680, 17 subpart 2, have been met. 18

19 4730.2475 RADIATION SAFETY REQUIREMENTS FOR THE USE OF MEDICAL20 PARTICLE ACCELERATORS.

Subpart 1. Applicability. In addition to the requirements of parts 4730.0100 to 4730.1695, this part applies to medical particle accelerators used in the treatment of humans.

24 Subp. 2. Medical committee to evaluate and approve medical 25 particle accelerators. The registrant shall appoint a medical 26 committee of at least three four members to evaluate and approve 27 uses of a medical particle accelerator for diagnosis, research, 28 and-therapy on a person. Membership of the committee must include the facility radiation safety officer and, a physician 29 30 expert in therapeutic radiology, and a therapeutic radiological physicist. Membership may include physicians who are experts in 31 32 internal medicine and hematology.

33 Subp. 3. Controls and interlock systems. All medical 34 particle accelerators used in the treatment of humans must meet 35 the requirements for controls and interlock systems in this

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1 subpart.

A. Instrumentation, readouts, and controls on the medical particle accelerator control console must be clearly identified and easily discernible.

B. Each entrance into a treatment room or other high
radiation area must be provided with a safety interlock that
shuts down the system under conditions of barrier penetration.

8 C. Each safety interlock must be on a circuit which
9 allows it to operate independently of all other safety
10 interlocks.

D. All safety interlocks must be designed so any defect or component failure in the safety interlock system prevents operation of the medical particle accelerator.

E. When a safety interlock system has been triggered, it must be possible to resume operation of the medical particle accelerator only by manually resetting controls at the position where the safety interlock has been tripped and, lastly, at the main control console.

F. Emergency "off" switches must be placed on <u>or near</u> the treatment console and-on-a-wall-outside-the-treatment-room. Inside the treatment room, emergency "off" switches must be placed on <u>or near</u> the treatment couch, on-walls-to-the-right-and left-of-the-couch,-in-front-of-the-primary-beam, and in <u>on or</u> <u>near both sides of</u> the gantry stand.

25 Subp. 4. Warning devices. All medical particle 26 accelerators used in the treatment of humans must meet the 27 requirements for warning devices in this subpart.

A. Each location designated as high radiation area, and each entrance to such location, must be equipped with easily observable warning lights that operate when, and only when, radiation is produced.

32 B. Barriers and pathways leading to high radiation 33 areas must be posted according to part 4730.0300.

34 Subp. 5. Operating procedures. All medical particle 35 accelerators used in the treatment of humans must be operated 36 according to the procedures in this subpart.

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1 Α. Medical particle accelerators, when not in 2 operation, must be secured to prevent unauthorized use. B. All safety and warning devices, including 3 4 interlocks, must be checked for proper operation at intervals not to exceed one month. Results of such tests must be recorded 5 in writing and be available at the medical particle accelerator 6 facility for inspection by the commissioner. These records must 7 be maintained until the next inspection by the commissioner. 8 9 Electrical circuit diagrams of the medical с. 10 particle accelerator and the associated safety interlock systems 11 must be kept current and maintained for inspection by the 12 commissioner and the operator at each medical particle accelerator facility. 13 14 D. If, for any reason, it is necessary to intentionally bypass a safety interlock or interlocks when 15 treating a patient, such action must require: 16 17 (1) prior authorization by the radiation safety committee or radiation safety officer or individuals given such 18 19 authorization in writing by the radiation safety officer; 20 (2) a record in a permanent log and a notice 21 posted at the medical particle accelerator control console; and 22 (3) termination as soon as possible. 23 Ε. A copy of the current operating and the emergency 24 procedures must at all times be available at the medical particle accelerator control panel. 25 4730.2500 INDUSTRIAL X-RAY INSTALLATIONS. 26 27 [For text of subps 1 and 2, see M.R.] 28 Subp. 3. Class A operating and emergency procedures. In 29 Class A installations: A. A written manual of operating and emergency 30 procedures shall be in the possession of the operator and the 31 32 person responsible for each installation. The operating 33 procedures shall be so designed that every practicable means 34 have been employed to minimize exposure and that no person is 35 likely to be exposed to radiation doses that exceed the maximum

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08/01/91 [REVISOR] LMB/BD AR1543 permissible doses specified in parts 4730.0310 to 4730.0380. 1 2 [For text of items B to E, see M.R.] 3 [For text of subps 4 to 8, see M.R.] 4730.2600 RADIUM USE IN HEALING ARTS. 4 Subpart 1. Requirements. The following special provisions 5 of this part apply to all registrants who use radium in the 6 healing arts and are in addition to, and not in substitution 7 for, other applicable provisions of this chapter. 8 9 [For text of subps 2 to 7, see M.R.] 10 Subp. 8. Procedure. The registrant shall ensure that: 11 [For text of item A, see M.R.] 12 в. The patient's room shall be identified as a 13 radiation area and all individuals entering the room shall comply with the requirements of part 4730.1510. 14 15 [For text of items C and D, see M.R.] Loss of radium sources shall be reported to the 16 Ε. commissioner of health according to parts 4730.1110 to 4730.1140. 17 18 [For text of subp 9, see M.R.] 4730.2700 RADIUM USED FOR INDUSTRIAL PURPOSES. 19 20 [For text of subps 1 to 3, see M.R.] 21 Subp. 4. Leak tests. Sources shall have leak tests performed as follows: 22 23 [For text of items A to E, see M.R.] 24 Leaking or lost sources shall be reported to the F. commissioner of health according to parts 4730.1110 to 4730.1140. 25 [For text of subp 5, see M.R.] 26 4730.2900 SPECIAL USES OF ELECTRIC EQUIPMENT. 27 28 Subpart 1. Accelerators, x-ray diffraction systems, and 29 electron microscopes. Accelerators, x-ray diffraction systems, 30 and electron microscopes shall be installed, shielded, and 31 operated in such a manner that no one shall be exposed beyond the appropriate limits specified in part 4730.0310. 32 [For text of subp 2, see M.R.] 33 Subp. 3. Research and teaching institutions. 34 The

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following special provisions of this part apply to all 1 registrants who use ionizing radiation in research and teaching 2 institutions and are in addition to, and not in substitution 3 for, other applicable provisions of this chapter: 4 5 [For text of items A and B, see M.R.] 6 c. Students under 18 years of age shall not receive in any period of one calendar quarter a whole body exposure 7 exceeding ten percent of the limits specified in parts 4730.0310 8 and 4730.0360. 9

10 4730.3605 CONCENTRATIONS IN AIR AND WATER ABOVE NATURAL 11 BACKGROUND.

12			Table	I	Table	II
13	Isotope	1	Column 1	Column 2	Column 1	Column 2
14			Air	Water	Air	Water
15			(µCi/ml)	(µCi/ml)	(µCi/ml)	(µCi/ml)
16						
17			A. Actinium	(89):		
18	Ac-227	S	2X10 ⁻¹²	6X10 ⁻⁵	8x10 ⁻¹⁴	2X10 ⁻⁶
19		I	3X10 ⁻¹¹	9X10 ⁻³	9X10 ⁻¹³	3X10 ⁻⁴
20	Ac-228	s	8X10 ⁻⁸	3X10 ⁻³	3X10 ⁻⁹	9x10 ⁻⁵
21		I	2X10 ⁻⁸	3X10 ⁻³	6X10 ⁻¹⁰	9X10 ⁻⁵
22			B. Americium	n (95):		
23	Am-241	s	6X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10-6
24		I	1X10 ⁻¹⁰	8X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
25	Am- 242m	S	6X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10 ⁻⁶
26		I	3X10 ⁻¹⁰	3X10 ⁻³	9X10 ⁻¹²	9x10 ⁻⁵
27	Am-242	s	4x10 ⁻⁸	4X10 ⁻³	1X10 ⁻⁹	1X10 ⁻⁴
28		I	5X10 ⁻⁸	4X10 ⁻³	2X10 ⁻⁹	1X10 ⁻⁴
29	Am-243	s	6X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10 ⁻⁶
30		I	1X10 ⁻¹⁰	8X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
31	Am-244	s	4x10 ⁻⁶	1X10 ⁻¹	1X10 ⁻⁷	5X10 ⁻³
3 2		I	2X10 ⁻⁵	1X10 ⁻¹	8x10 ⁻⁷	5X10 ⁻³

33

C. Antimony (51):

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1	Sb-122	S	2X10 ⁻⁷	8X10 ⁻⁴	6X10 ⁻⁹	3X10 ⁻⁵
2		I	1X10 ⁻⁷	8X10 ⁻⁴	5x10 ⁻⁹	3 X10⁻⁵
3	Sb-124	s	2X10 ⁻⁷	7X10 ⁻⁴	5x10 ⁻⁹	2x10 ⁻⁵
4		I	2X10 ⁻⁸	7X10 ⁻⁴	7X10 ⁻¹⁰	2x10 ⁻⁵
5	Sb-125	S	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
6		I	3X10 ⁻⁸	3X10 ⁻³	9X10 ⁻¹⁰	1X10 ⁻⁴
7			D Argon (70).		
/ Q	Ar-37		D. Argon (.	18):		
0	AI-57	ь2	C¥103			
10	54	.D	6x10-3		1 X1 0 - 4	
11	AR-11 S	uh	2210-6		1×10	
ΤT	AK 41 3	ub	2810		4X10	
12			E. Arsenic	(33):	,	
13	As-73	S	2X10 ⁻⁶	1X10 ⁻²	7X10 ⁻⁸	5X10 ⁻⁴
14		I	4X10 ⁻⁷	1X10 ⁻²	1X10 ⁻⁸	5X10 ⁻⁴
15	As-74	S	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	5X10 ⁻⁵
16		I	1X10 ⁻⁷	2X10 ⁻³	4x10 ⁻⁹	5X10 ⁻⁵
17	As-76	S	1X10 ⁻⁷	6X10 ⁻⁴	4x10 ⁻⁹	2X10 ⁻⁵
18		I	1X10 ⁻⁷	6X10 ⁻⁴	3X10 ⁻⁹	2X10 ⁻⁵
19	As-77	S	5X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	8X10 ⁻⁵
20		I	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	8X10 ⁻⁵
21			F. Astatine	e (85):		
22	At-211	S	7X10 ⁻⁹	5x10 ⁻⁵	2X10 ⁻¹⁰	2X10 ⁻⁶
23		I	3X10 ⁻⁸	2X10 ⁻³	1X10 ⁻⁹	7X10 ⁻⁵
24						
24	Ba-131	c	uvin-6	50): EV10-3	4810-8	2810-4
25	ba-131	э т	4810-7	5×10 ⁻³	4X10 -8	$2X10^{-4}$
20	Ba-140	⊥ c	4x10	ovio-4	1X10 ⁻⁹	2×10-5
27 28	Ba-140	ы т	4×10-8	7×10-4	4X10	2×10 ⁻⁵
20		Ŧ	4710	/X10	IXIO	2810
29]	H. Berkeliu	um (97):		
30	Bk-249	S	9X10 ⁻¹⁰	2X10 ⁻²	3X10 ⁻¹¹	6X10 ⁻⁴
31		I	1X10 ⁻⁷	2X10 ⁻²	4X10 ⁻⁹	6X10 ⁻⁴
32	Bk-250	S	1X10 ⁻⁷	6X10 ⁻³	5x10 ⁻⁹	2X10 ⁻⁴
33		I	1X10 ⁻⁶	6x10 ⁻³	4×10^{-8}	2×10^{-4}

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1			I. Berylli	um (4):		
2	Be-7	S	6X10 ⁻⁶	5x10 ⁻²	2X10 ⁻⁷	2x10 ⁻³
3		I	1X10 ⁻⁶	5X10 ⁻²	4X10 ⁻⁸	2X10 ⁻³
4			J. Bismuth	a (83):		
5	Bi-206	S	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	4x10 ⁻⁵
6		I	1X10 ⁻⁷	1X10 ⁻³	5X10 ⁻⁹	4x10 ⁻⁵
7	Bi-207	S	2X10 ⁻⁷	2x10 ⁻³	6X10 ⁻⁹	6x10 ⁻⁵
8		I	1X10 ⁻⁸	2X10 ⁻³	5X10 ⁻¹⁰	6x10 ⁻⁵
9	Bi-210	S	6x10 ⁻⁹	1X10 ⁻³	2X10 ⁻¹⁰	4x10 ⁻⁵
10		I	6X10 ⁻⁹	1X10 ⁻³	2X10 ⁻¹⁰	4X10 ⁻⁵
11	Bi-212	S	1X10 ⁻⁷	1X10 ⁻²	3X10 ⁻⁹	4×10^{-4}
12		I	2X10 ⁻⁷	1X10 ⁻²	7x10 ⁻⁹	4×10^{-4}
13			K. Bromine	(35):		
14	Br-82	S	1X10 ⁻⁶	8X10 ⁻³	4X10 ⁻⁸	3X10 ⁻⁴
15		I	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	4x10 ⁻⁵
16			L. Cadmium	(48):		
17	Cd-109	S	5X10 ⁻⁸	5X10 ⁻³	2X10 ⁻⁹	2x10 ⁻⁴
18		I	7X10 ⁻⁸	5X10 ⁻³	3X10 ⁻⁹	2X10 ⁻⁴
19	Cd-115m	s	4X10 ⁻⁸	7X10 ⁻⁴	1X10 ⁻⁹	3X10 ⁻⁵
20		I	4X10 ⁻⁸	7X10 ⁻⁴	1X10 ⁻⁹	3X10 ⁻⁵
21	Cd-115	S	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	3X10 ⁻⁵
22		I	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	4X10 ⁻⁵
23		j	M. Calcium	(20):		
24	Ca-45 ,	S	3X10 ⁻⁸	3X10 ⁻⁴	1X10 ⁻⁹	9x10 ⁻⁶
25		I	1X10 ⁻⁷	5X10 ⁻³	4X10 ⁻⁹	2X10 ⁻⁴
26	Ca-47	S	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	5X10 ⁻⁵
27		I	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	3X10 ⁻⁵
28]	N. Califor:	nium (98):		
29	Cf-249	S	2X10 ⁻¹²	1X10 ⁻⁴	5X10 ⁻¹⁴	4X10 ⁻⁶
30		I	1X10 ⁻¹⁰	7X10 ⁻⁴	3X10 ⁻¹²	2X10 ⁻⁵
31	C£-250	s	5X10 ⁻¹²	4×10^{-4}	2X10 ⁻¹³	1X10 ⁻⁵
32		I	1X10 ⁻¹⁰	7X10 ⁻⁴	3X10 ⁻¹²	3X10 ⁻⁵
33	Cf-251	s	2X10 ⁻¹²	$l \times l 0^{-4}$	6X10 ⁻¹⁴	4X10 ⁻⁶

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l		I	1X10-10	8x10 ⁻⁴	3X10 ⁻¹	2 _{3X10} -5	
2	Cf-252	S	6X10 ⁻¹²	2X10 ⁻⁴	2X10 ⁻¹	3 _{7X10} -6	
3		I	3X10 ⁻¹¹	2X10 ⁻⁴	1X10 ⁻¹	2 _{7X10} -6	
4	Cf-253	S	8X10 ⁻¹⁰	4x10 ⁻³	3X10 ⁻¹	l 1x10 ⁻⁴	
5		I	8X10 ⁻¹⁰	4x10 ⁻³	3X10 ⁻¹	1 1x10 ⁻⁴	
6	Cf-254	S	5X10 ⁻¹²	4X10-6	2X10 ⁻¹	3 1X10 ⁻⁷	
7		I	5X10 ⁻¹²	4X10-6	2X10 ⁻¹	3 1X10 ⁻⁷	
0		~	Carbon	(6).			
0	C-14	e C	$A_{V10}-6$	(b):	1 1 1 0 - 7	0110-4	
ע 10		5 h2	4A10 -5	2810 -	1X10 ×	8XI0 -	
τu	CO2 Su	D	JYT0		IXIO C		
11		F	. Cerium	(58):			
12	Ce-141	S	4X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	9X10 ⁻⁵	
13		I	2X10 ⁻⁷	3X10 ⁻³	5X10 ⁻⁹	9x10 ⁻⁵	
14	Ce-143	S	3X10 ⁻⁷	1X10 ⁻³	9x10 ⁻⁹	4X10 ⁻⁵	
15		I	2X10 ⁻⁷	1X10 ⁻³	7X10 ⁻⁹	4x10 ⁻⁵	
16	Ce-144	S	1X10 ⁻⁸	3X10 ⁻⁴	3X10 ⁻¹	0 _{1X10} -5	
17		I	6X10 ⁻⁹	3X10 ⁻⁴	2X10 ⁻¹	0 _{1X10} -5	
18		Q	. Cesium	(55):			
19	Cs-131	S	1X10 ⁻⁵	7X10 ⁻²	4X10 ⁻⁷	2X10 ⁻³	
20		I	3X10-6	3X10 ⁻²	1X10-7	9x10 ⁻⁴	
21	Cs-134m	S	4X10 ⁻⁵	2X10 ⁻¹	1X10-6	6x10 ⁻³	
22		I	6X10-6	3X10 ⁻²	2X10 ⁻⁷	1X10 ⁻³	
23	Cs-134	S	4x10 ⁻⁸	3X10 ⁻⁴	1X10 ⁻⁹	9X10-6	
24		I	1X10 ⁻⁸	1X10 ⁻³	4X10 ⁻¹⁰	0 4x10 ⁻⁵	
25	Cs-135	S	5X10 ⁻⁷	3X10-3	2X10 ⁻⁸	1X10 ⁻⁴	
26		I	9x10 ⁻⁸	7X10 ⁻³	3X10 ⁻⁹	2x10 ⁻⁴	
27	Cs-136	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	9x10 ⁻⁵	
28		I	2X10 ⁻⁷	2X10 ⁻³	6x10 ⁻⁹	6x10 ⁻⁵	
29	Cs-137	S	6x10 ⁻⁸	4X10 ⁻⁴	2x10 ⁻⁹	2x10 ⁻⁵	
30		I	1X10 ⁻⁸	1X10 ⁻³	5x10 ⁻¹⁰	4×10^{-5}	
31		D	Chlorin	a (17).			
ער ער	C 1-36	c r	4x10 ⁻⁷	2v10-3	1 21 0 - 8	8v10-5	
22		T	2v10-8	2AIU 2VIA-3) $\epsilon_{v10} = 5$	
27	C1-29	T C	2x10-6	2AIU - 1V10-2	0×10-8		
7.4	CT-20	5	JATO .	TVTO	JATO -	4ALU	

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1		I	2X10 ⁻⁶	1X10 ⁻²	7X10 ⁻⁸	4X10 ⁻⁴
2			S. Chromiu	ım (24):		
3	Cr-51	s	1X10 ⁻⁵	5X10 ⁻²	4x10 ⁻⁷	2X10 ⁻³
4		I	2X10 ⁻⁶	5x10 ⁻²	8X10 ⁻⁸	2X10 ⁻³
5			T. Cobalt	(27):		
6	Co-57	s	3X10-6	2X10 ⁻²	1X10 ⁻⁷	5X10 ⁻⁴
7		I	2X10 ⁻⁷	1X10 ⁻²	6X10 ⁻⁹	4X10 ⁻⁴
8	Co-58m	s	2X10 ⁻⁵	8X10 ⁻²	6X10 ⁻⁷	3X10 ⁻³
9		I	9X10-6	6X10 ⁻²	3X10 ⁻⁷	2X10 ⁻³
10	Co-58	s	8x10 ⁻⁷	4x10 ⁻³	3X10 ⁻⁸	1X10 ⁻⁴
11		I	5X10 ⁻⁸	3X10 ⁻³	2X10 ⁻⁹	9X10 ⁻⁵
12	Co-60	S	3X10 ⁻⁷	1X10 ⁻³	1X10 ⁻⁸	5X10 ⁻⁵
13		I	9x10 ⁻⁹	1X10 ⁻³	3X10-10	3X10 ⁻⁵
14			U. Copper	(29):		
15	Cu-64	s	2X10 ⁻⁶	1X10 ⁻²	7X10 ⁻⁸	3X10 ⁻⁴
16		I	1X10 ⁻⁶	6X10 ⁻³	4X10 ⁻⁸	2X10 ⁻⁴
17			V. Curium	(96):		
18	Cm-242	s	1X10 ⁻¹⁰	7X10 ⁻⁴	4X10 ⁻¹²	2X10 ⁻⁵
19		I	2X10 ⁻¹⁰	7X10 ⁻⁴	6X10 ⁻¹²	2X10 ⁻⁵
20	Cm-243	s	6X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	5X10 ⁻⁶
21		I	1X10 ⁻¹⁰	7X10 ⁻⁴	3X10 ⁻¹²	2X10 ⁻⁵
22	Cm-244	s	9X10 ⁻¹²	2X10 ⁻⁴	3X10 ⁻¹³	7X10 ⁻⁶
2 3		I	1X10 ⁻¹⁰	8x10 ⁻⁴	3X10 ⁻¹²	3X10 ⁻⁵
24,	Cm-245	s	5X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10 ⁻⁶
25		I	1X10 ⁻¹⁰	8X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
26	Cm-246	s	5X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10 ⁻⁶
27		I	1X10 ⁻¹⁰	8X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
28	Cm-247	s	5X10 ⁻¹²	1X10 ⁻⁴	2X10 ⁻¹³	4X10 ⁻⁶
29		I	1X10-10	6X10 ⁻⁴	4X10 ⁻¹²	2X10 ⁻⁵
30	Cm-248	s	6X10 ⁻¹³	1X10 ⁻⁵	2X10 ⁻¹⁴	4X10 ⁻⁷
31		I	1X10 ⁻¹¹	4X10 ⁻⁵	4X10 ⁻¹³	1X10 ⁻⁶
3 2	Cm-249	s	1X10 ⁻⁵	6X10 ⁻²	4X10 ⁻⁷	2X10 ⁻³
33		I	1X10 ⁻⁵	6X10 ⁻²	4X10 ⁻⁷	2X10 ⁻³

Approved by Revisor _

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l		V	N. Dysprosium	(66):		
2	Dy-165	S	3 X 10 ⁻⁶	1X10 ⁻²	9X10 ⁻⁸	4×10^{-4}
3		I	2X10 ⁻⁶	1X10 ⁻²	7X10 ⁻⁸	4×10^{-4}
4	Dy-166	S	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	4X10 ⁻⁵
5		I	2X10 ⁻⁷	1X10 ⁻³	7X10 ⁻⁹	4X10 ⁻⁵
б		Х	. Einsteinium	n (99):		
7	Es-25 3	S	8X10 ⁻¹⁰	7×10^{-4}	3X10 ⁻¹¹	2×10^{-5}
8		I	6X10-10	7X10 ⁻⁴	2X10 ⁻¹¹	2×10^{-5}
9	Es-254m	s	5x10 ⁻⁹	5×10^{-4}	2x10 ⁻¹⁰	2x10 ⁻⁵
10		I	6X10 ⁻⁹	5X10 ⁻⁴	2x10 ⁻¹⁰	2x10 ⁻⁵
11	Es-254	S	2X10 ⁻¹¹	4X10 ⁻⁴	6X10 ⁻¹³	1x10 ⁻⁵
12		I	1X10-10	4×10^{-4}	4X10 ⁻¹²	1x10 ⁻⁵
13	Es-255	S	5X10 ⁻¹⁰	8X10 ⁻⁴	2X10 ⁻¹¹	3x10 ⁻⁵
14		I	4X10 ⁻¹⁰	8X10 ⁻⁴	1X10 ⁻¹¹	3X10 ⁻⁵
15		Y	. Erbium (68)	:		
16	Er-169	S	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	9X10 ⁻⁵
17		I	4X10 ⁻⁷	3 X10⁻³	1X10 ⁻⁸	9X10 ⁻⁵
18	Er-171	S	7X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
19		I	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
20		Z	. Europium (6	<i>(3)</i> :		
21	Eu-152	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
22	(Tr=9.2					
2 3	hrs)	S	3X10-7	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
24	Eu-152	S	1X10 ⁻⁸	2X10 ⁻³	4X10 ⁻¹⁰	8X10 ⁻⁵
25	(Tr=13					
26	yrs)	I	2X10 ⁻⁸	2X10 ⁻³	6X10 ⁻¹⁰	8X10 ⁻⁵
27	Eu-154	S	4X10 ⁻⁹	6X10 ⁻⁴	1X10 ⁻¹⁰	2X10 ⁻⁵
28		I	7X10 ⁻⁹	6X10 ⁻⁴	2X10 ⁻¹⁰	2X10 ⁻⁵
29	Eu-155	S	9X10 ⁻⁸	6X10 ⁻³	3X10 ⁻⁹	2x10 ⁻⁴
30		I	7X10 ⁻⁸	6X10 ⁻³	3X10 ⁻⁹	2X10 ⁻⁴
31		A	A. Fermium (1	00):	-	
3 2	Fm-254	S	6X10 ⁻⁸	4X10 ⁻³	2X10 ⁻⁹	1X10 ⁻⁴
33		I	7X10 ⁻⁸	4X10 ⁻³	2X10 ⁻⁹	1X10 ⁻⁴
34	Fm-255	S	2X10 ⁻⁸	1X10 ⁻³	6X10 ⁻¹⁰	3X10 ⁻⁵

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	08/01/9	91			[REVISOR] LMB/BD	AR1543
1		I	1X10 ⁻⁸	1X10 ⁻³	4X10 ⁻¹⁰	3X10 ⁻⁵
2	Fm-256	S	3X10 ⁻⁹	3X10 ⁻⁵	1X10 ⁻¹⁰	9X10 ⁻⁷
3		I	2X10 ⁻⁹	3X10 ⁻⁵	6X10 ⁻¹¹	9X10 ⁻⁷
			~~ ~1 (
4		_	BB. Fluorin	e (9):	-7	- 1
5	F,-T8	S	5X10 0	2X10 ⁻²	2X10 7	8X10 ⁻⁴
6		I	3X10 0	1X10 ⁻²	9X10 ⁻⁸	5X10 ⁻⁴
7			CC. Gadolin	ium (64):		
8	Gd-153	s	2X10 ⁻⁷	6X10 ⁻³	8x10 ⁻⁹	2X10 ⁻⁴
9		I	9X10 ⁻⁸	6X10 ⁻³	3X10 ⁻⁹	2X10 ⁻⁴
10	Gd-159	s	5X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	8x10 ⁻⁵
11		I	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	8X10 ⁻⁵
12			DD. Gallium	(31):	0	-
13	Ga-72	S	2X10-7	1X10 ⁻³	8X10 ⁻⁹	4X10 ⁻⁵
14		I	2X10-7	1X10 ⁻³	8X10 ⁻⁹	4X10 ⁻⁵
15			EE. Germani:	um (32):		
16	Ge-68*	s	4X10 ⁻⁶	2X10 ⁻²	1X10 ⁻⁷	8X10 ⁻⁴
17		I	1X10 ⁻⁸		5X10 ⁻¹⁰	
18	Ge-71	S	1X10 ⁻⁵	5X10 ⁻²	4X10 ⁻⁷	2X10 ⁻³
19		I	6X10 ⁻⁶	5X10 ⁻²	2X10 ⁻⁷	2X10 ⁻³
20			FF. Gold (79	9):	_	2
21	Au-195*	S	8X10 ⁻⁶	4X10 ⁻²	3X10 ⁻⁷	1X10 ⁻³
22		I	6X10 ⁻⁸	6X10 ⁻³	2X10 ⁻⁹	2X10 ⁻⁴
23	Au-196	S	1X10 ⁻⁶	5X10 ⁻³	4X10 ⁻⁸	2X10 ⁻⁴
24		I	6X10 ⁻⁷	4X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
25	Au-198	S	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	5X10 ⁻⁵
26		I	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	5X10 ⁻⁵
2 7	Au-199	S	1X10 ⁻⁶	5X10 ⁻³	4X10 ⁻⁸	2X10 ⁻⁴
28		I	8X10 ⁻⁷	4×10^{-3}	3X10 ⁻⁸	2X10 ⁻⁴
20			CC Hafnium	(72).		
20	¥F-191	c	1V10-8	2210-3	1×10 ⁻⁹	7 V 10 ⁻⁵
50	TT TOT	ы т	4ALU 7V1 A-8	2ALU 2V1 A-3	9	7810-5
JΤ		Ŧ	/X10 -	ZXIU	JXIU -	XIU S
32			HH. Holmium	(67):		

1Ho-166S 2×10^{-7} 9×10^{-4} 7×10^{-9} 3×10^{-5} 2I 2×10^{-7} 9×10^{-4} 6×10^{-9} 3×10^{-5} 3II. $Hydrogen (1):$ 2×10^{-7} 3×10^{-3} 4H-3S 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 5I 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 6Sub ² 2×10^{-3} $$ 4×10^{-7} 3×10^{-3} 7JJ.Indium (49):8In-113m S 8×10^{-6} 4×10^{-2} 3×10^{-7} 1×10^{-3} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10In-114m S 1×10^{-7} 5×10^{-4} 7×10^{-10} 2×10^{-5} 11I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 14In-115S 2×10^{-7} 3×10^{-3} 1×10^{-9} 8×10^{-7} 16KK.Iodine (53):I 1×10^{-7} 3×10^{-7} 3×10^{-7} 18I 2×10^{-7} 5×10^{-5} 9×10^{-11} 3×10^{-7} 20I 3×10^{-7} 3×10^{-3} 2×10^{-11} 3×10^{-7} 21I-129S $2 \times 10^{-$
2I 2×10^{-7} 9×10^{-4} 6×10^{-9} 3×10^{-5} 3II. Hydrogen (1):4H-3S 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 5I 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 6 $S ub^2$ 2×10^{-3} $$ 4×10^{-5} $$ 7JJ. Indium (49):8In-113m S 8×10^{-6} 4×10^{-2} 3×10^{-7} 8In-113m S 8×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10In-114m S 1×10^{-7} 5×10^{-4} 4×10^{-9} 2×10^{-5} 11I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13I 2×10^{-6} 1×10^{-2} 6×10^{-8} 4×10^{-4} 14In-115 S 2×10^{-7} 3×10^{-3} 9×10^{-5} 8×10^{-10} 15I 3×10^{-7} 3×10^{-3} 1×10^{-9} 8×10^{-7} 16KK. Iodine (53):I 1×10^{-7} 3×10^{-7} 3×10^{-7} 16I 2×10^{-7} 3×10^{-7} 3×10^{-7} 3×10^{-7} 16I 2×10^{-7} 3×10^{-5} 9×10^{-7} 17I-126 S 8×10^{-9} 5×10^{-5} 9×10^{-7} 20I 3×10^{-7} 3×10^{-5} 2×10^{-11} </td
3 II. Hydrogen (1): 4 H-3 S 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 5 I 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 6 Sub ² 2×10^{-3} $$ 4×10^{-7} 3×10^{-3} 7 JJ. Indium (49): 4×10^{-5} 8 In-113m S 8×10^{-6} 4×10^{-2} 3×10^{-7} 1×10^{-3} 9 I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10 In-114m S 1×10^{-7} 5×10^{-4} 4×10^{-9} 2×10^{-5} 11 I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13 I 2×10^{-6} 1×10^{-2} 6×10^{-8} 4×10^{-4} 14 In-115 S 2×10^{-7} 3×10^{-3} 9×10^{-5} 8×10^{-4} 14 In-115 S 5×10^{-9} 4×10^{-5} 8×10^{-11} 2×10^{-7} 15 I 3×10^{-7} <
3II.Hydrogen (1):4H-3S 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 5I 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 6Sub ² 2×10^{-3} 4×10^{-5} 7JJ.Indium (49):8In-113m S 8×10^{-6} 4×10^{-2} 3×10^{-7} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10In-114m S 1×10^{-7} 5×10^{-4} 4×10^{-9} 2×10^{-5} 11I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 14In-115S 2×10^{-7} 3×10^{-3} 9×10^{-9} 8×10^{-5} 16KK.Iodine (53):I 1×10^{-7} 8×10^{-7} 8×10^{-7} 18I 2×10^{-7} 5×10^{-9} 8×10^{-5} 9×10^{-7} 20I 3×10^{-9} 5×10^{-9} 2×10^{-7} 6×10^{-3} 21I-129S 2×10^{-9} 1×10^{-5} 2×10^{-11} 6×10^{-7} 24I 3×10^{-9} 6×10^{-5} 1×10^{-8} 6×10^{-5} 25I-132S 2×10^{-7} 2×10^{-3} 3×10^{-9} 8×10^{-6} <
4H=3S 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 5I 5×10^{-6} 1×10^{-1} 2×10^{-7} 3×10^{-3} 6 Sub^2 2×10^{-3} $$ 4×10^{-5} $$ 7JJ.Indium (49):8In-113m S 8×10^{-6} 4×10^{-2} 3×10^{-7} 9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10In-114m S 1×10^{-7} 5×10^{-4} 4×10^{-9} 2×10^{-5} 11I 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13I 2×10^{-6} 1×10^{-2} 6×10^{-8} 4×10^{-4} 14In-115 S 2×10^{-7} 3×10^{-3} 9×10^{-9} 9×10^{-5} 15I 3×10^{-7} 3×10^{-3} 9×10^{-9} 8×10^{-5} 16KK.Iodine (53):I 1×10^{-8} 9×10^{-7} 18I 2×10^{-7} 6×10^{-3} 6×10^{-9} 2×10^{-4} 19I-126S 8×10^{-9} 5×10^{-5} 9×10^{-11} 3×10^{-7} 20I 3×10^{-7} 3×10^{-3} 1×10^{-8} 9×10^{-5} 21I-129S 2×10^{-9} 1×10^{-5} 2×10^{-11} 6×10^{-8} 22I 7×10^{-8} 6×10^{-5} 1×10^{-10} 3×10^{-7} 24I 3×10^{-7} 2×10^{-3} 1×10^{-8} 6×10^{-5} 25I-132S 2×10^{-7} 2×10^{-3} 3×10^{-9
5 1 $5X10^{-7}$ $1X10^{-1}$ $2X10^{-7}$ $3X10^{-3}$ 6 Sub^2 $2X10^{-3}$ $4X10^{-5}$ 7 JJ. Indium (49): 8 In-113m S $8X10^{-6}$ $4X10^{-2}$ $3X10^{-7}$ $1X10^{-3}$ 9 I $7X10^{-6}$ $4X10^{-2}$ $2X10^{-7}$ $1X10^{-3}$ 10 In-114m S $1X10^{-7}$ $5X10^{-4}$ $4X10^{-9}$ $2X10^{-5}$ 11 I $2X10^{-8}$ $5X10^{-4}$ $7X10^{-10}$ $2X10^{-5}$ 12 In-115m S $2X10^{-6}$ $1X10^{-2}$ $8X10^{-8}$ $4X10^{-4}$ 13 I $2X10^{-6}$ $1X10^{-2}$ $6X10^{-8}$ $4X10^{-4}$ 14 In-115 S $2X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $9X10^{-5}$ 15 I $3X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $8X10^{-7}$ 16 KK. Iodine (53): In-125 S $5X10^{-9}$ $9X10^{-11}$ $3X10^{-7}$ 19 I-126 S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$
3 3 2 2 4 4 3 $$ 7 JJ . Indium (49): 3 3 10 $1n-113m$ S $8x10^{-6}$ $4x10^{-2}$ $3x10^{-7}$ $1x10^{-3}$ 9 I $7x10^{-6}$ $4x10^{-2}$ $2x10^{-7}$ $1x10^{-3}$ 10 $In-114m$ S $1x10^{-7}$ $5x10^{-4}$ $4x10^{-9}$ $2x10^{-5}$ 11 I $2x10^{-8}$ $5x10^{-4}$ $7x10^{-10}$ $2x10^{-5}$ 12 $In-115m$ S $2x10^{-6}$ $1x10^{-2}$ $8x10^{-8}$ $4x10^{-4}$ 13 I $2x10^{-6}$ $1x10^{-2}$ $6x10^{-8}$ $4x10^{-4}$ 14 $In-115$ S $2x10^{-6}$ $1x10^{-2}$ $6x10^{-8}$ $4x10^{-4}$ 14 $In-115$ S $2x10^{-7}$ $3x10^{-3}$ $9x10^{-5}$ $8x10^{-11}$ $2x10^{-7}$ 15 I $3x10^{-7}$ $6x10^{-3}$ $8x10^{-11}$ $2x10^{-7}$ 16 KK . $Iodine$ (53): I I $2x10^{-7}$ $8x10^{-11}$ $3x10^{-7}$
7 JJ. Indium (49): 8 In-113m S $8x10^{-6}$ $4x10^{-2}$ $3x10^{-7}$ $1x10^{-3}$ 9 I $7x10^{-6}$ $4x10^{-2}$ $2x10^{-7}$ $1x10^{-3}$ 10 In-114m S $1x10^{-7}$ $5x10^{-4}$ $4x10^{-9}$ $2x10^{-5}$ 11 I $2x10^{-8}$ $5x10^{-4}$ $7x10^{-10}$ $2x10^{-5}$ 12 In-115m S $2x10^{-6}$ $1x10^{-2}$ $8x10^{-8}$ $4x10^{-4}$ 13 I $2x10^{-6}$ $1x10^{-2}$ $6x10^{-8}$ $4x10^{-4}$ 14 In-115 S $2x10^{-7}$ $3x10^{-3}$ $9x10^{-9}$ $9x10^{-5}$ 15 I $3x10^{-7}$ $3x10^{-3}$ $9x10^{-9}$ $8x10^{-5}$ 16 KK. <i>Iodine (53):</i> I $2x10^{-7}$ $6x10^{-3}$ $6x10^{-9}$ $2x10^{-7}$ 18 I $2x10^{-7}$ $6x10^{-3}$ $6x10^{-9}$ $2x10^{-7}$ 20 I $3x10^{-7}$ $3x10^{-3}$ $1x10^{-8}$ $9x10^{-5}$ 21 I-126 S $8x10^{-9}$ $1x10^{-5}$
8In-113m S $8X10^{-6}$ $4X10^{-2}$ $3X10^{-7}$ $1X10^{-3}$ 9I $7X10^{-6}$ $4X10^{-2}$ $2X10^{-7}$ $1X10^{-3}$ 10In-114m S $1X10^{-7}$ $5X10^{-4}$ $4X10^{-9}$ $2X10^{-5}$ 11I $2X10^{-8}$ $5X10^{-4}$ $7X10^{-10}$ $2X10^{-5}$ 12In-115m S $2X10^{-6}$ $1X10^{-2}$ $8X10^{-8}$ $4X10^{-4}$ 13I $2X10^{-6}$ $1X10^{-2}$ $6X10^{-8}$ $4X10^{-4}$ 14In-115 S $2X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $9X10^{-5}$ 15I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-9}$ $8X10^{-5}$ 16KK. Iodine (53):I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-7}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129 S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131 S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132 S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$
9I 7×10^{-6} 4×10^{-2} 2×10^{-7} 1×10^{-3} 10In-114m S 1×10^{-7} 5×10^{-4} 4×10^{-9} 2×10^{-5} 11I 2×10^{-8} 5×10^{-4} 7×10^{-10} 2×10^{-5} 12In-115m S 2×10^{-6} 1×10^{-2} 8×10^{-8} 4×10^{-4} 13I 2×10^{-6} 1×10^{-2} 6×10^{-8} 4×10^{-4} 14In-115 S 2×10^{-7} 3×10^{-3} 9×10^{-9} 9×10^{-5} 15I 3×10^{-7} 3×10^{-3} 1×10^{-9} 8×10^{-5} 16KK. Iodine (53):I 2×10^{-7} 6×10^{-3} 6×10^{-9} 18I 2×10^{-7} 6×10^{-3} 6×10^{-9} 2×10^{-7} 19I-126S 8×10^{-9} 5×10^{-5} 9×10^{-11} 3×10^{-7} 20I 3×10^{-7} 3×10^{-3} 1×10^{-8} 9×10^{-5} 21I-129S 2×10^{-9} 1×10^{-5} 2×10^{-11} 6×10^{-8} 22I 7×10^{-8} 6×10^{-3} 2×10^{-9} 2×10^{-4} 23I-131S 9×10^{-9} 6×10^{-5} 1×10^{-8} 6×10^{-5} 24I 3×10^{-7} 2×10^{-3} 3×10^{-9} 8×10^{-6} 25I-132S 2×10^{-7} 2×10^{-3} 3×10^{-9} 8×10^{-6}
10In-114m S $1X10^{-7}$ $5X10^{-4}$ $4X10^{-9}$ $2X10^{-5}$ 11I $2X10^{-8}$ $5X10^{-4}$ $7X10^{-10}$ $2X10^{-5}$ 12In-115m S $2X10^{-6}$ $1X10^{-2}$ $8X10^{-8}$ $4X10^{-4}$ 13I $2X10^{-6}$ $1X10^{-2}$ $6X10^{-8}$ $4X10^{-4}$ 14In-115 S $2X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $9X10^{-5}$ 15I $3X10^{-8}$ $3X10^{-3}$ $1X10^{-9}$ $8X10^{-5}$ 16KK.Iodine (53):I17I-125 S $5X10^{-9}$ $4X10^{-5}$ $8X10^{-11}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-4}$ 19I-126 S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129 S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-10}$ $3X10^{-7}$ 23I-131 S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132 S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$
11I $2x10^{-8}$ $5x10^{-4}$ $7x10^{-10}$ $2x10^{-5}$ 12In-115m S $2x10^{-6}$ $1x10^{-2}$ $8x10^{-8}$ $4x10^{-4}$ 13I $2x10^{-6}$ $1x10^{-2}$ $6x10^{-8}$ $4x10^{-4}$ 14In-115 S $2x10^{-7}$ $3x10^{-3}$ $9x10^{-9}$ $9x10^{-5}$ 15I $3x10^{-8}$ $3x10^{-3}$ $1x10^{-9}$ $8x10^{-5}$ 16KK. Iodine (53):I17I-125 S $5x10^{-9}$ $4x10^{-5}$ $8x10^{-11}$ $2x10^{-7}$ 18I $2x10^{-7}$ $6x10^{-3}$ $6x10^{-9}$ $2x10^{-4}$ 19I-126 S $8x10^{-9}$ $5x10^{-5}$ $9x10^{-11}$ $3x10^{-7}$ 20I $3x10^{-7}$ $3x10^{-3}$ $1x10^{-8}$ $9x10^{-5}$ 21I-129 S $2x10^{-9}$ $1x10^{-5}$ $2x10^{-11}$ $6x10^{-8}$ 22I $7x10^{-8}$ $6x10^{-3}$ $2x10^{-9}$ $2x10^{-4}$ 23I-131 S $9x10^{-9}$ $6x10^{-5}$ $1x10^{-10}$ $3x10^{-7}$ 24I $3x10^{-7}$ $2x10^{-3}$ $1x10^{-8}$ $6x10^{-5}$ 25I-132 S $2x10^{-7}$ $2x10^{-3}$ $3x10^{-9}$ $8x10^{-6}$
12In-115m S $2X10^{-6}$ $1X10^{-2}$ $8X10^{-8}$ $4X10^{-4}$ 13I $2X10^{-6}$ $1X10^{-2}$ $6X10^{-8}$ $4X10^{-4}$ 14In-115 S $2X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $9X10^{-5}$ 15I $3X10^{-8}$ $3X10^{-3}$ $1X10^{-9}$ $8X10^{-5}$ 16KK. Iodine (53):I17I-125 S $5X10^{-9}$ $4X10^{-5}$ $8X10^{-11}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-4}$ 19I-126 S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129 S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131 S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132 S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$
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14In-115S $2X10^{-7}$ $3X10^{-3}$ $9X10^{-9}$ $9X10^{-5}$ 15I $3X10^{-8}$ $3X10^{-3}$ $1X10^{-9}$ $8X10^{-5}$ 16KK. Iodine (53):17I-125S $5X10^{-9}$ $4X10^{-5}$ $8X10^{-11}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-4}$ 19I-126S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$
15I $3X10^{-8}$ $3X10^{-3}$ $1X10^{-9}$ $8X10^{-5}$ 16KK. Iodine (53):17I-125S $5X10^{-9}$ $4X10^{-5}$ $8X10^{-11}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-4}$ 19I-126S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131S $9X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$ 26I $9X10^{-7}$ $5X10^{-3}$ $2X10^{-8}$ $2X10^{-4}$
16KK. Iodine (53) :17I-125S $5X10^{-9}$ $4X10^{-5}$ $8X10^{-11}$ $2X10^{-7}$ 18I $2X10^{-7}$ $6X10^{-3}$ $6X10^{-9}$ $2X10^{-4}$ 19I-126S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$
17 $I-125$ S $5x10^{-9}$ $4x10^{-5}$ $8x10^{-11}$ $2x10^{-7}$ 18 I $2x10^{-7}$ $6x10^{-3}$ $6x10^{-9}$ $2x10^{-4}$ 19 $I-126$ S $8x10^{-9}$ $5x10^{-5}$ $9x10^{-11}$ $3x10^{-7}$ 20 I $3x10^{-7}$ $3x10^{-3}$ $1x10^{-8}$ $9x10^{-5}$ 21 $I-129$ S $2x10^{-9}$ $1x10^{-5}$ $2x10^{-11}$ $6x10^{-8}$ 22 I $7x10^{-8}$ $6x10^{-3}$ $2x10^{-9}$ $2x10^{-4}$ 23 $I-131$ S $9x10^{-9}$ $6x10^{-5}$ $1x10^{-10}$ $3x10^{-7}$ 24 I $3x10^{-7}$ $2x10^{-3}$ $1x10^{-8}$ $6x10^{-5}$ 25 $I-132$ S $2x10^{-7}$ $2x10^{-3}$ $3x10^{-9}$ $8x10^{-6}$ 26 I $9x10^{-7}$ $5x10^{-3}$ $2x10^{-8}$ $2x10^{-4}$
18 I $2x10^{-7}$ $6x10^{-3}$ $6x10^{-9}$ $2x10^{-4}$ 19 I-126S $8x10^{-9}$ $5x10^{-5}$ $9x10^{-11}$ $3x10^{-7}$ 20 I $3x10^{-7}$ $3x10^{-3}$ $1x10^{-8}$ $9x10^{-5}$ 21 I-129S $2x10^{-9}$ $1x10^{-5}$ $2x10^{-11}$ $6x10^{-8}$ 22 I $7x10^{-8}$ $6x10^{-3}$ $2x10^{-9}$ $2x10^{-4}$ 23 I-131S $9x10^{-9}$ $6x10^{-5}$ $1x10^{-10}$ $3x10^{-7}$ 24 I $3x10^{-7}$ $2x10^{-3}$ $1x10^{-8}$ $6x10^{-5}$ 25 I-132S $2x10^{-7}$ $2x10^{-3}$ $3x10^{-9}$ $8x10^{-6}$ 26 I $9x10^{-7}$ $5x10^{-3}$ $2x10^{-8}$ $2x10^{-4}$
19I-126S $8X10^{-9}$ $5X10^{-5}$ $9X10^{-11}$ $3X10^{-7}$ 20I $3X10^{-7}$ $3X10^{-3}$ $1X10^{-8}$ $9X10^{-5}$ 21I-129S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23I-131S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25I-132S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$ 26I $9X10^{-7}$ $5X10^{-3}$ $2X10^{-8}$ $2X10^{-4}$
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21 $I-129$ S $2X10^{-9}$ $1X10^{-5}$ $2X10^{-11}$ $6X10^{-8}$ 22I $7X10^{-8}$ $6X10^{-3}$ $2X10^{-9}$ $2X10^{-4}$ 23 $I-131$ S $9X10^{-9}$ $6X10^{-5}$ $1X10^{-10}$ $3X10^{-7}$ 24I $3X10^{-7}$ $2X10^{-3}$ $1X10^{-8}$ $6X10^{-5}$ 25 $I-132$ S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$ 26I $9X10^{-7}$ $5X10^{-3}$ $2X10^{-8}$ $2X10^{-4}$
22 I 7×10^{-8} 6×10^{-3} 2×10^{-9} 2×10^{-4} 23 I-131S 9×10^{-9} 6×10^{-5} 1×10^{-10} 3×10^{-7} 24 I 3×10^{-7} 2×10^{-3} 1×10^{-8} 6×10^{-5} 25 I-132S 2×10^{-7} 2×10^{-3} 3×10^{-8} 8×10^{-6} 26 I 9×10^{-7} 5×10^{-3} 2×10^{-8} 2×10^{-4}
23I-131S 9×10^{-9} 6×10^{-5} 1×10^{-10} 3×10^{-7} 24I 3×10^{-7} 2×10^{-3} 1×10^{-8} 6×10^{-5} 25I-132S 2×10^{-7} 2×10^{-3} 3×10^{-9} 8×10^{-6} 26I 9×10^{-7} 5×10^{-3} 3×10^{-8} 3×10^{-4}
24 I $3x10^{-7}$ $2x10^{-3}$ $1x10^{-8}$ $6x10^{-5}$ 25 I-132 S $2x10^{-7}$ $2x10^{-3}$ $3x10^{-9}$ $8x10^{-6}$ 26 I $9x10^{-7}$ $5x10^{-3}$ $3x10^{-8}$ $3x10^{-4}$
25 I-132 S $2X10^{-7}$ $2X10^{-3}$ $3X10^{-9}$ $8X10^{-6}$ 26 I $9X10^{-7}$ $5X10^{-3}$ $3X10^{-8}$ $3X10^{-4}$
26 T 9X10 ⁻⁷ 5X10 ⁻³ 2X10 ⁻⁸ 2X10 ⁻⁴
27 I-133 S 3X10 ⁻⁸ 2X10 ⁻⁴ 4X10 ⁻¹⁰ 1X10 ⁻⁶
28 I 2X10 ⁻⁷ 1X10 ⁻³ 7X10 ⁻⁹ 4X10 ⁻⁵
29 I-134 S 5X10 ⁻⁷ 4X10 ⁻³ 6X10 ⁻⁹ 2X10 ⁻⁵
30 I 3X10 ⁻⁶ 2X10 ⁻² 1X10 ⁻⁷ 6X10 ⁻⁴
31 I-135 S 1X10 ⁻⁷ 7X10 ⁻⁴ 1X10 ⁻⁹ 4X10 ⁻⁶
32 I 4X10 ⁻⁷ 2X10 ⁻³ 1X10 ⁻⁸ 7X10 ⁻⁵
$33 \qquad LL \qquad Tridium (77).$
$34 \text{ Ir} - 190 \text{ S} 1 \times 10^{-6} \text{ 6} \times 10^{-3} \text{ A} \times 10^{-8} \text{ 2} \times 10^{-4}$
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1		I	4X10 ⁻⁷	5x10 ⁻³	1X10 ⁻⁸	³ 2x10 ⁻⁴	
2	Ir-192	S	1X10 ⁻⁷	1X10 ⁻³	4X10 ⁻⁹	4X10 ⁻⁵	
3		I	3X10 ⁻⁸	1X10 ⁻³	9x10 ⁻¹	.0 4x10 ⁻⁵	
4	Ir-194	S	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	3x10-5	
5		I	2X10 ⁻⁷	9X10 ⁻⁴	5X10 ⁻⁹	3x10 ⁻⁵	
6		,	MM. Trond	(26) •			
7	Fe-55	s	9X10 ⁻⁷	2x10 ⁻²	38-0-8	8810-4	
8		I	1X10 ⁻⁶	$7x_{10}^{-2}$	3x10 ⁻⁸	$2x10^{-3}$	
9	Fe-59	S	1X10 ⁻⁷	2x10 ⁻³	5x10 ⁻⁹	6x10 ⁻⁵	
10		I	5X10 ⁻⁸	2X10 ⁻³	2X10 ⁻⁹	5x10 ⁻⁵	
11	W = 05=	1	NN. Krypto	on (36):			
12	Kr-85m	ь 2	cwi o Th		7		
13	Su Wm OF O		6X10 °		1X10 ,		
14	KI-85 5	dub			3X10 '		
15	Kr-8/ S	iub			2X10 °		
16	Kr-88 S	lub	1X10 0		2X10 ⁻⁰		
17		C	0. Lantha	num (57):			
18	La-140	S	2X10 ⁻⁷	7X10 ⁻⁴	5X10 ⁻⁹	2X10 ⁻⁵	
19		I	1X10 ⁻⁷	7X10 ⁻⁴	4x10 ⁻⁹	2X10 ⁻⁵	
20		F	P. Lead (82):			
21	Pb-203	S	3X10 ⁻⁶	1X10 ⁻²	9X10 ⁻⁸	4×10^{-4}	
22		I	2X10 ⁻⁶	1X10 ⁻²	6X10 ⁻⁸	4×10^{-4}	
23	Pb-210	S	1X10 ⁻¹⁰	4X10-6	4x10 ⁻¹	2 1X10 ⁻⁷	
24		I	2X10 ⁻¹⁰	5X10 ⁻³	8X10 ⁻¹	2 2X10 ⁻⁴	
25	Pb-212	S	2X10 ⁻⁸	6X10 ⁻⁴	6X10 ⁻¹	0 2X10 ⁻⁵	
26		I	2X10 ⁻⁸	5X10 ⁻⁴	7X10 ⁻¹	0 _{2X10} -5	
27		0	0. Luteti	um (71):			
28	Lu-177	s	6X10 ⁻⁷	3x10 ⁻³	$2x10^{-8}$	1×10^{-4}	
29	24 277	т	5x10 ⁻⁷	3×10-3	2x10 ⁻⁸	1×10 ⁻⁴	
		-	JATO	JAIU	. 2410	IALU	
30		R	R. Mangan	ese (25):			
31	Mn-52	S	2X10 ⁻⁷	1X10 ⁻³	7X10 ⁻⁹	3X10 ⁻⁵	
32		I	1X10 ⁻⁷	9X10 ⁻⁴	5X10 ⁻⁹	3X10 ⁻⁵	
33	Mn-54	S	4x10 ⁻⁷	4x10 ⁻³	1X10 ⁻⁸	1X10 ⁻⁴	

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1		Ī	4X10 ⁻⁸	3X10 ⁻³	1x10 ⁻⁹	1X10 ⁻⁴
2	Mn-56	S	8X10 ⁻⁷	4X10 ⁻³	3X10 ⁻⁸	1X10 ⁻⁴
3		I	5X10 ⁻⁷	3X10-3	2X10 ⁻⁸	1X10 ⁻⁴
Д			SS Marcuru	(80).		
5	Ha-197m	S	7×10 ⁻⁷	6×10 ⁻³	8-012	2×10^{-4}
5	119 197m	т	8X10 ⁻⁷	5×10 ⁻³	2×10 ⁻⁸	2×10^{-4}
7	Ha-197	÷ د	<u>1х10</u> -б	av10-3	4×10-8	$2x10^{-4}$
, 8	mg 197	т	3810-6	1 1 1 0 - 2	4X10 0X10 ⁻⁸	5x10-4
9	Ha-203	r c	7810-8	5×10 ⁻⁴	9×10 ⁻⁹	5x10 ⁵
10	119 205	т	1×10-7	3×10-3	2×10 ⁻⁹	$2X10^{-4}$
ŦŬ		Ŧ	INIO	JALO .	4410	IXIO
11			TT. Molybder	num (42):		
12	Mo-99	S	7X10 ⁻⁷	5X10 ⁻³	3X10 ⁻⁸	2X10 ⁻⁴
13		I	2X10 ⁻⁷	1X10 ⁻³	7X10 ⁻⁹	4X10 ⁻⁵
14			UU. Neodumiu	ım (60):		
15	Nd-144	S	8x10 ⁻¹¹	$2x10^{-3}$	3x10 ⁻¹²	7X10 ⁻⁵
16		I	3X10 ⁻¹⁰	2×10^{-3}	1×10-11	8x10 ⁻⁵
17	Nd-147	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6x10 ⁻⁵
18		I	2X10 ⁻⁷	2×10^{-3}	8x10 ⁻⁹	6X10 ⁻⁵
19	Nd-149	S	2X10 ⁻⁶	8X10 ⁻³	6x10 ⁻⁸	3×10^{-4}
20		I	1X10-6	8X10 ⁻³	5x10 ⁻⁸	3×10^{-4}
21			VV. Neptuniu	ım (93):		_
22	Np-237	S	4X10 ⁻¹²	9x10 ⁻⁵	1X10 ⁻¹³	3X10 ⁻⁶
23		Ι	1X10 ⁻¹⁰	9X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
24	Np-239	S	8X10 ⁻⁷	4X10 ⁻³	3X10 ⁻⁸	1X10 ⁻⁴
25		Ι	7X10 ⁻⁷	4X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
26			WW. Nickel (28):	·	
27	Ni-59	S	5X10 ⁻⁷	6X10 ⁻³	2X10 ⁻⁸	2X10 ⁻⁴
28		I	8x10 ⁻⁷	6X10 ⁻²	3X10 ⁻⁸	2X10 ⁻³
29	Ni-63	S	6X10 ⁻⁸	8X10 ⁻⁴	2X10 ⁻⁹	3X10 ⁻⁵
30		I	3X10 ⁻⁷	2X10 ⁻²	1X10 ⁻⁸	7X10 ⁻⁴
31	Ni-65	S	9X10 ⁻⁷	4X10 ⁻³	3X10 ⁻⁸	1X10 ⁻⁴
32		I	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
33			XX. Niobium	(41):		

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1	Nb-93m	S	1X10 ⁻⁷	1X10 ⁻²	4X10 ⁻¹	Ð	4X10 ⁻⁴	
2		I	2X10 ⁻⁷	1X10 ⁻²	5x10 ⁻⁹	Ð	4x10 ⁻⁴	
3	Nb-95	S	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	3	1X10 ⁻⁴	
4		I	1X10 ⁻⁷	3X10 ⁻³	3X10 ⁻⁹	Ð	1X10 ⁻⁴	
5	Nb-97	S	6X10 ⁻⁶	3X10 ⁻²	2x10-	7	9x10 ⁻⁴	
6		I	5X10 ⁻⁶	3X10 ⁻²	2X10-	7	9x10 ⁻⁴	
7		Y	Y. Osmium (7	6):				
8	Os-185	S	5X10 ⁻⁷	2x10 ⁻³	2X10 ⁻⁸	3	7x10 ⁻⁵	
9		I	5X10 ⁻⁸	2X10 ⁻³	2X10 ⁻⁹	9	7x10 ⁻⁵	
10	Os-191m	S	2X10 ⁻⁵	7X10 ⁻²	6X10-	7	3X10 ⁻³	
11 .		I	9x10-6	7X10 ⁻²	3X10-7	7	2X10 ⁻³	
12	Os-191	S	lXl0 ⁻⁶	5X10 ⁻³	4X10 ⁻⁸	3	2X10 ⁻⁴	
13		I	4X10 ⁻⁷	5x10 ⁻³	1X10-8	3	2X10 ⁻⁴	
14	Os-193	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	3	6X10 ⁻⁵	
15		I	3X10 ⁻⁷	2X10 ⁻³	9X10 ⁻⁹)	5X10 ⁻⁵	
16		Z	Z. Palladium	(46):				
17	Pd-103	S	1X10 ⁻⁶	1X10 ⁻²	5X10 ⁻⁸	3	3X10 ⁻⁴	
18		I	7X10 ⁻⁷	8x10 ⁻³	3x10-8	3	3X10 ⁻⁴	
19	Pd-109	S	6x10 ⁻⁷	3X10 ⁻³	2x10 ⁻⁸	}	9x10 ⁻⁵	
20		I	4X10 ⁻⁷	2X10 ⁻³	1X10-8	; .	7x10 ⁻⁵	
21		Δ		ng (15).				
21 22	D-32	ۍ ح	7×10^{-8}	5×10^{-4}	2210-9) .	2210-5	
23	1 92	т	8x10 ⁻⁸	7×10^{-4}	3x10-9	· .	2x10-5	
25		-	<i>P</i> .	/ 110	JAIO		2710	
24		B	BB. Platinum	(78):				
25	Pt-191	S	8x10 ⁻⁷	4X10 ⁻³	3x10-8		1X10 ⁻⁴	
26		I	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	;	1X10 ⁻⁴	
27	Pt-193m	S	7X10 ⁻⁶	3X10 ⁻²	2X10 ⁻⁷	, .	1X10 ⁻³	
28		I	5X10 ⁻⁶	3X10 ⁻²	2X10 ⁻⁷	· · ·	1X10 ⁻³	
29	Pt-193	S	1X10 ⁻⁶	3X10 ⁻²	4X10 ⁻⁸	9	9X10 ⁻⁴	
30		I	3X10 ⁻⁷	5X10 ⁻²	1X10-8		2X10 ⁻³	
31	Pt-197m	S	6X10 ⁻⁶	3X10 ⁻²	2X10 ⁻⁷		1X10 ⁻³	
32		I	5X10 ⁻⁶	3X10 ⁻²	2X10 ⁻⁷	9	9x10 ⁻⁴	
33	Pt-197	S	8X10 ⁻⁷	4X10 ⁻³	3X10 ⁻⁸		1X10 ⁻⁴	
34		I	6x10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸		LX10 ⁻⁴	

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1			CCC. Plutor	nium (94):		
2	Pu-238	S	2X10 ⁻¹²	1X10 ⁻⁴	7X10 ⁻¹⁴	5X10 ⁻⁶
3		I	3X10 ⁻¹¹	8X10 ⁻⁴	1X10-12	3X10 ⁻⁵
4	Pu-239	S	2X10 ⁻¹²	1X10 ⁻⁴	6X10 ⁻¹⁴	5X10 ⁻⁶
5		I	4X10 ⁻¹¹	8X10 ⁻⁴	1X10-12	3X10 ⁻⁵
6	Pu-240	S	2X10 ⁻¹²	1X10 ⁻⁴	6X10 ⁻¹⁴	5X10 ⁻⁶
7		I	4X10 ⁻¹¹	8X10 ⁻⁴	1X10 ⁻¹²	3X10 ⁻⁵
8	Pu-241	S	9x10 ⁻¹¹	7X10 ⁻³	3X10 ⁻¹²	$2X10^{-4}$
9		I	4X10 ⁻⁸	4X10 ⁻²	1X10 ⁻⁹	1X10 ⁻³
10	Pu-242	S	2X10 ⁻¹²	1×10^{-4}	6X10 ⁻¹⁴	5X10 ⁻⁶
11		I	4X10 ⁻¹¹	9X10 ⁻⁴	1X10 ⁻¹²	3X10 ⁻⁵
12	Pu-243	S	2X10 ⁻⁶	1X10 ⁻²	6X10 ⁻⁸	3X10 ⁻⁴
13		I	2X10 ⁻⁶	1X10 ⁻²	8X10 ⁻⁸	3X10 ⁻⁴
14	Pu-244	S	2X10 ⁻¹²	1X10 ⁻⁴	6X10 ⁻¹⁴	4X10 ⁻⁶
15		I	3X10 ⁻¹¹	3X10 ⁻⁴	1X10 ⁻¹²	1X10 ⁻⁵
16				··· (94) ·		
17	Do . 210	c	EV10-10	.um (84):	2810-11	73710-7
10	P0-210	5	5×10^{-10}	2X10 -4	2×10^{-12}	/X10 /
10		T	2810 -5	8X10	/XI0	3X10 -
19			EEE. Potass	ium (19):		
20	K-42	S	2X10 ⁻⁶	9X10 ⁻³	7X10 ⁻⁸	3X10 ⁻⁴
21		I	1X10 ⁻⁷	6X10 ⁻⁴	4X10 ⁻⁹	2X10 ⁻⁵
-				<i>Aumium (50)</i>		
22	D= 142	G	rrr. praeso	ovi 0 ⁻⁴	7710-9	28710-5
23	Pr-142	5	2X10 /	9x10 -	/XIU 9	3X10 °
24		I	2X10 '	9X10 =	5X10 ⁹	3X10 5
25	Pr-143	S	3X10 ⁻⁷	1X10 ⁻⁵	1X10-8	5X10 ⁻⁵
26		Ι	2X10 ⁻ /	1X10 ⁻⁵	6X10 ⁻⁹	5X10 ⁻⁵
27		(GGG. Promet	hium (61):		
28	Pm-147	S	6X10 ⁻⁸	6X10 ⁻³	2X10 ⁻⁹	2X10 ⁻⁴
29		I	1X10 ⁻⁷	6X10 ⁻³	3X10 ⁻⁹	2X10 ⁻⁴
30	Pm-149	S	3X10 ⁻⁷	1X10 ⁻³	1X10 ⁻⁸	4X10 ⁻⁵
31		I	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	4X10 ⁻⁵
32		I	HHH. Protac	tinium (91):		<u>-</u>
33	Pa-230	S	$2X10^{-9}$	7X10 ⁻³	6X10 ⁻¹¹	2X10 ⁻⁴

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1		I	8X10 ⁻¹⁰	7X10 ⁻³	3X10 ⁻¹¹	$2X10^{-4}$
2	Pa-231	5	3 1X10 ⁻¹²	3x10 ⁻⁵	4X10 ⁻¹⁴	9X10 ⁻⁷
3		I	1X10 ⁻¹⁰	8X10 ⁻⁴	4X10 ⁻¹²	2X10 ⁻⁵
4	Pa-2 33	S	6X10 ⁻⁷	4x10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
5		I	2X10 ⁻⁷	3X10 ⁻³	6X10 ⁻⁹	1X10 ⁻⁴
6			III. Radium (88) : -5	11	7
7	Ra-223	S	2X10 ⁻⁹	2X10-5	6X10 ⁻¹¹	7X10 ⁻⁷
8		I	2X10 ⁻¹⁰	1X10 ⁻⁴	8X10 ⁻¹²	4X10 ⁻⁶
9	Ra-224	S	5X10 ⁻⁹	7X10 ⁻⁵	2X10 ⁻¹⁰	2X10 ⁻⁶
10		I	7X10 ⁻¹⁰	$2X10^{-4}$	2X10 ⁻¹¹	5X10 ⁻⁶
11	Ra-226	S	3X10 ⁻¹¹	4X10 ⁻⁷	3X10 ⁻¹²	3X10 ⁻⁸
12		I	5X10 ⁻¹¹	9X10 ⁻⁴	2X10 ⁻¹²	3X10-5
13	Ra-228	S	7X10 ⁻¹¹	8X10 ⁻⁷	2X10 ⁻¹²	3X10 ⁻⁸
14		I	4X10 ⁻¹¹	7X10 ⁻⁴	1X10 ⁻¹²	3X10 ⁻⁵
. –				~)		
15			JJJ. Radon (8	6):	0	
16	Rn-220	S	3X10 /		1x10-8	
17	Rn-2223	S	3X10 ⁻⁸		3X10-9	
18			KKK. Rhenium	(75):		
19	Re-183	S	3X10 ⁻⁶	2X10 ⁻²	9x10 ⁻⁸	6X10 ⁻⁴
20		I	2X10 ⁻⁷	8X10 ⁻³	5x10 ⁻⁹	3X10 ⁻⁴
21	Re-186	S	6X10 ⁻⁷	3 X10⁻³	2X10 ⁻⁸	9X10 ⁻⁵
22		I	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	5X10 ⁻⁵
23	Re-187	s	9X10 ⁻⁶	7X10 ⁻²	3X10 ⁻⁷	3X10 ⁻³
24		I	5X10 ⁻⁷	4X10 ⁻²	2X10 ⁻⁸	2X10 ⁻³
25	Re-188	s	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
26		I	2X10 ⁻⁷	9x10 ⁻⁴	6X10 ⁻⁹	3X10 ⁻⁵
27			LLL. Rhodium	(45):		
28	Rh-103m	S	8X10 ⁻⁵	4X10 ⁻¹	3X10 ⁻⁶	1X10 ⁻²
29		I	6X10 ⁻⁵	3X10 ⁻¹	2X10 ⁻⁶	1X10 ⁻²
30	Rh-105	s	8x10 ⁻⁷	4×10^{-3}	3X10 ⁻⁸	1X10 ⁻⁴
31		I	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
32			MMM. Rubidium	(37):		
33	Rb-86	S	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	7X10 ⁻⁵

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1		I	7X10 ⁻⁸	7X10 ⁻⁴	2x10 ⁻⁹	2X10 ⁻⁵	
2	Rb-87	S	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1x10 ⁻⁴	
3		I	7X10 ⁻⁸	5x10 ⁻³	2X10 ⁻⁹	2X10 ⁻⁴	
1							
4	Bu-07	c		2111 UM (44):	ow1 o ⁻⁸	4.112 0 - 4	
5	Ku-97	э т	2210		8×10	$4X10^{-4}$	
0	Pu-103	±	5×10 ⁻⁷		5X10 ⁻⁸	3X10 -	
, 8	Ku-105	ъ	ov10 ⁻⁸	2×10 ⁻³	2×10 -9	8X10 °	
0	Bu - 105	T C	7×10-7	2X10 -3	3X10	8X10 9	
10	KU-105	ъ	5×10 ⁻⁷	2×10 ⁻³	2810	1×10^{-4}	
11	R11-106	r c	8810-8	4×10-4	2×10-9	1×10-5	
12	nu 100	т	6×10 ⁻⁹	3×10-4	2×10 ⁻¹⁰	1×10 ⁻⁵	
- 2		-	UNIU	JAIO	2810	IXIO	
13			000. Samaı	cium (62):			
14	Sm-147	S	7X10 ⁻¹¹	2X10 ⁻³	2X10 ⁻¹²	6X10 ⁻⁵	
15		I	3X10 ⁻¹⁰	2X10 ⁻³	9X10 ⁻¹²	7X10 ⁻⁵	
16	Sm-151	S	6X10 ⁻⁸	1X10 ⁻²	2X10 ⁻⁹	$4X10^{-4}$	
17		I	1X10 ⁻⁷	1X10 ⁻²	5X10 ⁻⁹	4×10^{-4}	
18	Sm-153	S	5X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	8X10 ⁻⁵	
19		I	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	8X10 ⁻⁵	
20			PPP. Scand	lium (21):			
21	Sc-46	S	2X10 ⁻⁷	1X10 ⁻³	8X10 ⁻⁹	4X10 ⁻⁵	
22		I	2X10 ⁻⁸	1X10 ⁻³	8x10 ⁻¹⁰	4x10 ⁻⁵	
2 3	Sc-47	S	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	9x10 ⁻⁵	
24		I	5X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	9x10 ⁻⁵	
25	Sc-48	S	2X10 ⁻⁷	8X10 ⁻⁴	6X10 ⁻⁹	3x10 ⁻⁵	
26		I	1X10 ⁻⁷	8X10 ⁻⁴	5X10 ⁻⁹	3X10 ⁻⁵	
27			000 50100	ium (31).			
28	Se-75	c	1 v 10 ⁻ 6	ov10-3	AV10 ⁻⁸	2210-4	
29	56 /5	т	1×10^{-7}	8×10 ⁻³	4×10 ⁻⁹	3810-4	
~ /		Ŧ	LALU	GALU	AVIO	JUTO	
30	RRR. Silicon (14):						
31	Si-31	S	6X10 ⁻⁶	3X10 ⁻²	2X10 ⁻⁷	9X10 ⁻⁴	
32		I	1X10 ⁻⁶	6X10 ⁻³	3X10 ⁻⁸	2X10 ⁻⁴	
33		:	SSS. Silve	r (47):			

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1	Ag-105	S	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
2		I	8x10 ⁻⁸	3X10 ⁻³	3x10 ⁻⁹	1X10 ⁻⁴
3	Ag-110m	S	2X10 ⁻⁷	9x10 ⁻⁴	7x10 ⁻⁹	3X10 ⁻⁵
4		I	1X10 ⁻⁸	9X10 ⁻⁴	3X10 ⁻¹⁰	3X10 ⁻⁵
5	Ag-111	s	3X10 ⁻⁷	1X10 ⁻³	1X10 ⁻⁸	4X10 ⁻⁵
6		I	2X10 ⁻⁷	1X10 ⁻³	8x10 ⁻⁹	4X10 ⁻⁵
7			TTT. Sodium	(11):		
8	Na-22	s	2X10 ⁻⁷	1X10 ⁻³	6x10 ⁻⁹	4x10 ⁻⁵
9		I	9x10 ⁻⁹	9x10 ⁻⁴	3x10 ⁻¹⁰	3x10 ⁻⁵
10	Na-24	s	1X10 ⁻⁶	6X10 ⁻³	4x10 ⁻⁸	2X10 ⁻⁴
11		I	1X10 ⁻⁷	8X10 ⁻⁴	5x10 ⁻⁹	3X10 ⁻⁵
12			UUU. Stronti	.um (38):	r.	2
13	Sr-85m	S	4X10 ⁻⁵	2X10 ⁻¹	1X10 ⁻⁶	7X10 ⁻³
14		Ι	3X10 ⁻⁵	2X10 ⁻¹	1X10 ⁻⁶	7X10 ⁻³
15	Sr-85	S	2X10 ⁻⁷	3X10 ⁻³	8X10 ⁻⁹	1X10 ⁻⁴
16		Ι	1X10 ⁻⁷	5X10 ⁻³	4X10 ⁻⁹	2X10 ⁻⁴
17	Sr-89	S	3X10 ⁻⁸	3X10 ⁻⁴	3X10-10	3X10 ⁻⁶
18		Ι	4X10 ⁻⁸	8X10 ⁻⁴	1x10-9	3X10 ⁻⁵
19	Sr-90	S	1X10 ⁻⁹	1X10 ⁻⁵	3X10 ⁻¹¹	3X10 ⁻⁷
20		I	5x10 ⁻⁹	1X10 ⁻³	2X10 ⁻¹⁰	4X10 ⁻⁵
21	Sr-91	S	4X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	7X10 ⁻⁵
22		I	3X10 ⁻⁷	1X10 ⁻³	9X10 ⁻⁹	5X10 ⁻⁵
23	Sr-92	S	4X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	7X10 ⁻⁵
24		I	3x10 ⁻⁷ **	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
25			VVV. Sulfur	(16):	•	
26	S- 35	s	3X10 ⁻⁷	2X10 ⁻³	9x10 ⁻⁹	6X10 ⁻⁵
27		I	3X10 ⁻⁷	8X10 ⁻³	9x10 ⁻⁹	3X10 ⁻⁴
28		-	WWW. Tantalu	m (73):	9	-5
29	'Ta-182	s -	4X10	1X10 ⁻⁵	1X10 ²	4X10 5
30		I	2X10 0	1X10 ⁻⁵	7X10 ⁻¹⁰	4X10 ⁻⁵
31		2	XXX. Technet.	ium (43):		
32	Tc-96m	S	8X10 ⁻⁵	4X10 ⁻¹	3X10 ⁻⁶	1X10 ⁻²
33		I	3X10 ⁻⁵	3X10 ⁻¹	lXl0 ⁻⁶	1X10 ⁻²

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1	Tc-96	S	6x10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴
2		I	2X10 ⁻⁷	1X10 ⁻³	8x10 ⁻⁹	5x10 ⁻⁵
3	Tc-97m	S	2X10 ⁻⁶	1X10 ⁻²	8X10 ⁻⁸	4×10^{-4}
4		I	2X10 ⁻⁷	5X10 ⁻³	5x10 ⁻⁹	2X10 ⁻⁴
5	Tc-97	S	1X10 ⁻⁵	5X10 ⁻²	4x10 ⁻⁷	2X10 ⁻³
6		I	3X10 ⁻⁷	2X10 ⁻²	1X10 ⁻⁸	8X10 ⁻⁴
7	Tc-99m	S	4X10 ⁻⁵	2X10 ⁻¹	1X10 ⁻⁶	6x10 ⁻³
8		I	1X10 ⁻⁵	8X10 ⁻²	5X10 ⁻⁷	3X10 ⁻³
9	Tc-99	S	2X10 ⁻⁶	1X10 ⁻²	7X10 ⁻⁸	3X10 ⁻⁴
10		I	6X10 ⁻⁸	5X10 ⁻³	2X10 ⁻⁹	2X10 ⁻⁴
11			YYY. Tellu	rium (52):		
12	Te-125m	s	4X10 ⁻⁷	5x10 ⁻³	1X10 ⁻⁸	2X10 ⁻⁴
13		I	1X10 ⁻⁷	3X10 ⁻³	4X10 ⁻⁹	1X10 ⁻⁴
14	Te-127m	s	1X10 ⁻⁷	2X10 ⁻³	5x10 ⁻⁹	6x10 ⁻⁵
15		I	4X10 ⁻⁸	2X10 ⁻³	1X10 ⁻⁹	5x10 ⁻⁵
16	Te-127	S	2X10 ⁻⁶	8X10 ⁻³	6X10 ⁻⁸	3X10 ⁻⁴
17		I	9X10 ⁻⁷	5X10 ⁻³	3X10 ⁻⁸	2X10 ⁻⁴
18	Te-129m	S	8X10 ⁻⁸	1X10 ⁻³	3X10 ⁻⁹	3X10 ⁻⁵
19		I	3X10 ⁻⁸	6X10 ⁻⁴	1X10 ⁻⁹	2X10 ⁻⁵
20	Te-129	S	5X10 ⁻⁶	2X10 ⁻²	7X10 ⁻⁸	8X10 ⁻⁴
2 1		I	4X10 ⁻⁶	2X10 ⁻²	1X10 ⁻⁷	8X10 ⁻⁴
22	Te-131m	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
2 3		Ι	2X10 ⁻⁷	1X10-3	6X10 ⁻⁹	4x10 ⁻⁵
24	Te-132	S	2X10 ⁻⁷	9x10 ⁻⁴	7X10 ⁻⁹	3X10 ⁻⁵
25		I	1×10-7	6X10 ⁻⁴	4X10 ⁻⁹	2x10 ⁻⁵
26			ZZZ. Terbi	um (65):		
27	Tb-160	s	1X10 ⁻⁷	1X10 ⁻³	3X10 ⁻⁹	4x10 ⁻⁵
28		I	3X10 ⁻⁸	1X10 ⁻³	1X10 ⁻⁹	4x10 ⁻⁵
29			AAAA. Thal.	lium (81):		
30	T1-200	s	3X10-6	1x10 ⁻²	9x10 ⁻⁸	4x10 ⁻⁴
31		I	1X10 ⁻⁶	7X10 ⁻³	4X10 ⁻⁸	2X10 ⁻⁴
32	T1-201	S	2X10 ⁻⁶	9x10 ⁻³	7x10 ⁻⁸	3x10 ⁻⁴
33		I	9x10 ⁻⁷	5x10 ⁻³	3X10 ⁻⁸	2X10 ⁻⁴
34	T1-202	s	8x10 ⁻⁷	4x10 ⁻³	3X10 ⁻⁸	1X10 ⁻⁴

08/01/91 [REVISOR] LMB/BD AR1543 8X10⁻⁹ 2×10^{-7} 2×10^{-3} 7X10⁻⁵ 1 Ι 2X10⁻⁸ 6×10^{-7} 3X10⁻³ 1×10^{-4} T1-204 S 2 9X10⁻¹⁰ $2X10^{-3}$ 3X10⁻⁸ 6X10⁻⁵ 3 T BBBB. Thorium (90): 4 3X10⁻¹⁰ 2X10⁻⁵ 5×10^{-4} 1X10⁻¹¹ 5 Th-227 S 2×10^{-10} 6X10⁻¹² 5×10^{-4} 2X10⁻⁵ Ι 6 3X10⁻¹³ 9X10⁻¹² 2×10^{-4} 7X10⁻⁶ 7 Th-228 S 6X10⁻¹² 1X10⁻⁵ $4X10^{-4}$ 2X10⁻¹³ 8 Ι 2X10⁻¹² 2X10⁻⁶ 5×10^{-5} 8X10⁻¹⁴ Th-230 9 S lXl0^{-ll} 9X10⁻⁴ 3X10⁻¹³ 3X10⁻⁵ 10 Ι 1×10^{-6} 7X10⁻³ 5X10⁻⁸ $2X10^{-4}$ 11 Th-231 S 1X10⁻⁶ 7X10⁻³ 4×10^{-8} 2×10^{-4} 12 I 5X10⁻⁵ 3X10⁻¹¹ 1X10⁻¹² 2X10⁻⁶ 13 Th-232 S $3x10^{-11}$ 4X10⁻⁵ Ι 1×10^{-3} 1×10^{-12} 14 15 Th-nat-6X10⁻¹¹ 2X10⁻⁶ 6X10⁻⁵ 2×10^{-12} S 16 ural 6X10⁻⁴ 2X10⁻¹² 6X10⁻¹¹ 2X10⁻⁵ 17 Ι 6X10⁻⁸ 5X10⁻⁴ 2X10⁻⁹ 2X10⁻⁵ 18 Th-234 S 3X10⁻⁸ 5X10⁻⁴ 2X10⁻⁵ 19 Ι 1X10⁻⁹ CCCC. Thullium (69): 20 4X10⁻⁸ 1X10⁻⁹ 5X10⁻⁵ 1X10⁻³ 21 Tm-170 S 1X10⁻³ 1X10⁻⁹ 3X10⁻⁸ 5X10⁻⁵ 22 Ι 1X10⁻⁷ 1X10⁻² $4X10^{-9}$ 5X10⁻⁴ 23 Tm-171 S 2X10^{-7°°} 1X10⁻² 8x10⁻⁹ 5×10^{-4} 24 Ι 1 25 DDDD. *Tin* (50): $4X10^{-7}$ 2×10^{-3} 1X10⁻⁸ 9X10⁻⁵ 26 Sn-113 S 5x10⁻⁸ 2X10⁻⁹ 2×10^{-3} 8X10⁻⁵ 27 Т 2X10⁻⁵ 1×10^{-7} 5X10⁻⁴ 4×10^{-9} 28 Sn-125 S 2X10⁻⁵ 8×10⁻⁸ 5×10^{-4} 3X10⁻⁹ Ι 29 30 EEEE. Tungsten (74): 8x10⁻⁸ 2X10⁻⁶ 1X10⁻² 4×10^{-4} 31 W-181 S 1X10⁻⁷ 1X10⁻² 4X10⁻⁹ 3X10⁻⁴ 32 Ι 4X10⁻³ 1X10⁻⁴ 8X10⁻⁷ 3X10⁻⁸ 33 W-185 S 1X10⁻⁷ 3X10⁻³ $4X10^{-9}$ 1×10^{-4} 34 Ι

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1	W-187	S	4X10 ⁻⁷	2X10 ⁻³	2X10 ⁻⁸	7X10 ⁻⁵
2		I	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵
2						
3	11-220	c	pref. Urani	um (92):	1210-11	
4	0-230	ъ т	$3X10^{-10}$	1×10-4	1110 -12	5X10 °
5	11-222	L C		1X10 ⁻⁴	$4X10^{-12}$	5X10 °
7	0-232	5		8X10 ⁻⁴	$3X10^{-13}$	3X10 5
/	11 222	T	3X10 = -10	8X10 ⁻⁴	9x10 ⁻¹¹	3X10 5
8	U-233	- S	5×10^{-10}	9X10 =	$2X10^{-12}$	3X10 5
9	TT 004	1 a4	1×10^{-10}	9X10 -	4X10 12	3X10 5
10	U-234	5-	6×10^{-10}	9X10 -	2X10 11	3X10 5
		-4	1×10^{-10}	9X10 4	4X10 12	3X10 5
12	U-235	S⁺	5×10^{-10}	8X10 -	2X10 ¹¹	3X10 5
13		I	1X10-10	8X10 ⁻⁴	4X10 ⁻¹²	3X10 ⁻⁵
14	U-236	S	6X10 ⁻¹⁰	1X10 ⁻⁵	2X10-11	3X10 ⁻⁵
15		I	1X10 ⁻¹⁰	1X10 ⁻³	2X10-11	3X10 ⁻⁵
16	U-238	S ⁴	7X10 ⁻¹¹	1X10 ⁻³	3X10 ⁻¹²	4X10 ⁻⁵
17		I	1X10 ⁻¹⁰	1X10 ⁻³	5X10 ⁻¹²	4X10 ⁻⁵
18	U-240	S	2X10 ⁻⁷	1X10 ⁻³	8x10 ⁻⁹	3X10 ⁻⁵
19		I	2X10 ⁻⁷	1X10 ⁻³	6X10 ⁻⁹	3X10 ⁻⁵
20	U-nat	s ⁴	1X10 ⁻¹⁰	1X10 ⁻³	5X10 ⁻¹²	3X10 ⁻⁵
21		I	1X10 ⁻¹⁰	1X10 ⁻³	2X10 ⁻¹²	3X10 ⁻⁵
22			GGGG. Vanad	ium (23):		
23	V-48	s	2X10 ⁻⁷	9x10 ⁻⁴	6X10 ⁻⁹	3X10 ⁻⁵
24		I	6X10 ⁻⁸	8X10 ⁻⁴	2X10 ⁻⁹	3X10 ⁻⁵
25			НННН. Хелол	(54):		
26	Xe-13lr	n				
27	St	ub ²	2X10 ⁻⁵		4X10 ⁻⁷	
28	Xe-133r	n				
29	Su	1 ² 41	1X10 ⁻⁵		3X10 ⁻⁷	
30	Xe-133					
31	Su	1b ²	1X10 ⁻⁵		3X10 ⁻⁷	
32	Xe-135					
33	Sı	ıb ²	4X10 ⁻⁶		1X10 ⁻⁷	
34			IIII. Ytter	bium (70):		

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1	Yb-175	S	7X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴	
2		I	6X10 ⁻⁷	3X10 ⁻³	2X10 ⁻⁸	1X10 ⁻⁴	
3		J	JJJ. Ytt	rium (39):			
4	Y-88*	S	3X10 ⁻⁷	2X10 ⁻³	6x10 ⁻⁹	7X10 ⁻⁵	
5		I	5X10 ⁻⁸	3x10 ⁻³	2X10 ⁻⁹	9x10 ⁻⁵	
6	Y-90	S	1X10 ⁻⁷	6X10 ⁻⁴	4X10 ⁻⁹	2X10 ⁻⁵	
7		I	1X10 ⁻⁷	6X10 ⁻⁴	3X10 ⁻⁹	2X10 ⁻⁵	
8	Y-91m	S	2X10 ⁻⁵	1X10 ⁻¹	8X10 ⁻⁷	3X10 ⁻³	
9		I	2X10 ⁻⁵	1X10 ⁻¹	6X10 ⁻⁷	3X10 ⁻³	
10	Y-91	S	4X10 ⁻⁸	8X10 ⁻⁴	1X10 ⁻⁹	3X10 ⁻⁵	
11		I	3X10 ⁻⁸	8X10 ⁻⁴	1X10 ⁻⁹	3X10 ⁻⁵	
12	Y-92	S	4X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵	
13		I	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵	
14	Y-93	S	2X10 ⁻⁷	8X10 ⁻⁴	6x10 ⁻⁹	3X10 ⁻⁵	
15		I	1X10 ⁻⁷	8X10 ⁻⁴	5X10 ⁻⁹	3X10 ⁻⁵	
16		K	KKK. Zin	c (30):			
17	Zn-65	S	1X10 ⁻⁷	3X10 ⁻³	4X10 ⁻⁹	1X10 ⁻⁴	
18		I	6X10 ⁻⁸	5X10 ⁻³	2X10 ⁻⁹	2X10 ⁻⁴	
19	Zn-69m	S	4X10 ⁻⁷	2X10 ⁻³	6X10 ⁻⁸	7X10 ⁻⁵	
20		I	3X10 ⁻⁷	2X10 ⁻³	1X10 ⁻⁸	6X10 ⁻⁵	
21	Zn-69	S	7X10 ⁻⁶	5X10 ⁻²	2X10 ⁻⁷	2X10 ⁻³	
22		I	9X10 ⁻⁶	5X10 ⁻²	3X10 ⁻⁷	2X10 ⁻³	
2 3		L	LLL. Zire	conium (40):			
24	Zr-93	S	1X10 ⁻⁷	2X10 ⁻²	4X10 ⁻⁹	8X10 ⁻⁴	
25		I	3X10 ⁻⁷	2X10 ⁻²	1X10 ⁻⁸	8X10 ⁻⁴	
26	Zr-95	S	1X10 ⁻⁷	2X10 ⁻³	4X10 ⁻⁹	6X10 ⁻⁵	
2 7		I	3X10 ⁻⁸	2X10 ⁻³	1X10 ⁻⁹	6X10 ⁻⁵	
28	Zr-97	S	1X10 ⁻⁷	5X10 ⁻⁴	4X10 ⁻⁹	2X10 ⁻⁵	
29		I	9X10 ⁻⁸	5X10 ⁻⁴	3X10 ⁻⁹	2X10 ⁻⁵	
30		M	MMM. Any	single radio	nuclide not lis	sted in items A	
31	to LLLL	with	h decay mo	ode other tha	n alpha emissio	on or spontaneous	
3 2	2 fission and with radioactive half-life less than two hours:						
33	Sub	2	1X10 ⁻⁶		3X10 ⁻⁸		

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1NNNN. Any single radionuclide not listed in items A2to LLLL with decay mode other than alpha emission or spontaneous3fission and with radioactive half-life greater than two hours:4 $3x10^{-9}$ $9x10^{-5}$ $1x10^{-10}$ $3x10^{-9}$ $9x10^{-5}$ $1x10^{-10}$

5 0000. Any single radionuclide not listed in items A 6 to LLLL that decays by alpha emission or spontaneous fission: 7 6×10^{-13} 4×10^{-7} 2×10^{-14} 3×10^{-8}

8 * The values of Ge-68, Au-195, and Y-88 have been
9 calculated using the committed dose equivalent values of ICRP
10 Publication 30 for the controlling organ.

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¹ Soluble (S); Insoluble (I)

12 ² "Sub" means that values given are for submersion in a 13 semispherical infinite cloud of airborne material.

³ These radon concentrations are appropriate for protection 14 15 from radon-222 combined with its short-lived daughters. 16 Alternatively, the value in Table I may be replaced by one-third "working level." A working level is any combination of 17 18 short-lived radon-222 daughters, polonium-218, lead-214, 19 bismuth-214, and polonium-214, in one liter of air, without regard to the degree of equilibrium, that will result in the 20 ultimate emission of 1.3×10^5 MeV of alpha particle energy. 21 The Table II value may be replaced by one-thirtieth of a working 22 level. The limit on radon-222 concentrations in restricted 23 areas may be based 'on an annual average. 24

 4 For soluble mixtures of U-238, U-234, and U-235 in air, 25 chemical toxicity may be the limiting factor. If the percent by 26 weight (enrichment) of U-235 is less than five, the 27 concentration value for a 40-hour workweek, Table I, is 0.2 28 milligrams uranium per cubic meter of air average. For any 29 enrichment, the product of the average concentration and time of 30 exposure during a 40-hour workweek shall not exceed $8X10^{-3}$ SA 31 uCi-hr/ml, where SA is the specific activity of the uranium 32 inhaled. The concentration value for Table II is 0.007 33 milligrams uranium per cubic meter of air. The specific 34 activity for natural uranium is 6.77×10^{-7} curies per gram 35

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uranium. The specific activity for other mixtures of U-238, 1 2 U-235, and U-234, if not known, shall be: SA = 3.6×10^{-7} curies/gram U SA = $(0.4 + 0.38 \times +0.0034 \times 10^{-6})$ 3 U-depleted 4 E > 0.72where E is the percentage by weight of U-235, expressed as 5 6 percent. 7 Note: In any case where there is a mixture in air or water of more than one radionuclide, the limiting values for the 8 9 purpose of this Appendix shall be determined according to subitems (1) to (5). 10 11 (1) If the identity and concentration of each 12 radionuclide in the mixture are known, the limiting values shall be derived as follows: determine, for each radionuclide in the 13 mixture, the ratio between the quantity present in the mixture 14 and the limit otherwise established in Appendix A for the 15 specific radionuclide when not in a mixture. The sum of the 16 ratios for all the radionuclides in the mixture may not exceed 17 18 one. 19 If the radionuclides a, b, and c are present in Example: 20 concentrations Ca, Cb, and Cc, and if the applicable maximum permissible concentrations (MPC's) are MPCa, MPCb, and MPCc, 21 respectively, then the concentrations shall be limited so that 22 23 the following relationship exists: 24 C_C C_a + Ch < 1 25 26 MPCC MPCa MPCh 27 (2) If either the identity or the concentration 28 of any radionuclide in the mixture is not known, the limiting 29 values for purposes of Appendix A shall be: 30 (a) for purposes of Table I, Column 1, 6X10⁻¹³: 31 32 (b) for purposes of Table I, Column 2, $4 \times 10^{-7};$ 33 34 (c) for purposes of Table II, Column 1, $2X10^{-14}$; and 35 36 (d) for purposes of Table II, Column 2, 3X10⁻⁸. 37 38 (3) If any of the conditions in units (a) to (c) Approved

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08/01/91 [REVISOR] LMB/BD AR1543 are met, the corresponding values may be used in lieu of those 1 in subitem (2). 2 (a) If the identity of each radionuclide in 3 the mixture is known but the concentration of one or more of the 4 in the mixture is not known, the concentration limit for the 5 mixture is the limit in Appendix A for the radionuclide in the 6 mixture having the lowest concentration limit. 7 (b) If the identity of each radionuclide in 8 the mixture is not known but it is known that certain 9 radionuclides in Appendix A are not present in the mixture, the 10 concentration limit for the mixture is the lowest concentration 11 limit in Appendix A for any radionuclide that is not known to be 12 13 absent from the mixture. (c) Radionuclide 14 Table I Table II 15 Column 2 Column l 16 Column 1 Column 2 Air Water Air Water 17 (µCi/ml) (µCi/ml) (µCi/ml) (µCi/ml) 18 i. If it is known that Sr-90, I-125, 19 I-126, I-129, I-131, (I-133 Table II only), Pb-210, Po-210, 20 At-211, Ra-223, Ra-224, Ra-226, Ac-227, Ra-228, Th-230, Pa-231, 21 Th-232, Th-natural, Cm-248, Cf-254, and Fm-256 are not present: 22 9x10⁻⁵ $3X10^{-6}$. _____ -----23 <u>،</u> ii. If it is known that Sr-90, I-125, 24 I-126, I-129, (I-131, I-133 Table II only), Pb-210, Po-210, 25 Ra-223, Ra-226, Ra-228, Pa-231, Th-natural, Cm-248, Cf-254, and 26 Fm-256 are not present: 27 $2X10^{-6}$. 6X10⁻⁵ _____ ____ 28 iii. If it is known that Sr-90, I-129, 29 (I-125, I-126, I-131, Table II only), Pb-210, Ra-226, Ra-228, 30 Cm-248, and Cf-254 are not present: 31 6×10^{-7} . 2×10^{-5} _____ _____ 32 iv. If it is known that (I-129, Table 33

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08/01/91 [REVISOR] LMB/BD AR1543 II only), Ra-226, and Ra-228 are not present: 1 3X10⁻⁶ 2 _____ 1×10^{-7} . _____ 3 v. If it is known that alpha emitters and Sr-90, I-129, Pb-210, Ac-227, Ra-228, Ac-230 Pa-230, Pu-241, 4 5 and Bk-249 are not present: 3X10⁻⁹ 1X10⁻¹⁰ 6 ____ ----. 7 vi. If it is known that alpha emitters and Pb-210, Ac-227, Ra-228, and Pu-241 are not present: 8 3×10^{-10} _____ 1X10⁻¹¹ 9 _____ 10 vii. If it is known that alpha 11 emitters and Ac-227 are not present: 3×10^{-11} 1X10⁻¹² 12 _____ _____ 13 viii. If it is known that Ac-227, Th-230, Pa-231, Pu-238, Pu-239, Pu-240, Pu-242, Pu-244, Cm-248, 14 Cf-249, and Cf-251 are not present: 15 3×10^{-12} _____ $1X13^{-13}$ 16 _____ 17 (4) If a mixture of radionuclides consists of 18 uranium and its daughters in ore dust before chemical separation of the uranium from the ore, the values in units (a) and (b) may 19 20 be used for uranium and its daughters through radium-226, instead of those in subitems (1) to (3). 21 (a) For purposes of Table I, Column 1, 22 23 $1X10^{-10} \ \mu Ci/ml$ gross alpha activity; $5X10^{-11} \ \mu Ci/ml$ natural uranium; or 75 micrograms per cubic meter of air natural uranium. 24 25 (b) For purposes of Table II, Column I, $3X10^{-12} \mu Ci/ml$ gross alpha activity; $2X10^{-12} \mu Ci/ml$ natural 26 uranium; or 3 micrograms per cubic meter of air natural uranium. 27 28 (5) For purposes of this note, a radionuclide may be considered as not present in a mixture if: 29 30 (a) the ratio of the concentration of that 31 radionuclide in the mixture (C_a) to the concentration limit for 32 that radionuclide specified in Table II of Appendix A (MPCa) does not exceed 1/10, for example $C_a/MPC_a \le 1/10$; and 33

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1 (b) the sum of the ratios for all radionuclides considered as not present in the mixture does not 2 exceed 1/4, for example $C_a/MPC_a + C_b/MPC_b + \dots \le 1/4$. 3 Note: To convert $\mu \text{Ci}/\text{ml}$ to SI units of megabecquerels per 4 liter multiply the values in subitem (5) by 37. 5 Example: Zirconium (40) Zr-97 S (Table I, Column 1-Air) 6 $(1X10^{-7} \mu Ci/ml multiplied by 37 is equivalent to 37X10^{-7} MBq/l.)$ 7 REPEALER. Minnesota Rules, parts 4730.0100, subparts 11, 17, 8 21, 27, 29, 31, and 41; 4730.0300, subpart 4; 4730.0700, 9 subparts 1 and 2; 4730.1100; 4730.1200; 4730.1300; 4730.1500; 10 4730-1600; 4730.1650; 4730.1660; 4730.1700; 4730.1800; 11 4730.1900; 4730.2000; 4730.2100; 4730.2200; 4730.2300; 12 4730.2400; 4730.3300; and 4730.3600, are repealed. 13 14 EFFECTIVE DATE. Minnesota Rules, parts 4730.0100 to 15 16 4730.3605, shall be effective five working days after

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17 publication of the adopted rules in the State Register.

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